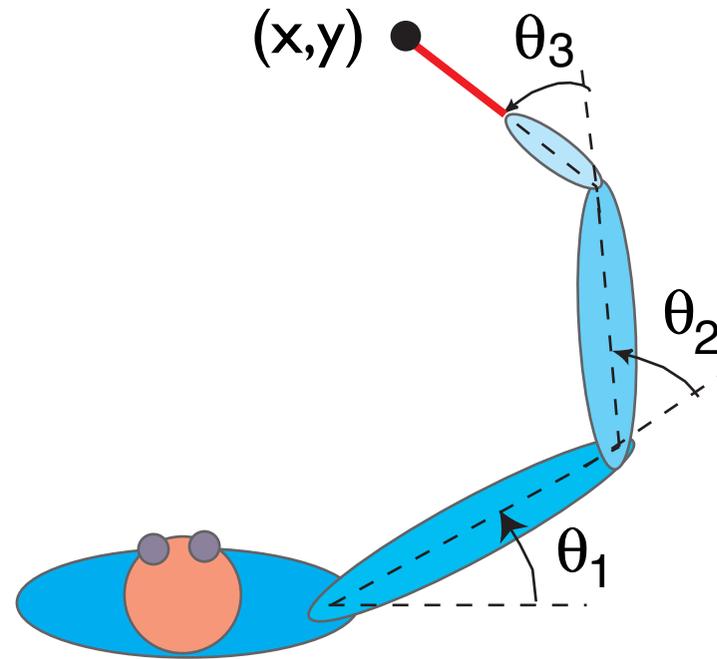


Degree of Freedom problem, synergies, and the uncontrolled manifold

Gregor Schöner
Institut für Neuroinformatik
Ruhr-Universität Bochum, Germany

Degree of freedom problem

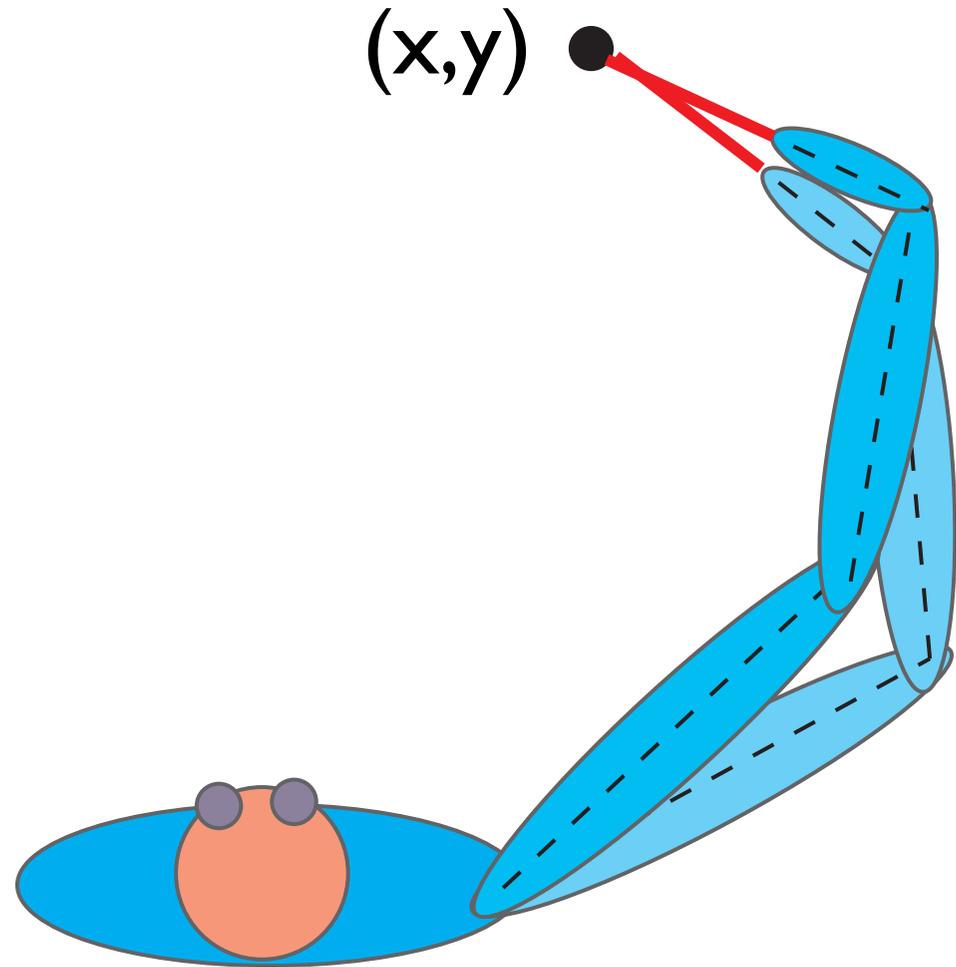
■ what is a DoF?



$$x = l_1 \cos(\theta_1) + l_2 \cos(\theta_1 + \theta_2) + l_3 \cos(\theta_1 + \theta_2 + \theta_3)$$
$$y = l_1 \sin(\theta_1) + l_2 \sin(\theta_1 + \theta_2) + l_3 \sin(\theta_1 + \theta_2 + \theta_3)$$

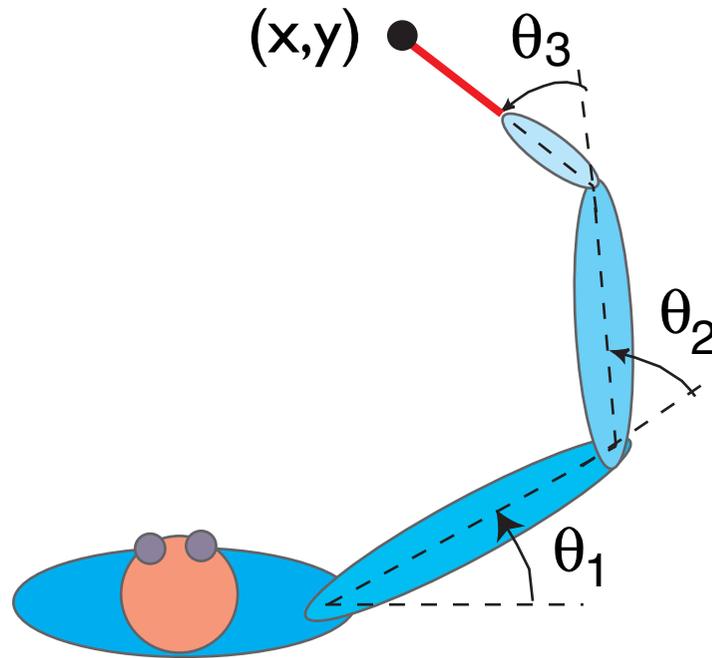
The degree of freedom problem

- The strongest form of the DoF problem:
redundant effector systems
- **redundance** being defined relative to a task



Redundancy formalized

- task variable (x,y)
- elemental variables joint angles θ_1 , θ_2 , θ_3



$$x = l_1 \cos(\theta_1) + l_2 \cos(\theta_1 + \theta_2) + l_3 \cos(\theta_1 + \theta_2 + \theta_3)$$
$$y = l_1 \sin(\theta_1) + l_2 \sin(\theta_1 + \theta_2) + l_3 \sin(\theta_1 + \theta_2 + \theta_3)$$

Degree of freedom problem

- is it relevant?
- yes... in many tasks redundancy occurs
 - e.g., 3D positioning in point vs. >10 joints in an arm
- second level of redundancy:
 - many muscles per joint (e.g. about 750 muscles in the human body vs. about 50 Dof)

Bernstein problem

- Nikolai Bernstein... 1930's... in the Soviet Union
- “how to harness the many DoF to achieve the task”

Bernstein's workers

- highly skilled workers wielding a hammer to hit a nail... => hammer trajectory in space less variable than body configuration
 - as detected in superposing spatial trajectories of lights on hammer vs. on body..
- but:
 - camera frame anchored to nail/space, while initial body configuration varied

Bernstein's workers

- was the hammer position in space less variable than the joint configuration?
 - that is, does the task structure variance?
 - so that the solution to the degree of freedom problem lies in the variance/stability of the joint configuration?
- but: does this make any sense?
 - different reference frames for body vs. task
 - different units in the task vs joint space

The concept of a synergy: classical

- multiple degrees of freedom/muscles are co-activated in a characteristic pattern
- leading to covariation of these DoF/muscle activations in time
- leading to covariation of these DoF/muscle activation when movement parameters are varied
- “sharing” aspect of synergies

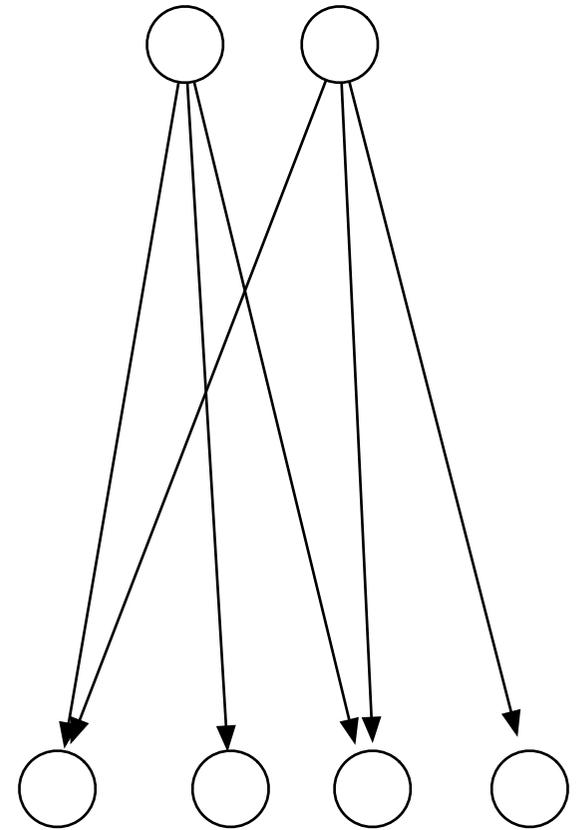
Classical synergy: data analysis

- Throw data from time series under different conditions (sometimes including repetitions of movements) into one big data set and look for principal components
- if a small number of PC's is sufficient to account for most of the variance, conclude that few synergies are at work
- or establish co-variation among DoF/ muscles directly by testing for significant correlation

Classical synergy: accounts

- A small number of descending commands specify the synergies
- these are distributed to a large number of DoFs/muscles by a forward neural network
- the forward connectivity pattern defines the synergy
- induces the co-variation among the DoF when the command varies.

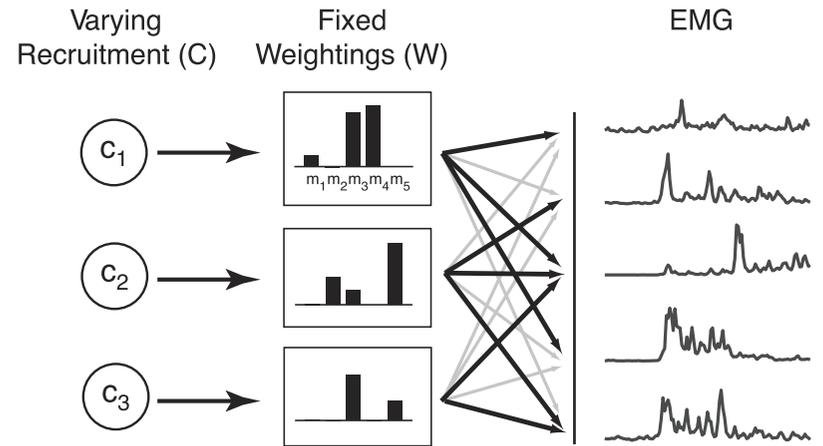
motor commands



DoF/muscles

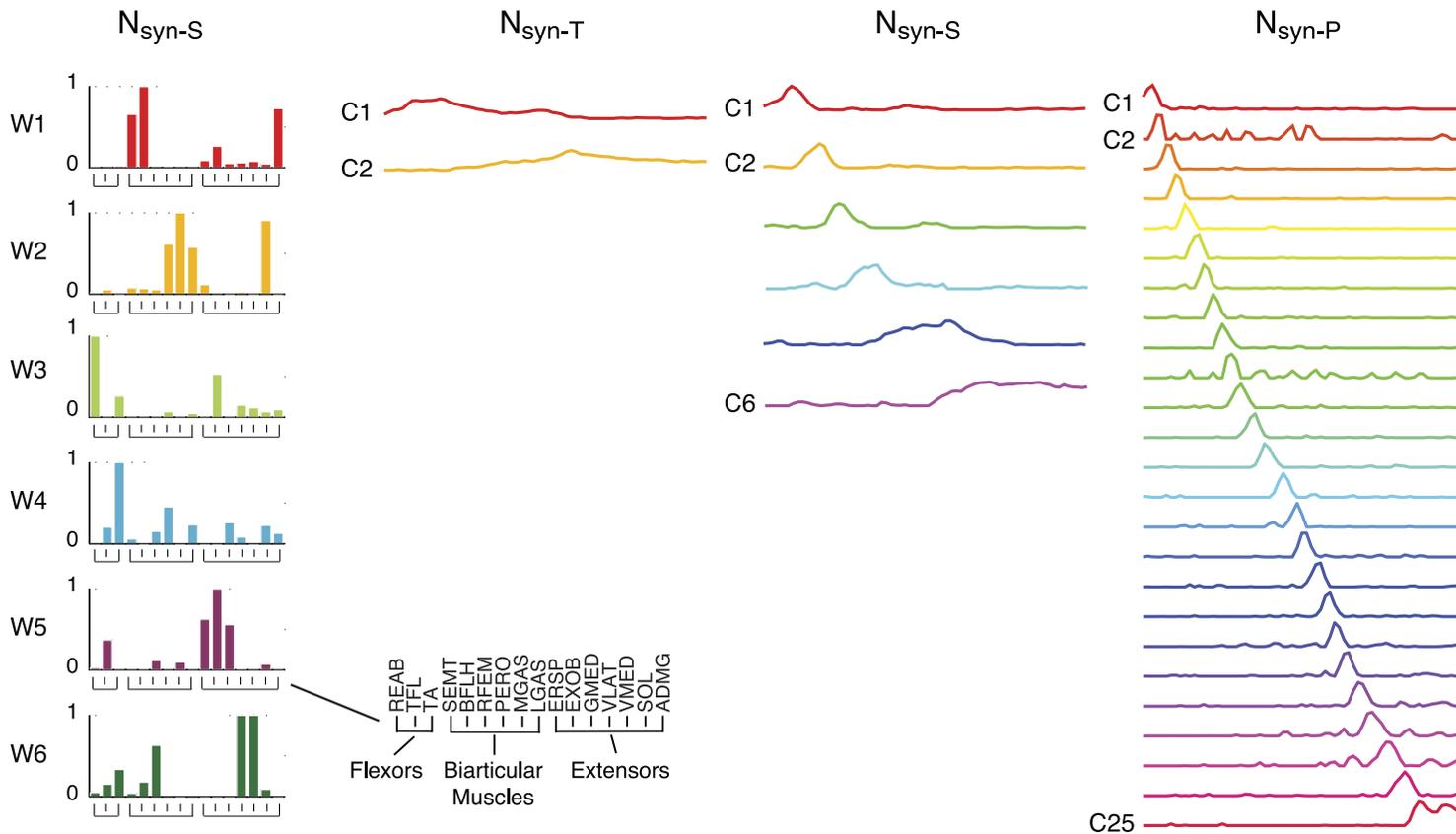
Synergy: experimental use

■ E.g, Safavynia, Ting, 2012:



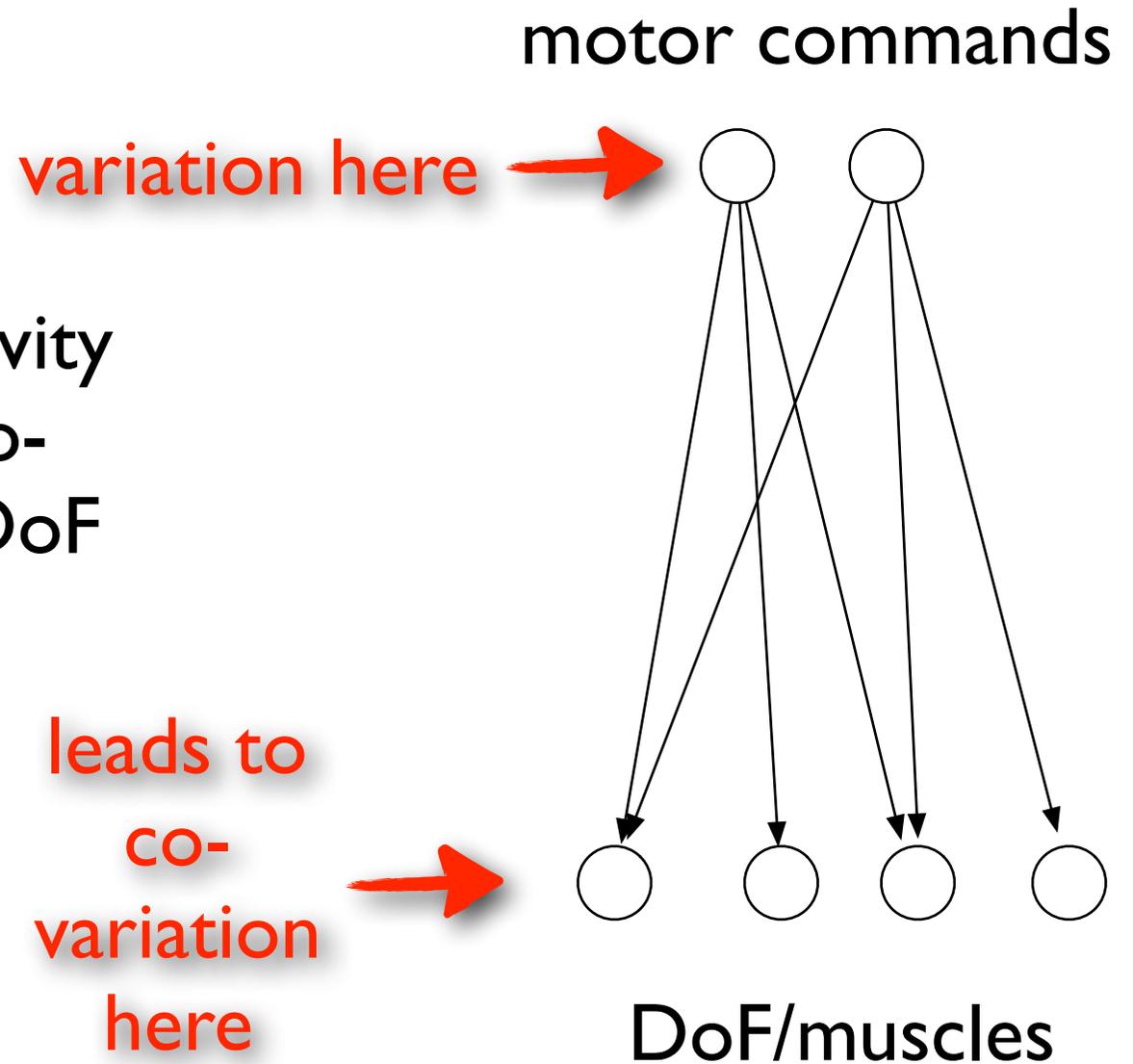
SF Muscle Synergies

TF Muscle Synergies



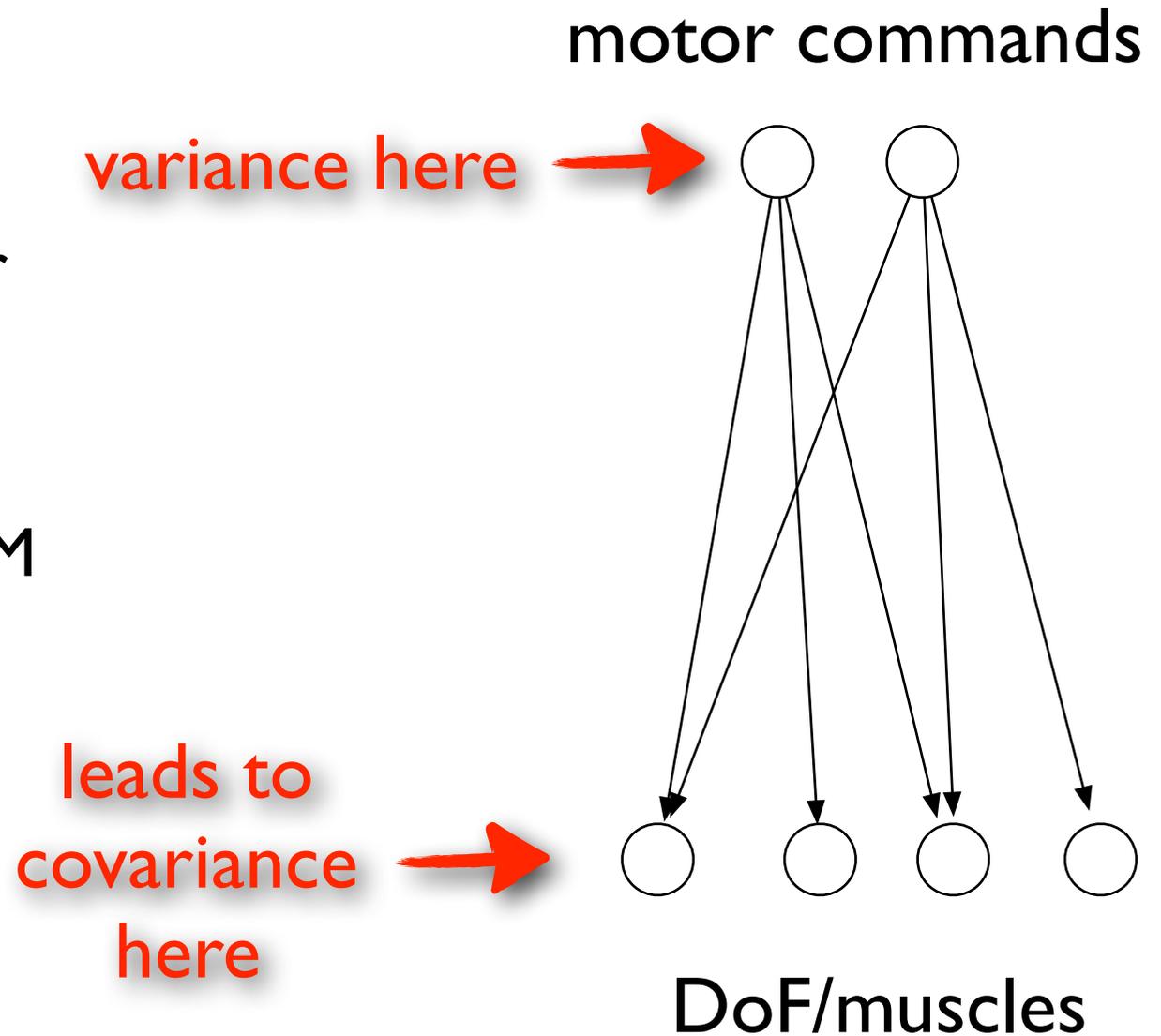
Classical synergy: accounts

- The forward connectivity pattern induces the co-variation among the DoF when the command varies.



Classical synergy: variance

- Variance that arises from stochastic motor commands induces covariance at DoFs
- = opposite of the UCM (“anti-correlation” or “compensation”)
- => tension between classical synergy and UCM

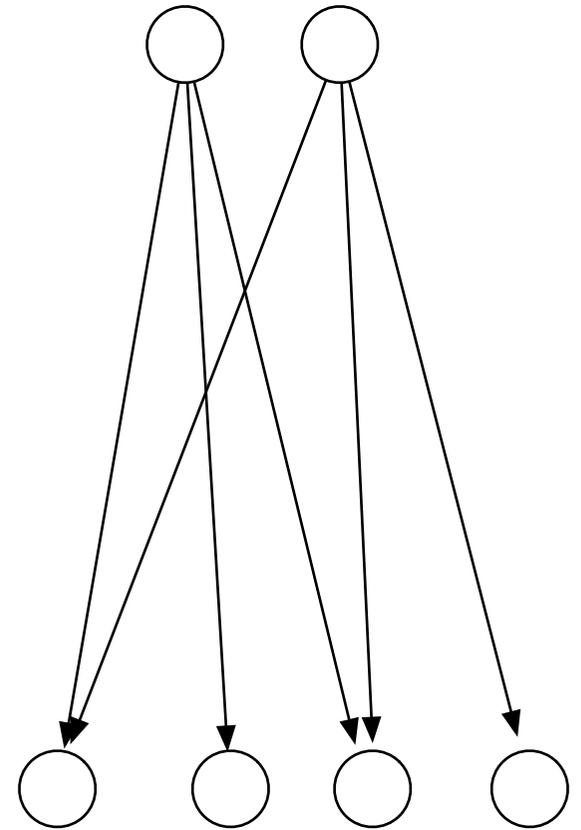


Classical synergy: variance

- variance induced at the level of the individual DoF/muscles is uncorrelated
- = the null hypothesis of UCM: the same variance in all direction
- => tension between classical synergy and UCM

variance induced here: is uncorrelated →

motor commands



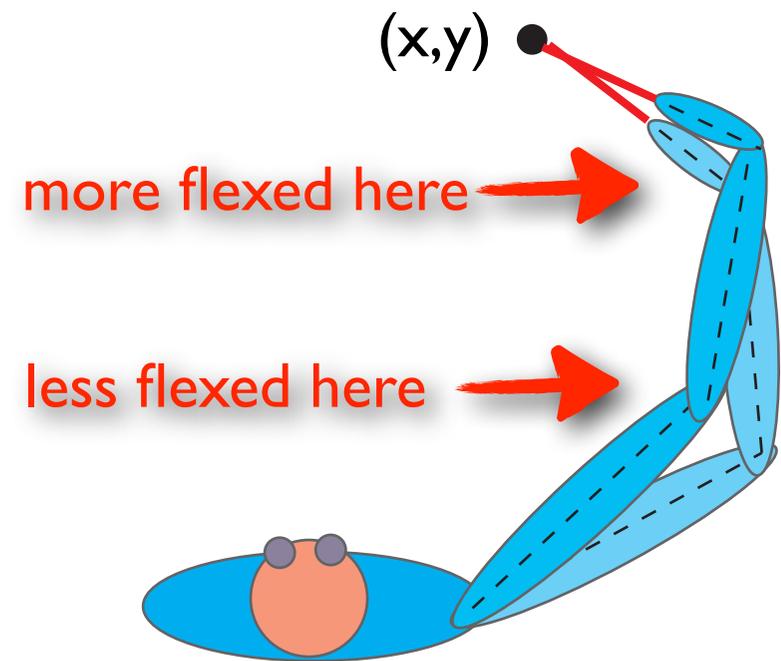
DoF/muscles

Classical synergy: DoF problem

- classical synergy concept is thought of as a solution to the DoF problem: shared input

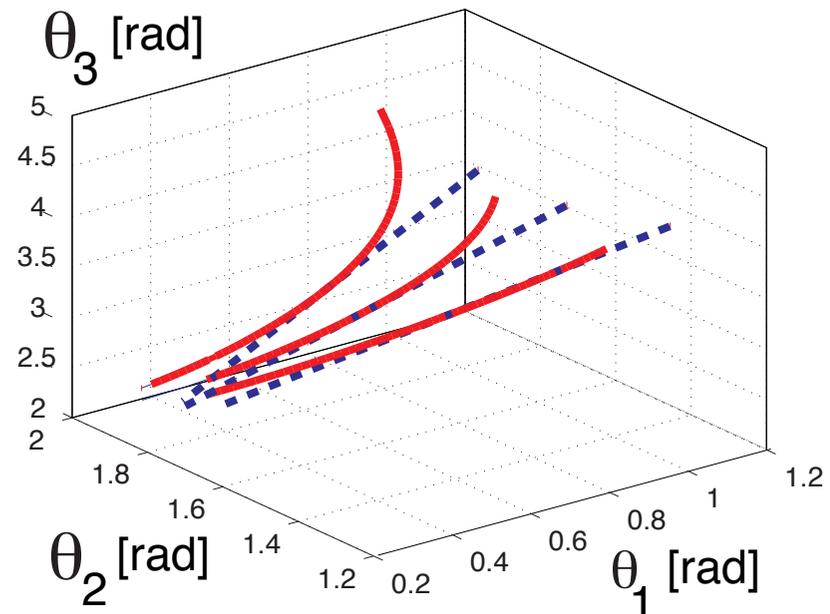
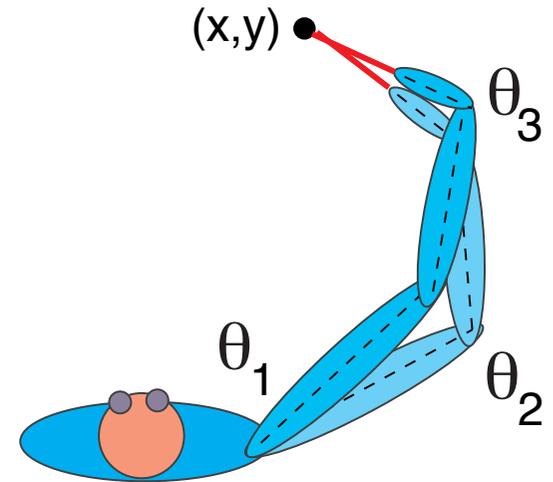
uncontrolled manifold (UCM)

- the many DoF are coordinated such that variance that affects a smaller number of task variables is smaller than variance that does not affect a task variable
- leading to compensation among DoF (or “anti-correlation”)



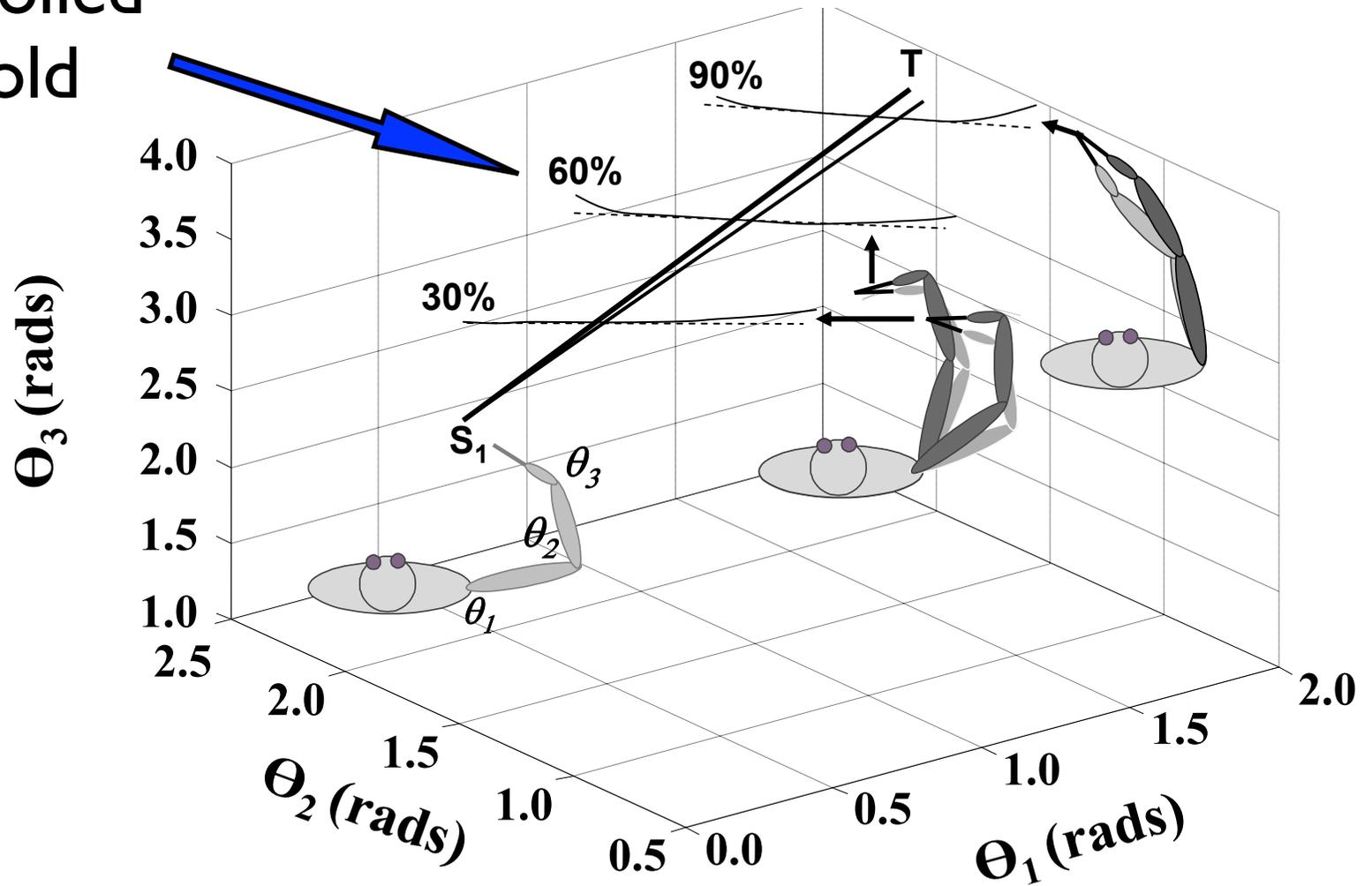
UCM synergy: data analysis

- hypothesis testing
 - align trials in time, computer variance at each time slices
 - formulate hypothesis about task variable
 - compute null-space (tangent to the “uncontrolled manifold”)
 - predict there is more variance within null space than perpendicular to it



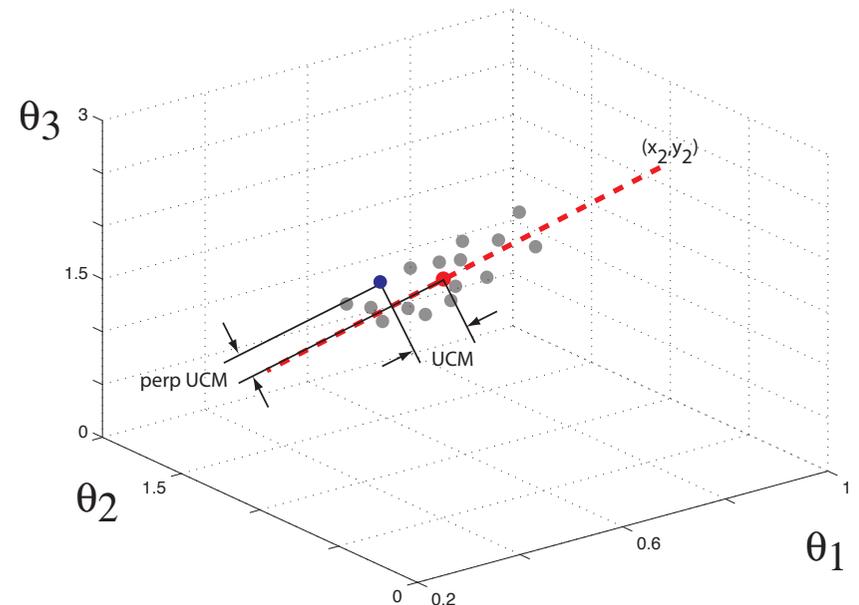
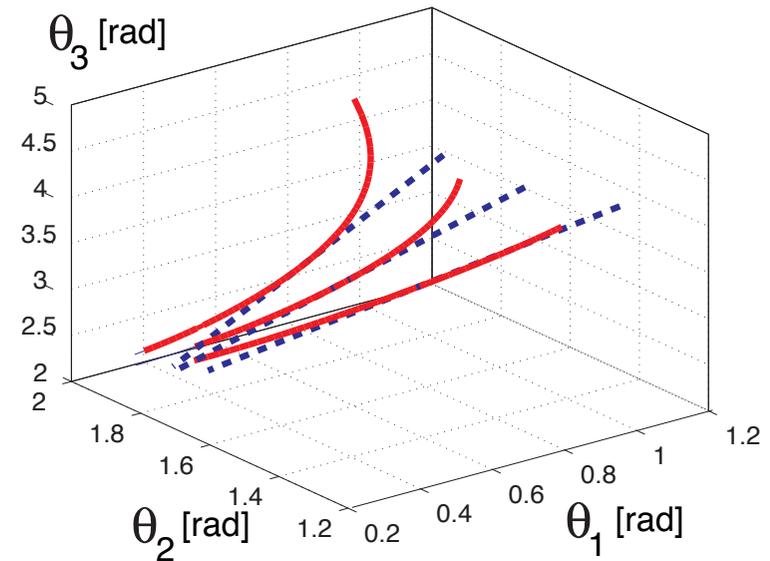
uncontrolled manifold hypothesis

uncontrolled manifold



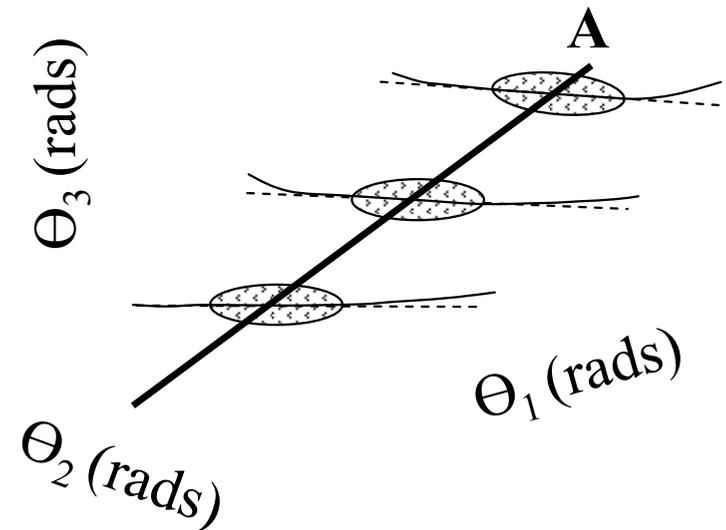
UCM synergy: data analysis

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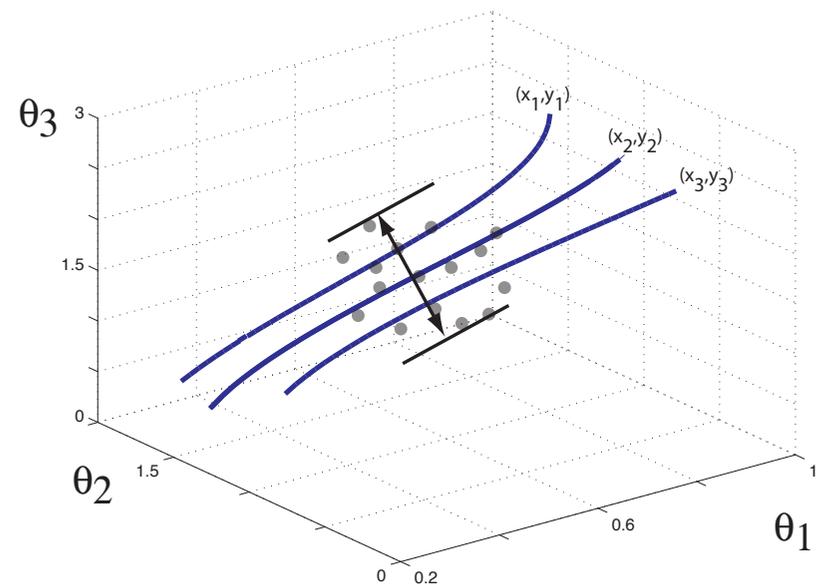
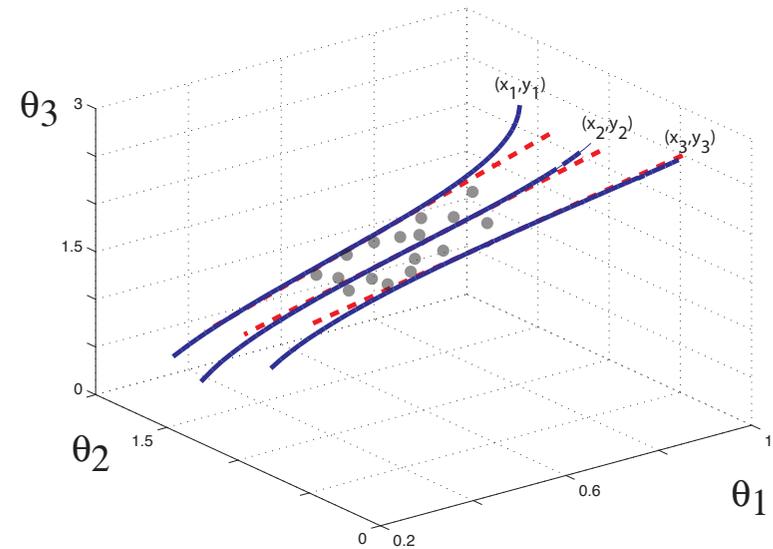
UCM synergy: data analysis

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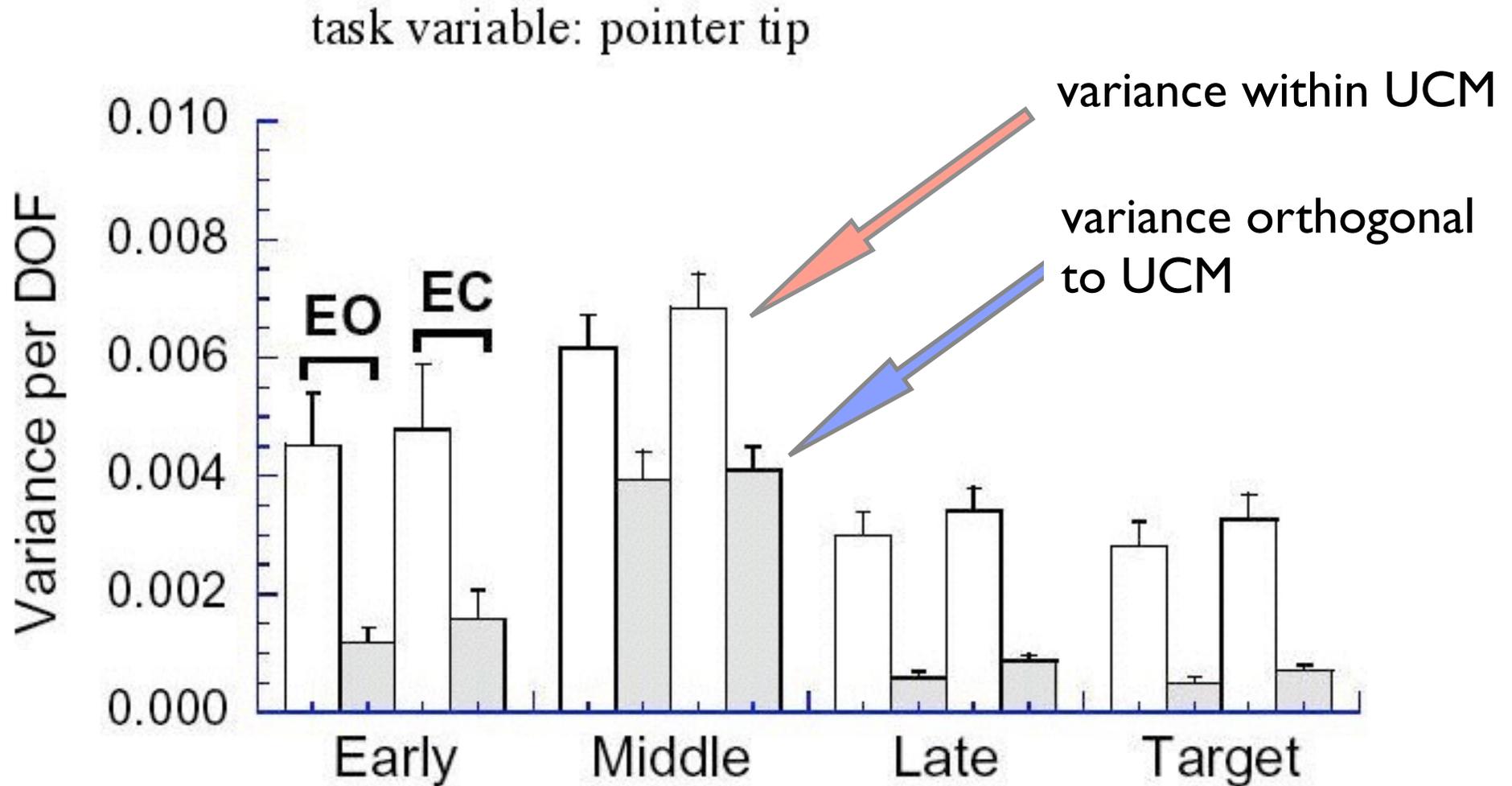


UCM synergy: data analysis

- supplement hypothesis testing by checking for correlation (Hermann, Sternad...)
- look for increase in variance of task variable when correlation within data is destroyed



Example 1: pointing with 10 DoF arm at targets in 3D

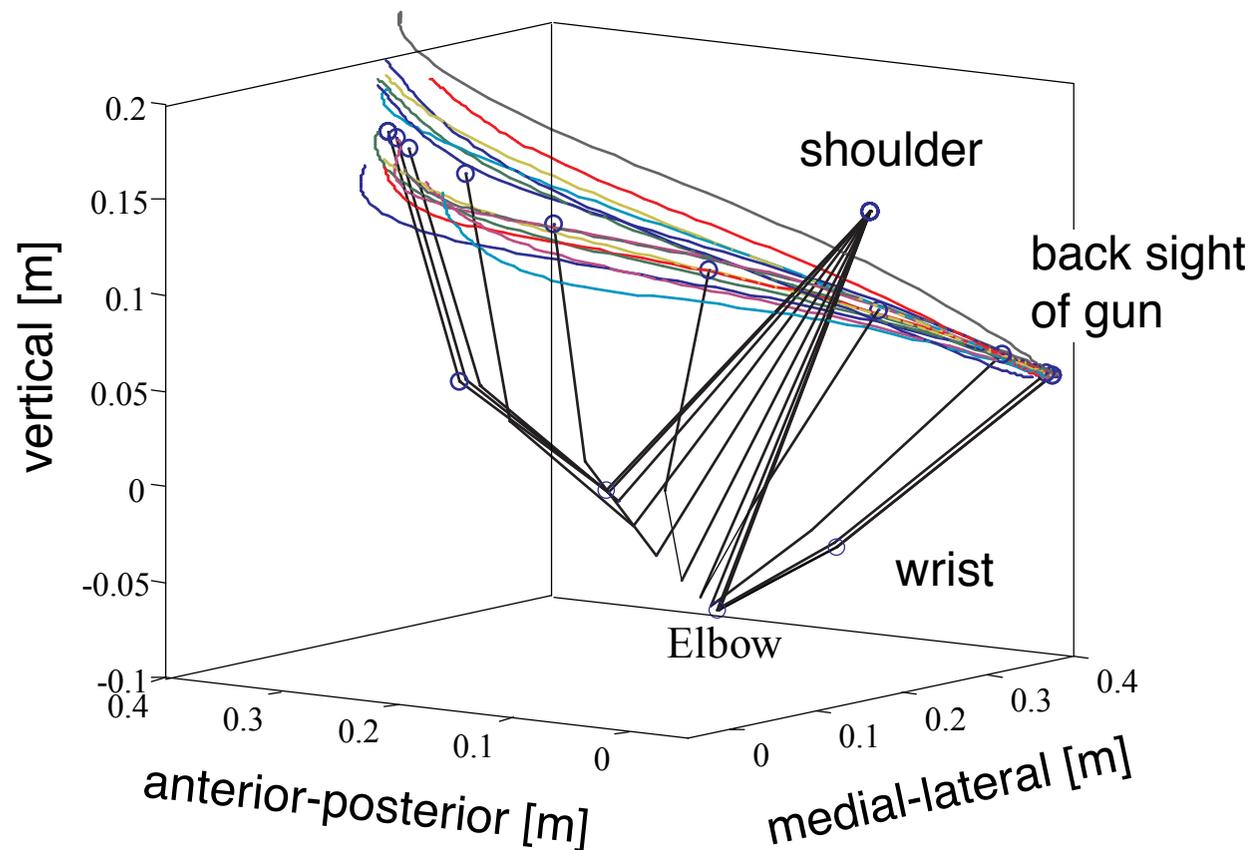
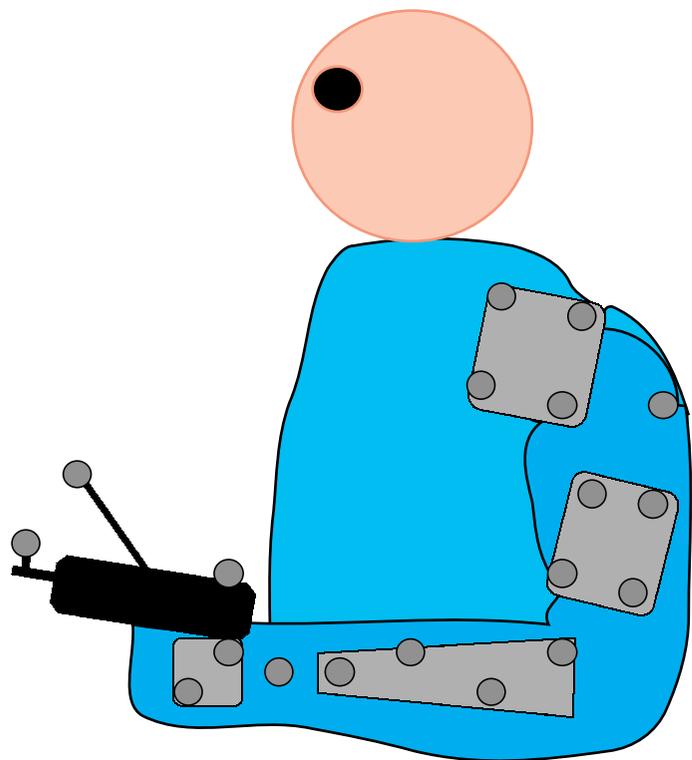


[from: Tseng, Scholz, Schöner: Motor Control (2002)]

task specificity of the structure of the joint variance

- is joint variance always structured by the end-effector spatial position?
- no: depends on task

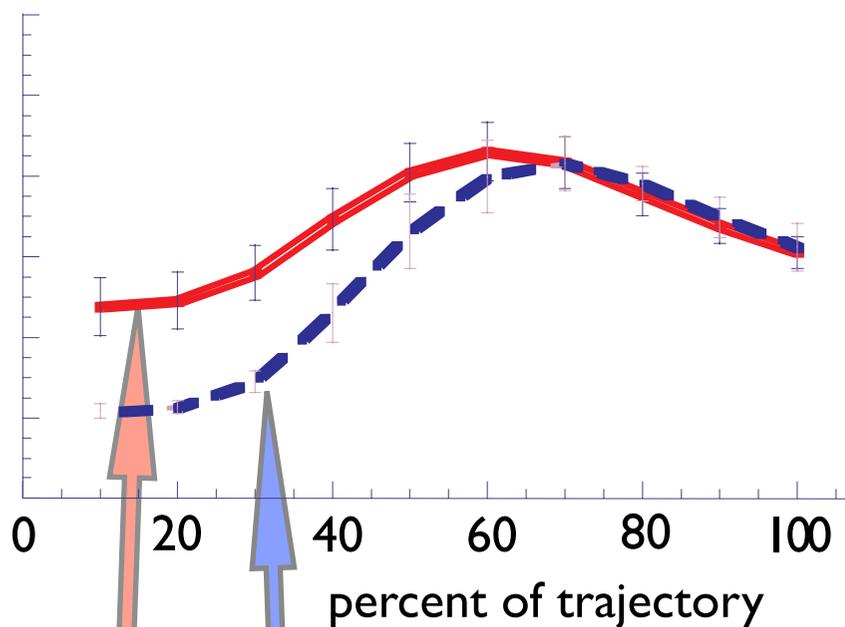
Example 2: shooting with 7 DoF arm at targets in 3D



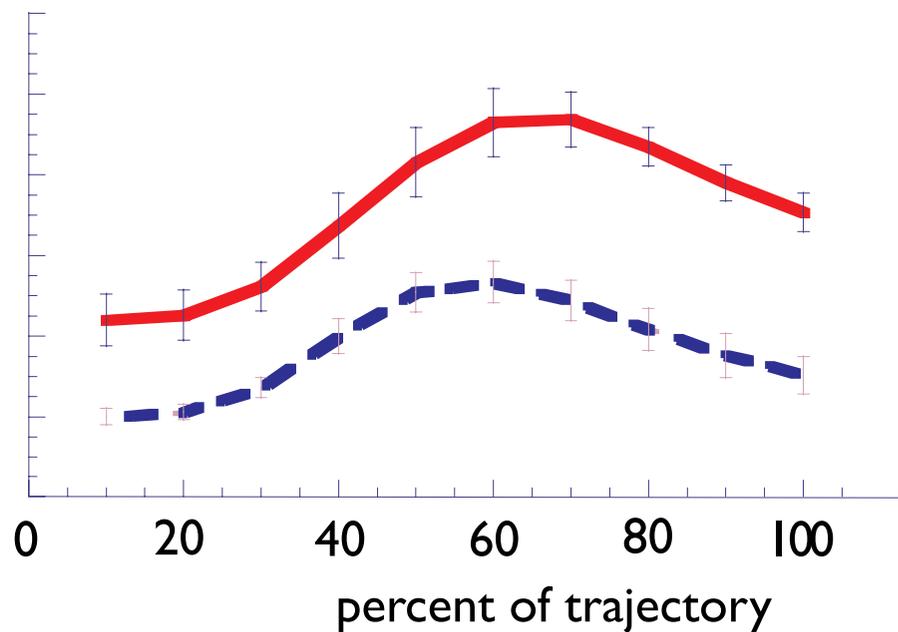
[from Scholz, Schöner, Latash: EBR 135:382 (2000)]

Example 2: shooting with 7 DoF arm at targets in 3D

gun spatial position



gun orientation to target



[from Scholz, Schöner, Latash: EBR 135:382 (2000)]

variance
within
UCM

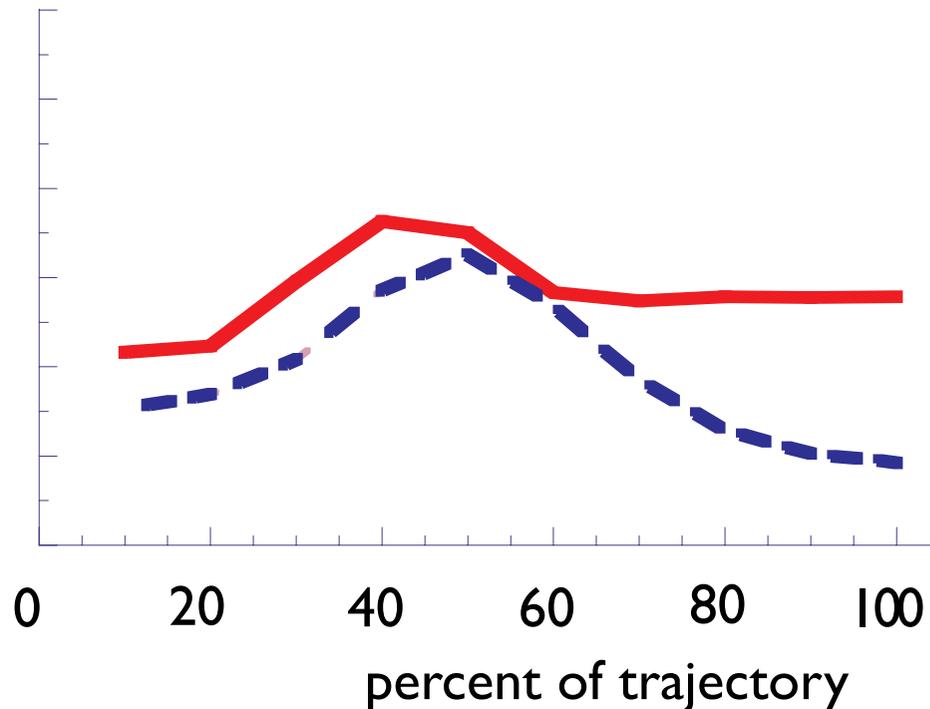
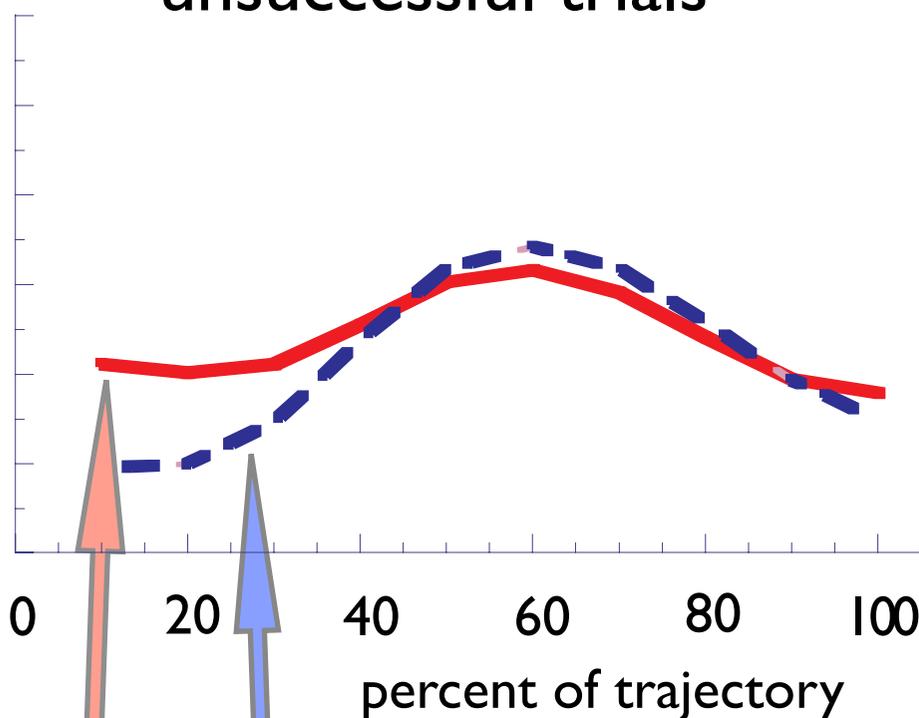
variance
perpendicular
to UCM

Example 2: shooting with 7 DoF arm at targets in 3D

hypothesis: gun orientation, data from one participant

unsuccessful trials

successful trials



[from Scholz, Schöner, Latash: EBR 135:382 (2000)]

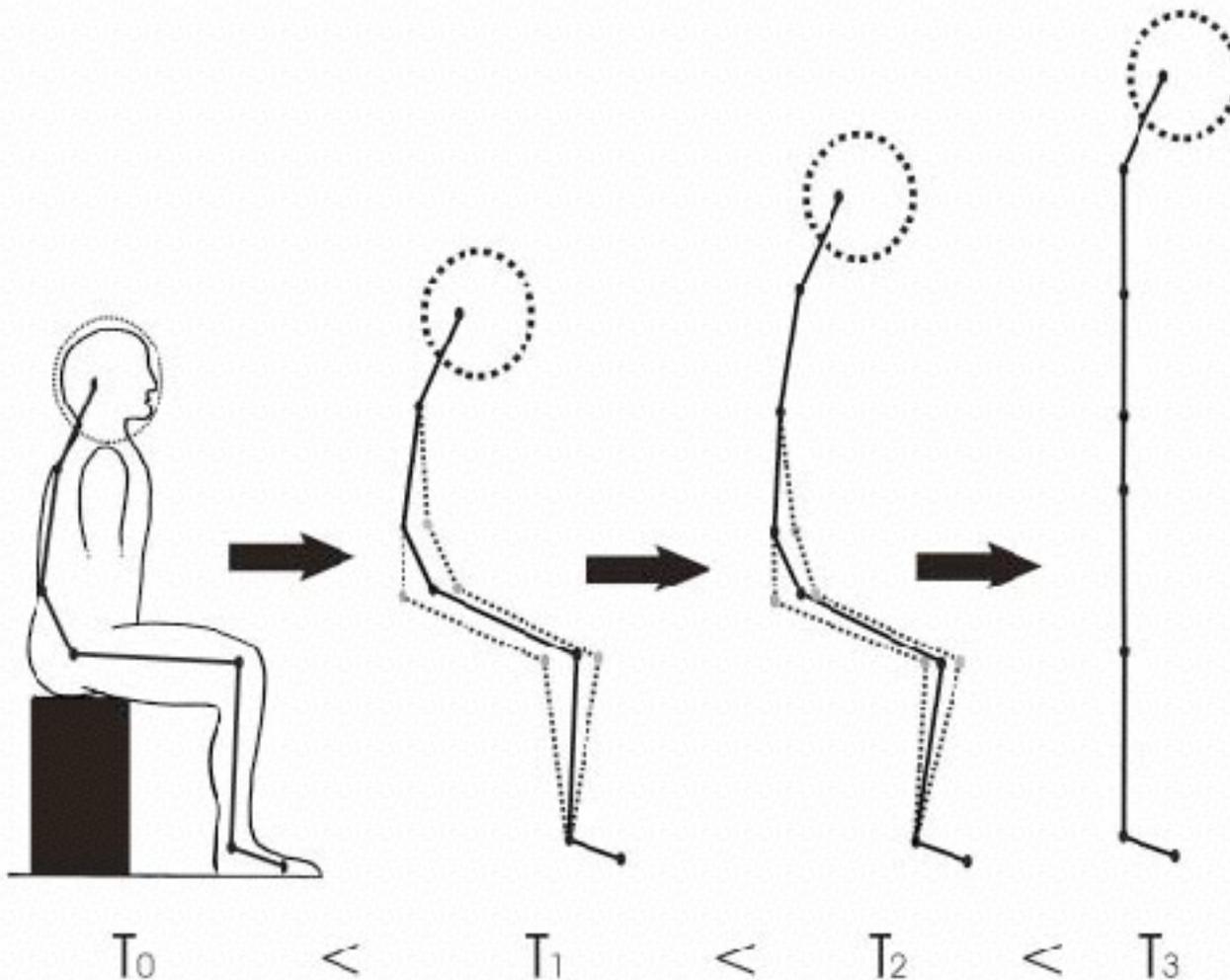
variance
within
UCM

variance
perpendicular
to UCM

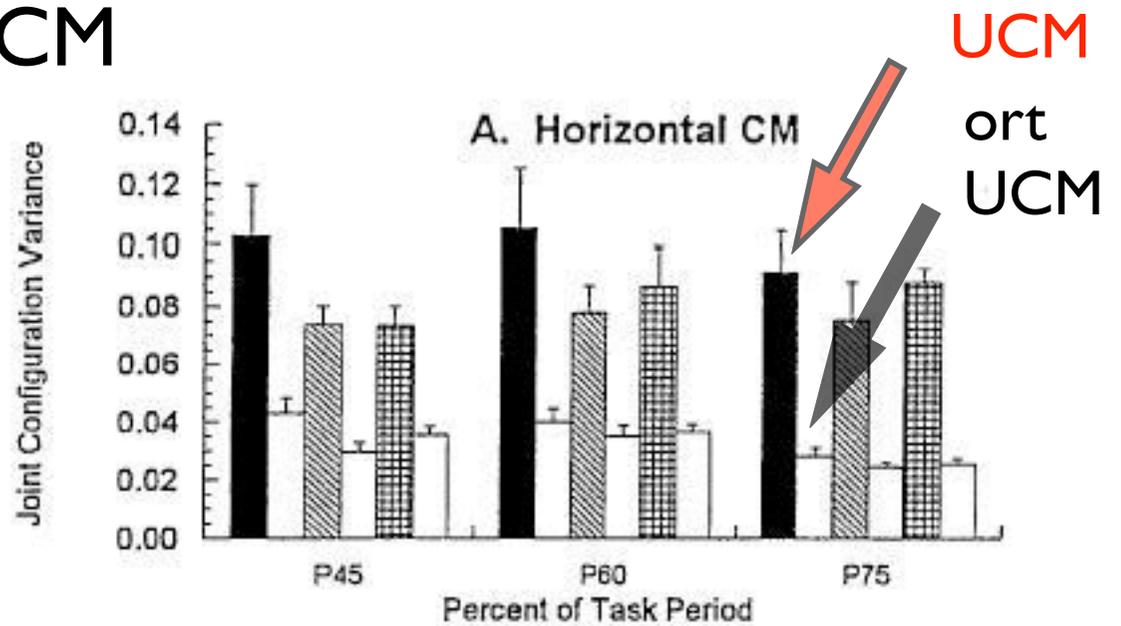
limits of redundancy

Example 3:

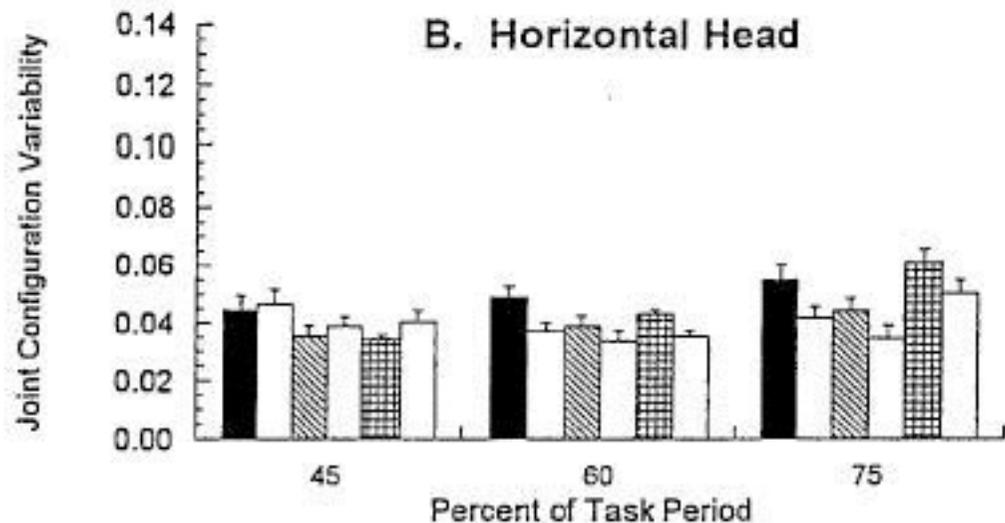
sit to stand transition as a whole body movement



hypothesis: horizontal CM

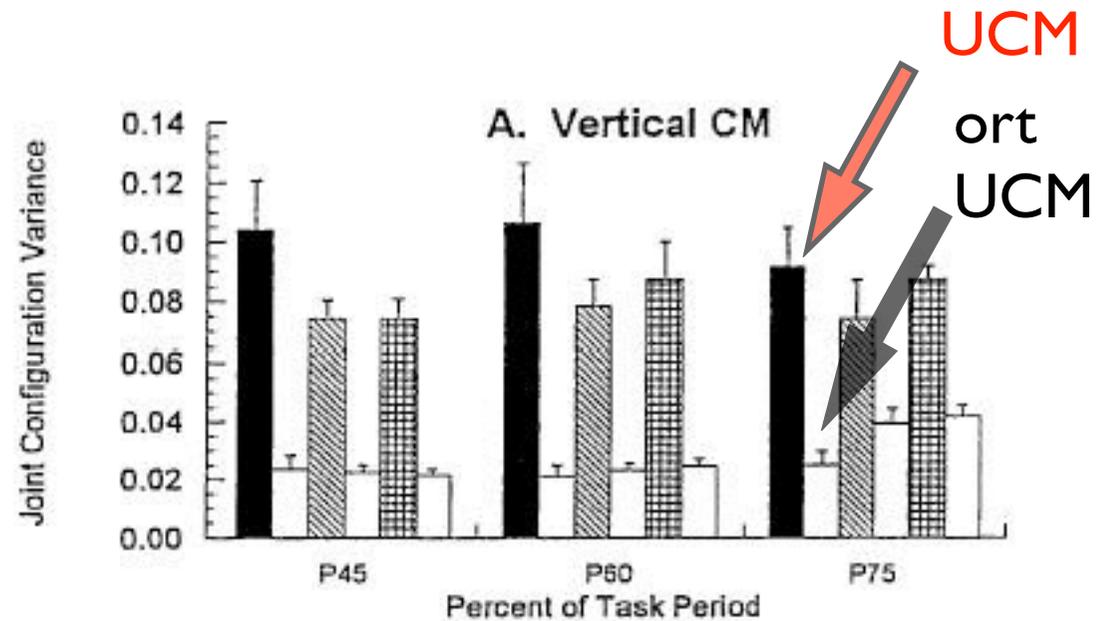


hypothesis: horizontal head position



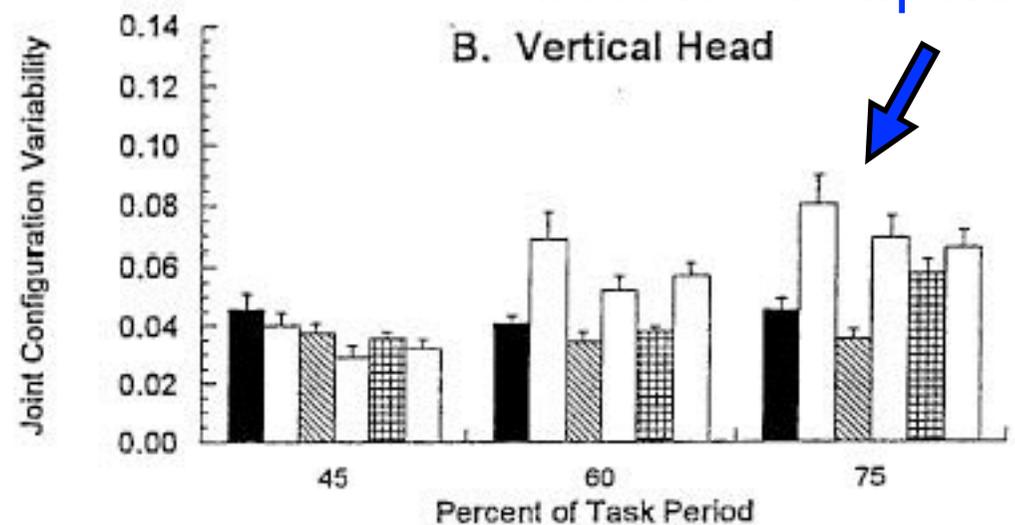
[from: Scholz, Schöner EBR 126:289 (1999)]

hypothesis: vertical CM



hypothesis: vertical head position

loss of redundancy at the limit of workspace



[from: Scholz, Schöner, EBR 126:289 (1999)]

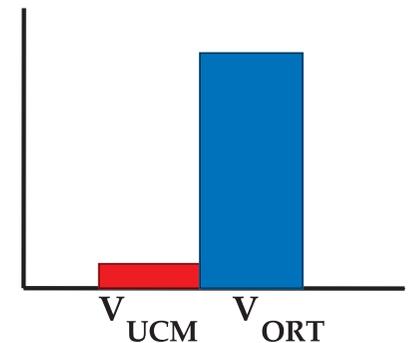
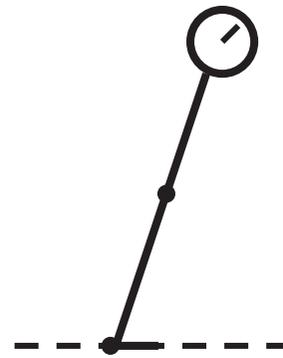
UCM synergy: account

- more complex than for classical synergy...
let's go through case studies first

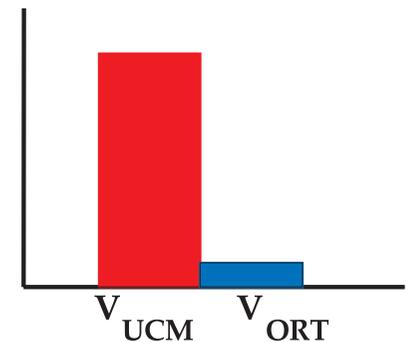
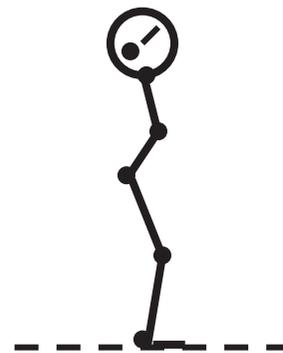
UCM synergy: accounts.

Case study posture

■ UCM non-trivial in posture because the classical inverted pendulum hypothesis predicts the opposite:

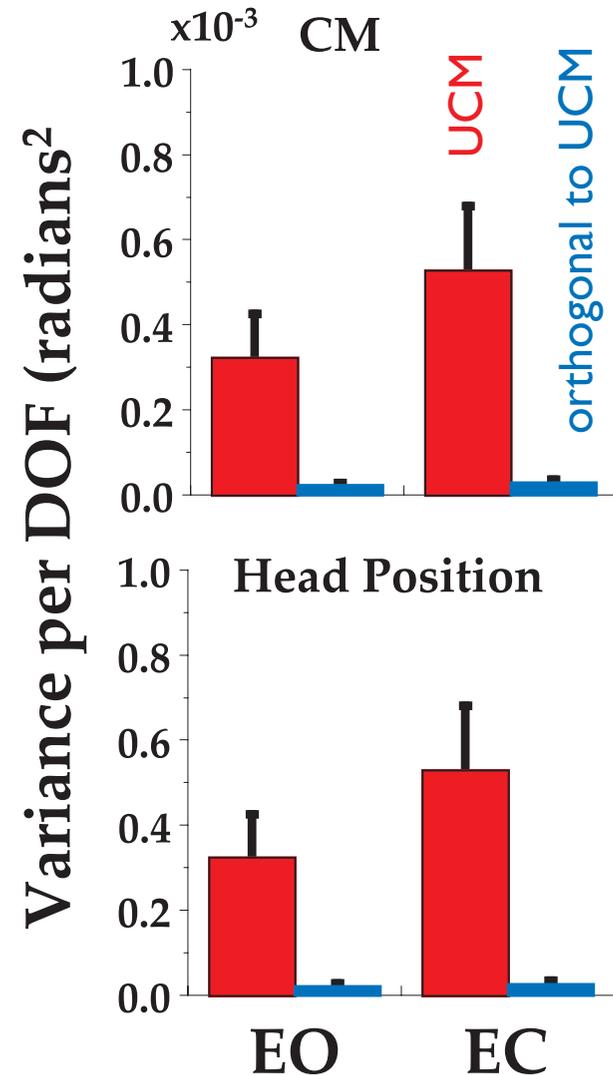


■ because the ankle moves the body in space, it lies orthogonal to the UCM predicting more variance in ORT than in UCM

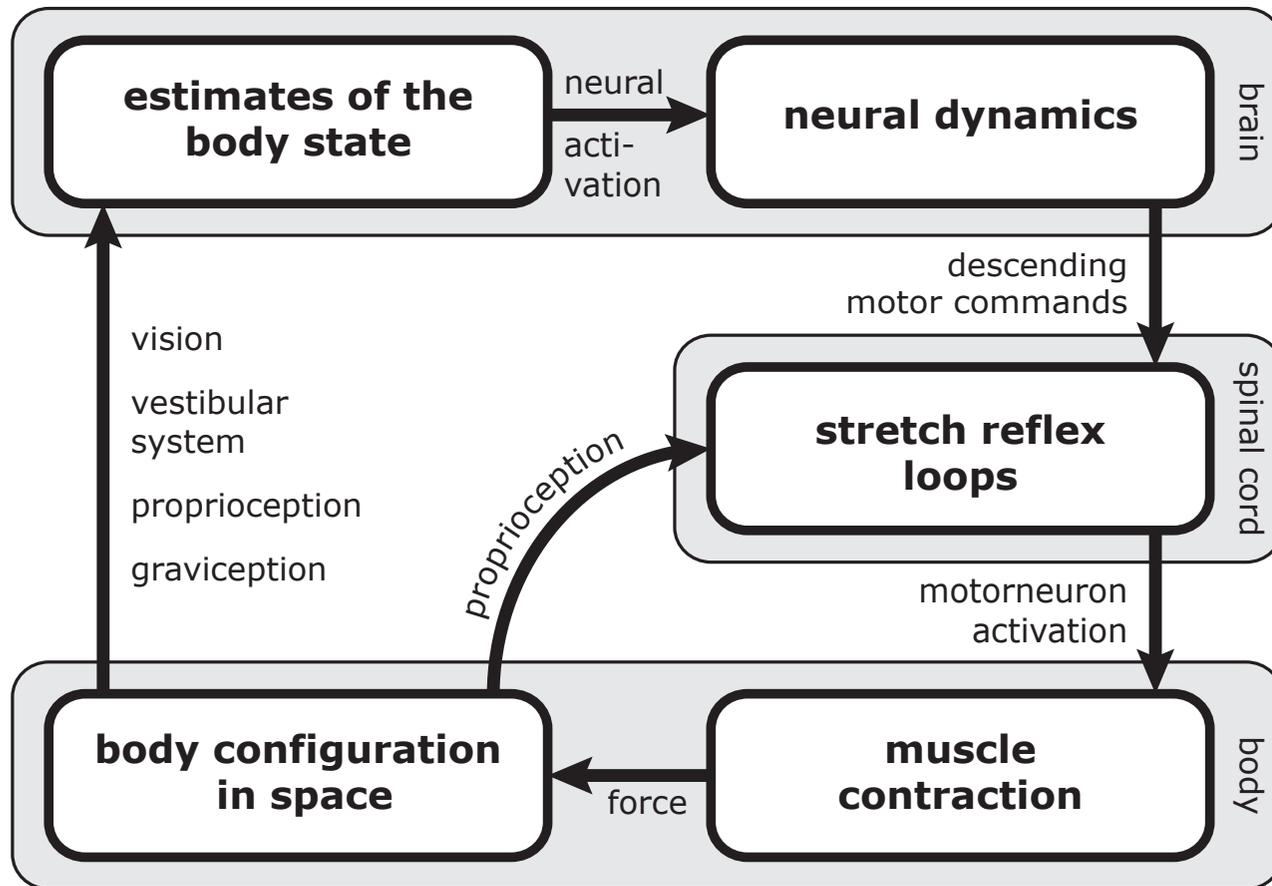
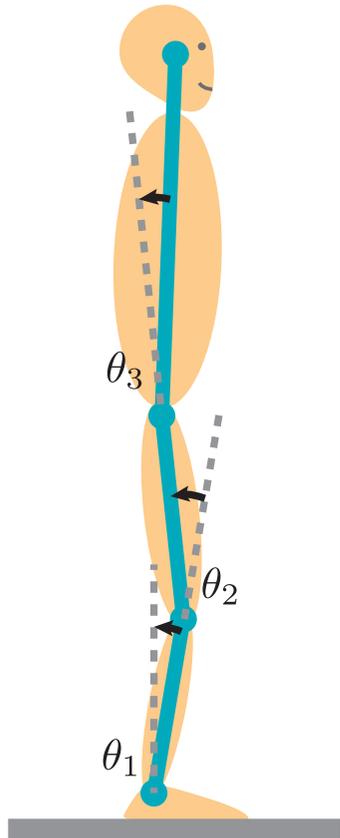


UCM synergy: accounts. Case study posture

■ but: find signature of UCM synergy



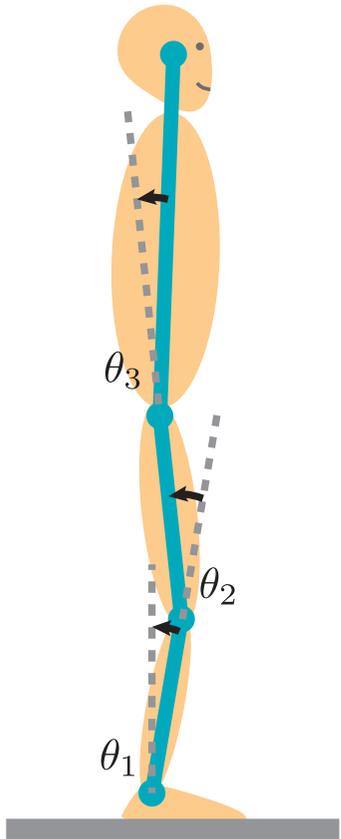
Multi-segment postural control model



PhD thesis Hendrik Reimann
Reiman, Scholz, Schöner (in preparation)

Multi-segment postural control model

■ bio-mechanical dynamics

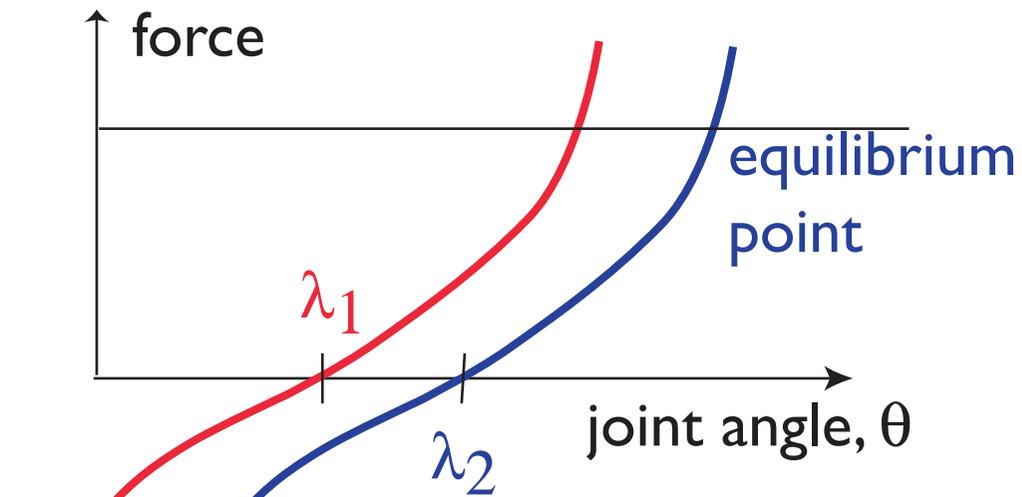
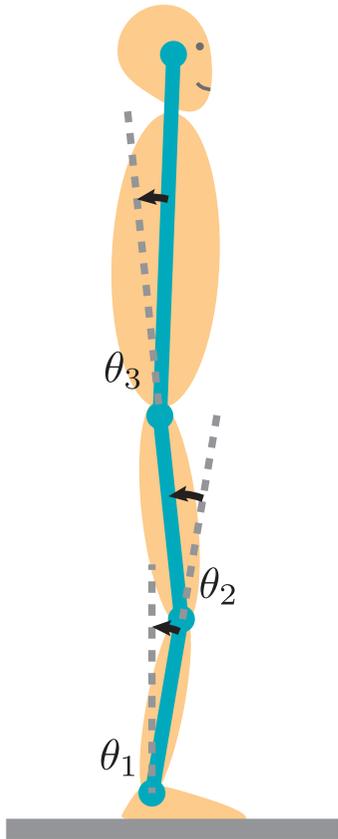


$$M(\theta)\ddot{\theta} + C(\theta, \dot{\theta})\dot{\theta} + N(\theta) = T$$

PhD thesis Hendrik Reimann
Reiman, Scholz, Schöner (in preparation)

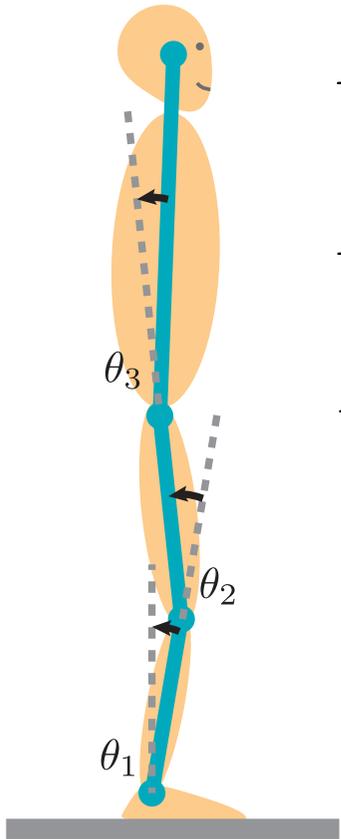
Multi-segment postural control model

■ muscle model



Multi-segment postural control model

■ muscle model



$$E_{AG} = e \left[\alpha_E \left(\hat{\theta} - \lambda + \rho + \mu(\hat{\dot{\theta}} - \dot{\lambda}) \right) \right]^+ - 1,$$

$$E_{AN} = e \left[-\alpha_E \left(\hat{\theta} - \lambda - \rho + \mu(\hat{\dot{\theta}} - \dot{\lambda}) \right) \right]^+ - 1.$$

$$E = (-E_{AG} + E_{AN}) \eta_m$$

$$\tilde{T}_{act} = AE$$

$$\tau_m^2 \ddot{T}_{act} + 2\tau_m \dot{T}_{act} + T_{act} = \tilde{T}_{act}$$

← muscle activation

← active muscle torque

Multi-segment postural control model

■ muscle model

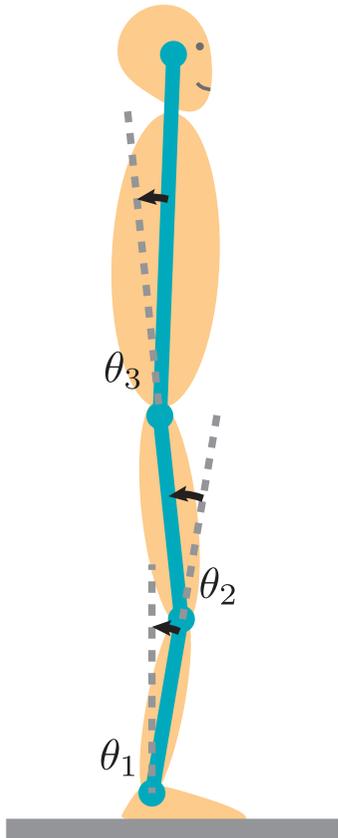
$$T_{\text{ela},j} = \exp(a_{j0} + \sum_{i=1}^3 a_{ji}\theta_i) - \exp(b_{j0} + \sum_{i=1}^3 b_{ji}\theta_i) + c_{ji}$$

$$T_{\text{vis}} = -B\dot{\theta}$$

← passive
torques

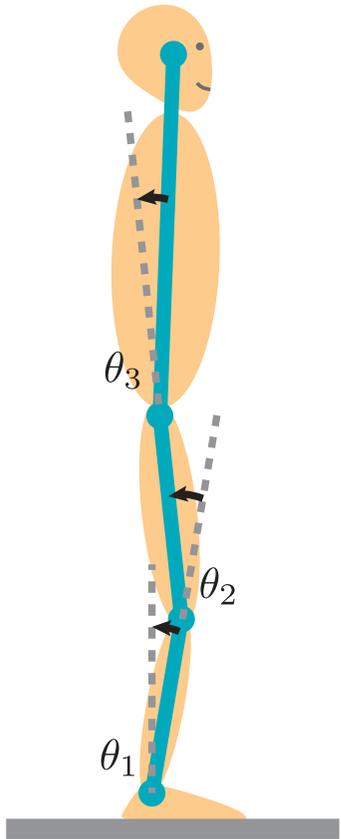
$$T = T_{\text{act}} + T_{\text{ela}} + T_{\text{vis}}$$

← total muscle
torque



Multi-segment postural control model

■ sensor model



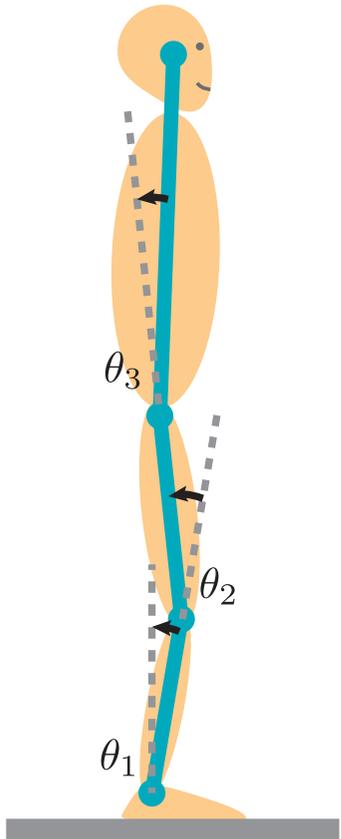
$$\hat{\dot{c}}(t) = \dot{c}(t - d_c) + \eta \dot{c},$$

$$\hat{\ddot{c}}(t) = \ddot{c}(t - d_c) + \eta \ddot{c},$$

← body in space

Multi-segment postural control model

■ control model



$$\dot{\lambda} = F_c = R^{-1} A^{-1} M J_c^+ \left(-\alpha_{\dot{c}} \hat{c} - \alpha_{\ddot{c}} \hat{\ddot{c}} \right)$$



active
stiffness



inertial
tensor

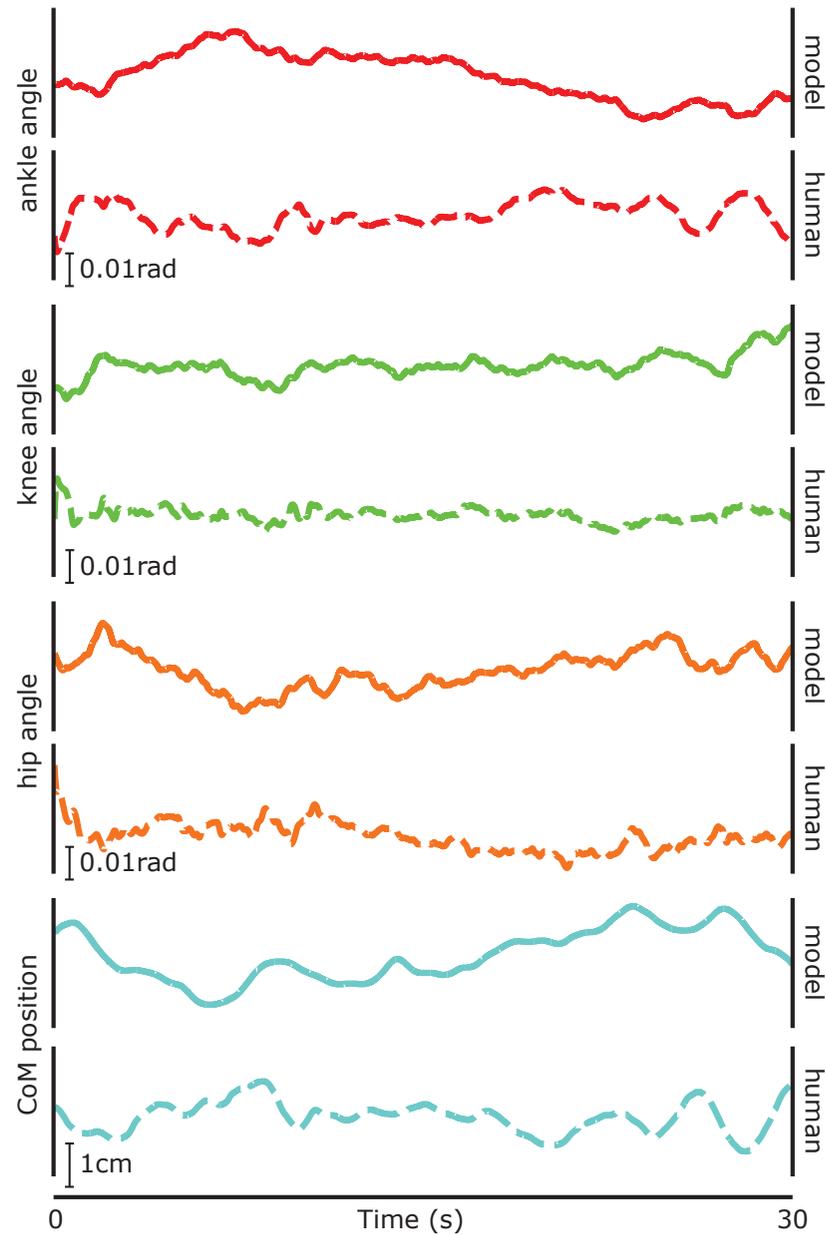


kinematic
pseudo-
inverse



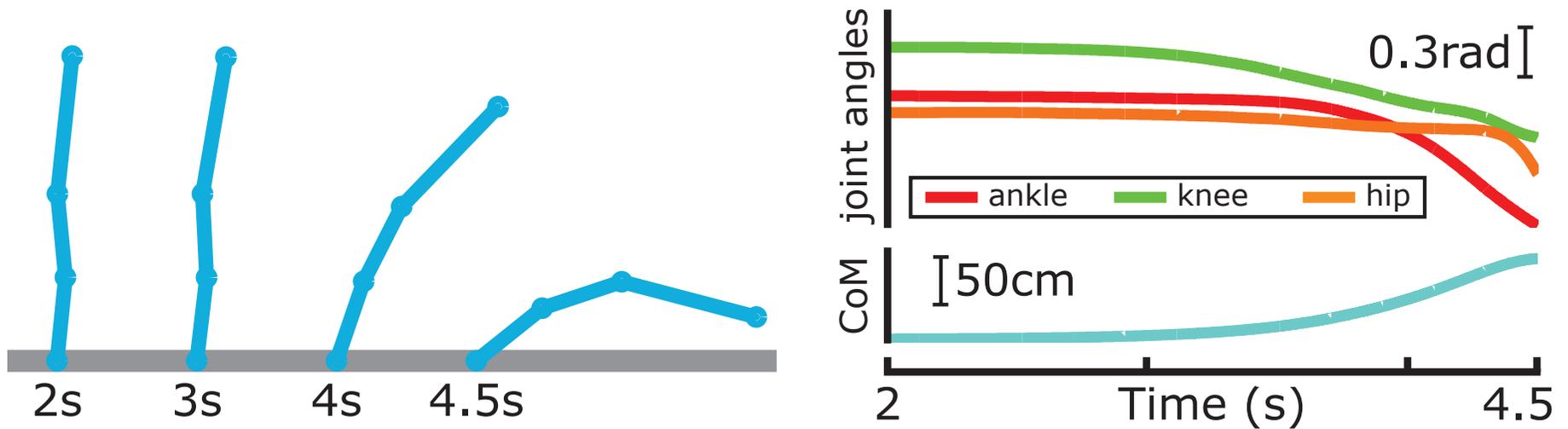
sensory
estimate
body in
space

Results: model stands



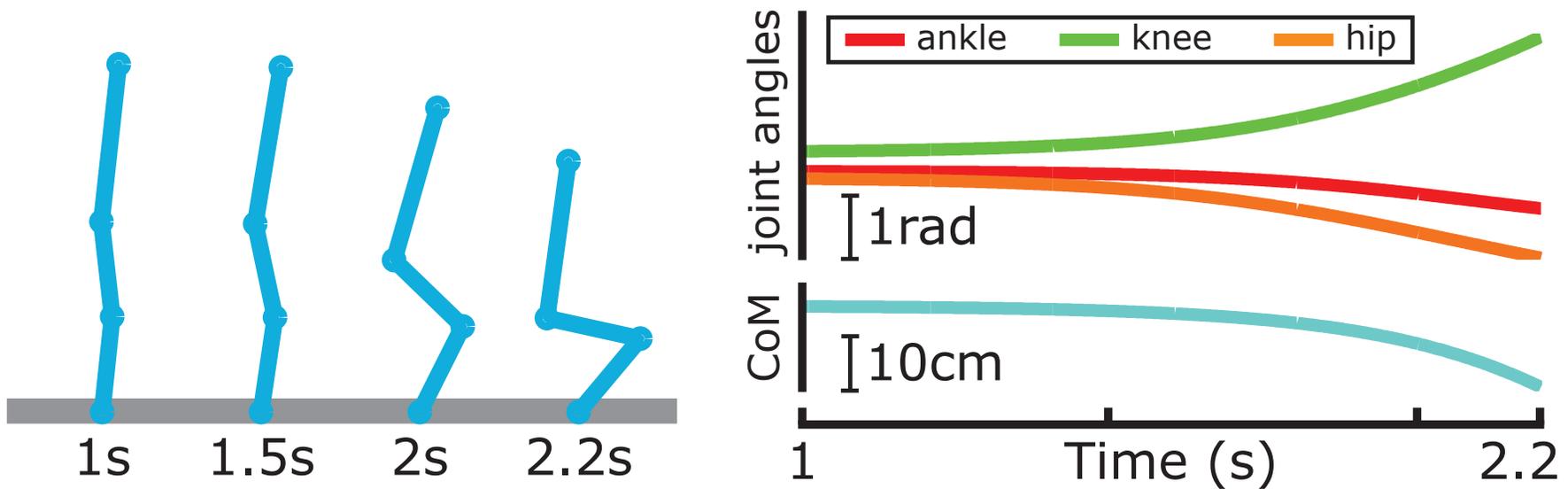
Results: model falls

- when the sensory feedback loop about the body in space is removed

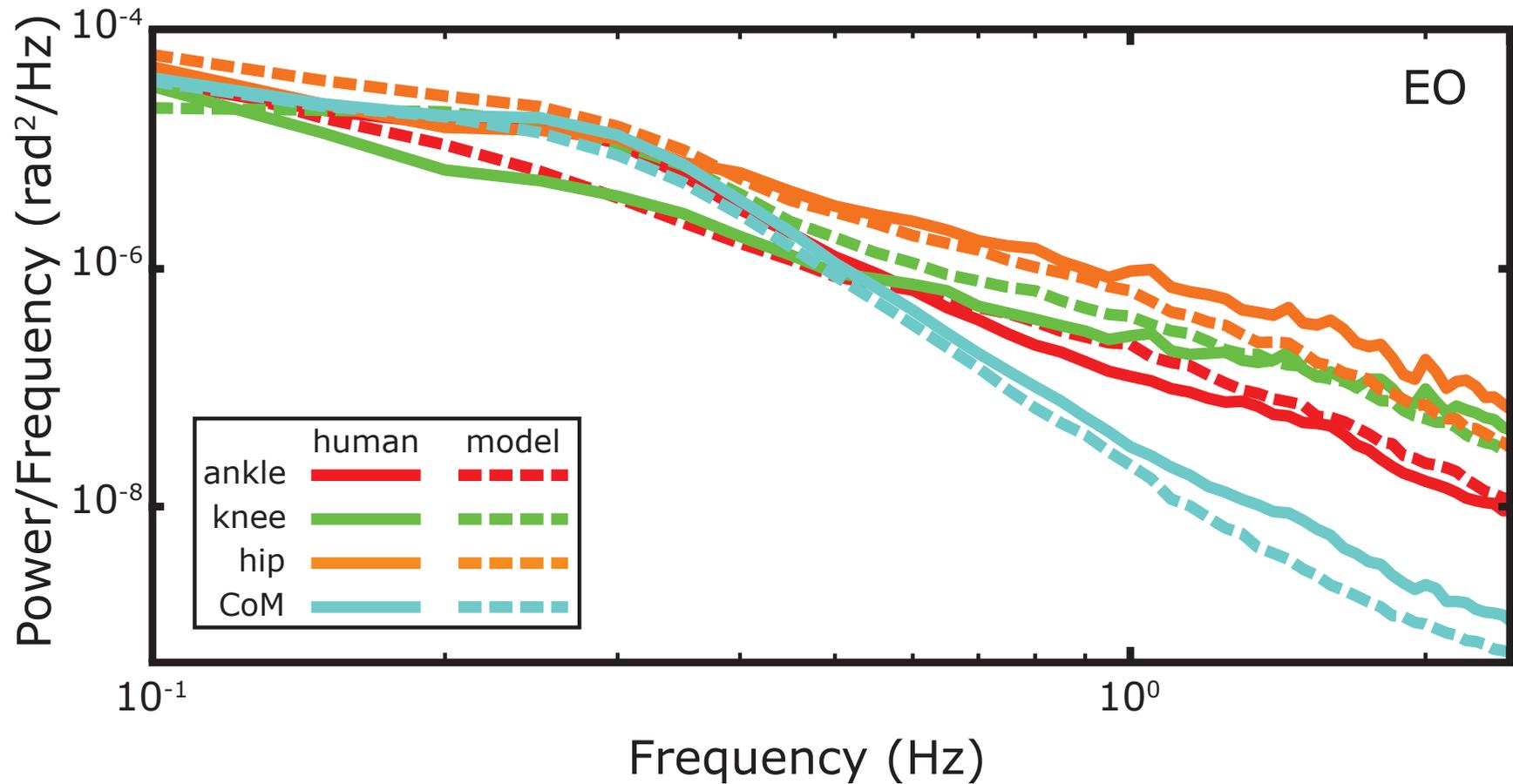


Results: model falls

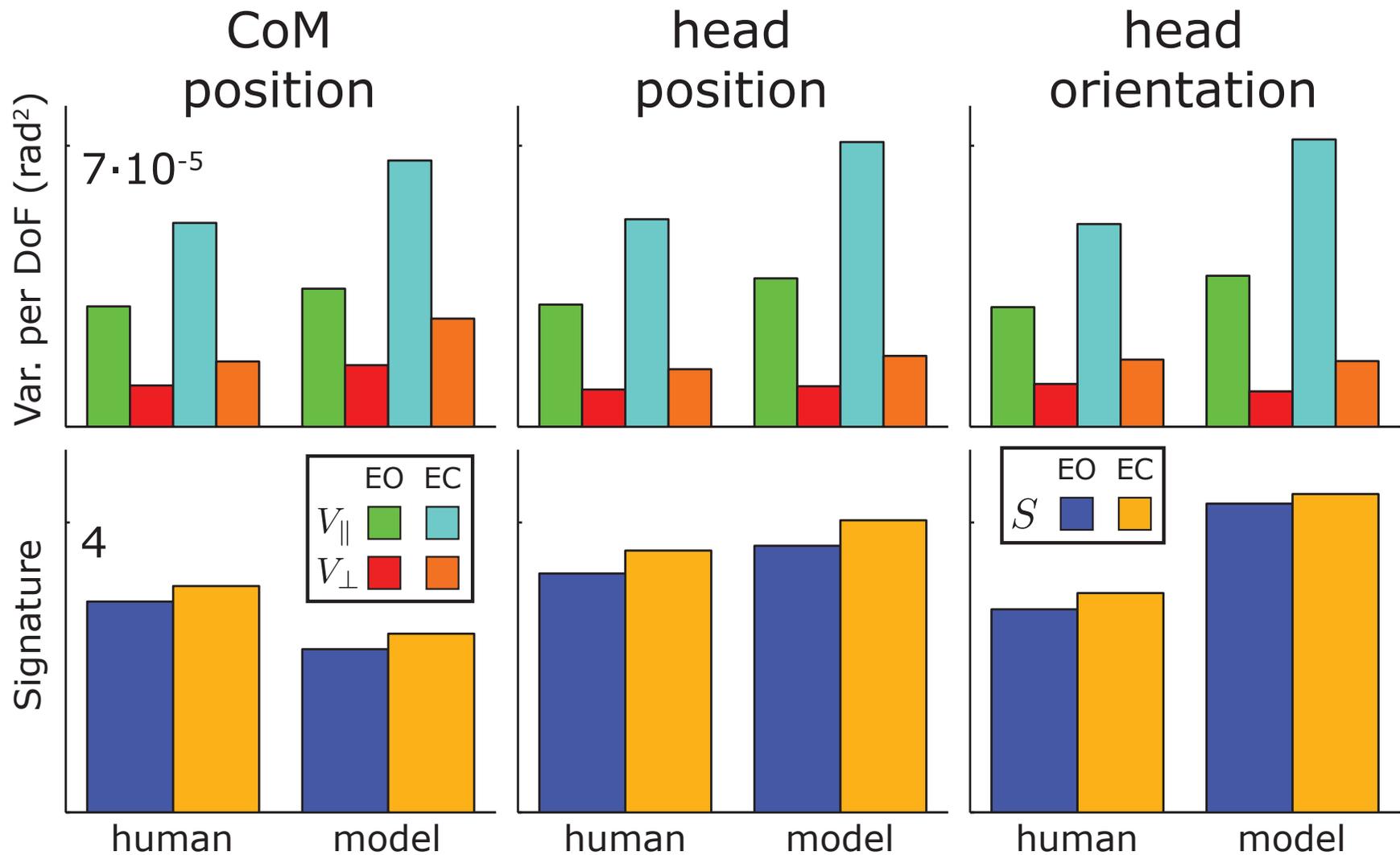
- when the spinal reflex loop within muscle model is removed (constant activation level of motor neurons)



Results: model predicts joint spectra



Results: model predicts UCM signature

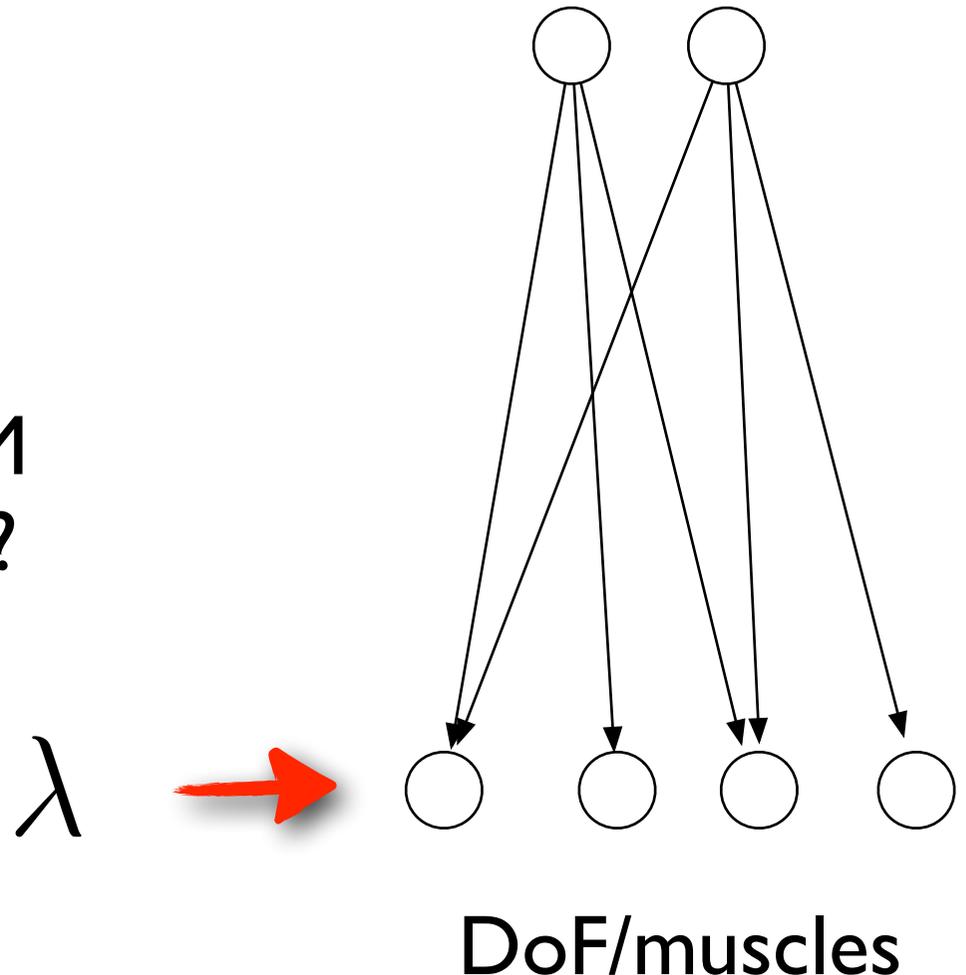


Why does this work?

$$\dot{\lambda} = F_c = R^{-1} A^{-1} M J_c^+ \left(-\alpha_{\dot{c}} \hat{c} - \alpha_{\ddot{c}} \hat{\ddot{c}} \right)$$

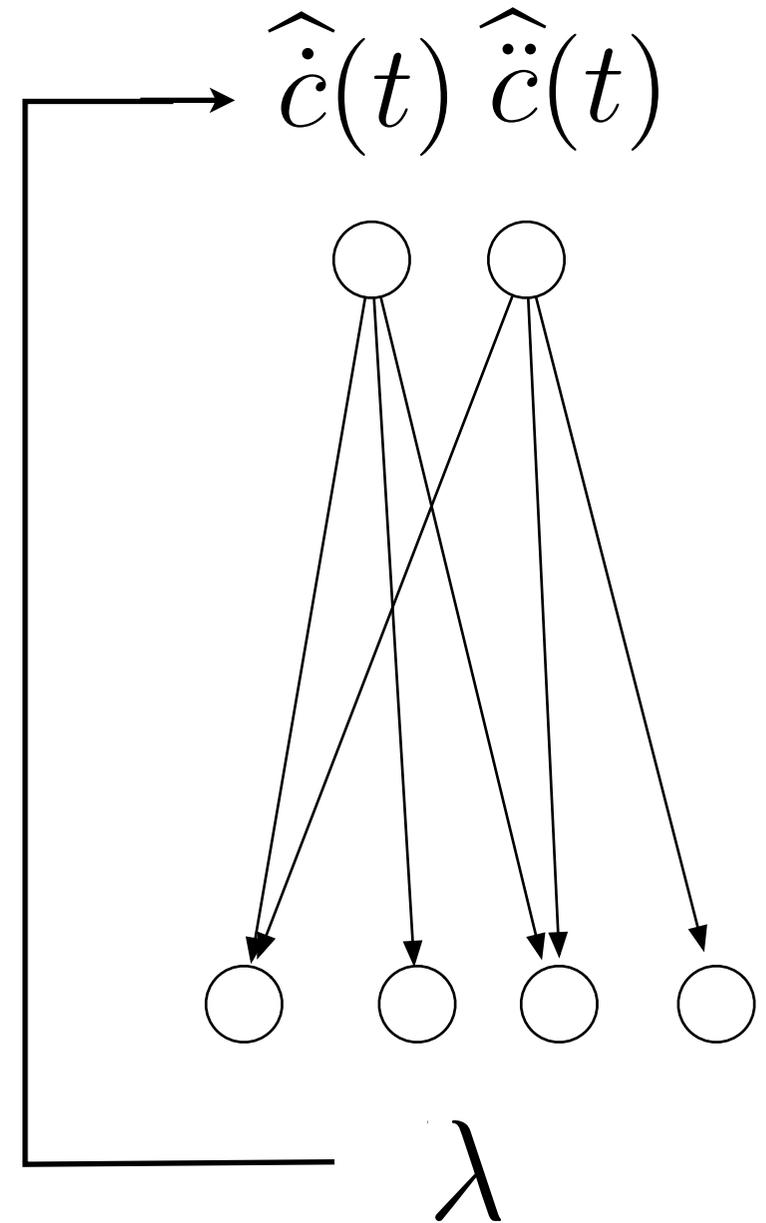
$\hat{c}(t) \hat{\ddot{c}}(t) \rightarrow$ motor commands

- model looks like a feed-forward neural network
- \Rightarrow should not have a UCM signature: classical synergy?



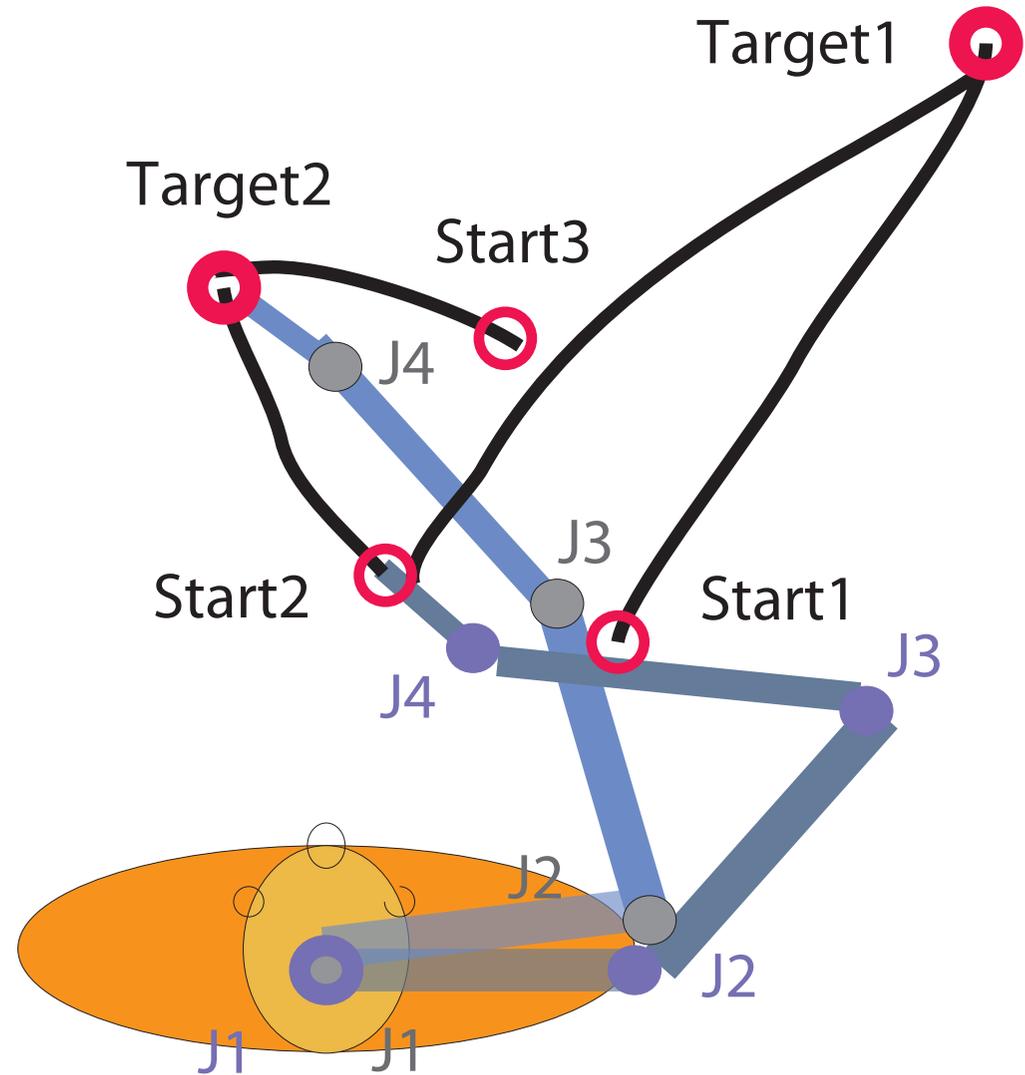
Why does this work?

- feedback loop through the world stabilizes configuration in ORT space
- DoF are effectively coupled through that loop to generate the compensatory signature



UCM synergy accounts: Case study: Reaching movements

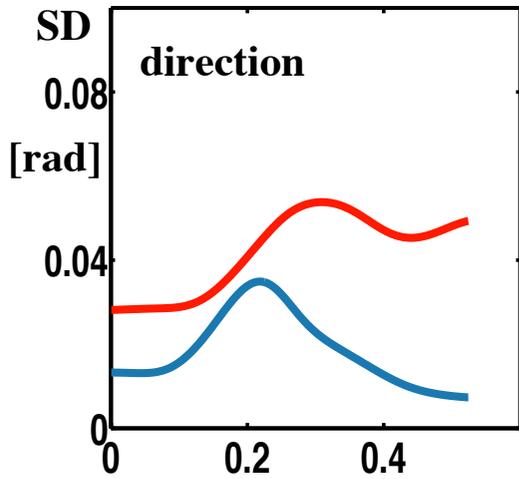
- Experiment from John Scholz's lab:
- reaching with 4DoF in 2D



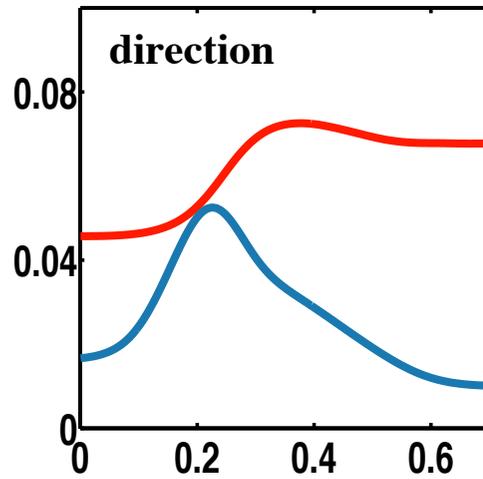
UCM structure of variance

Movement 1

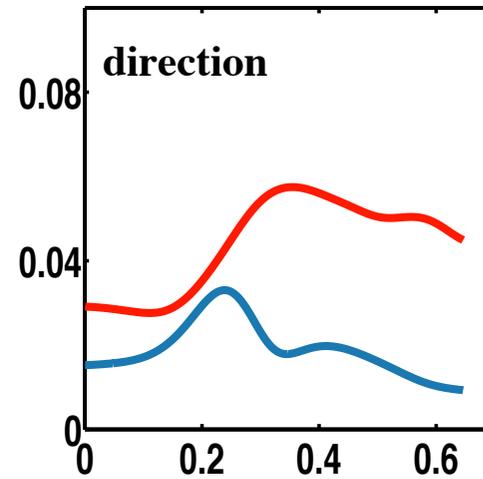
Experiment S1



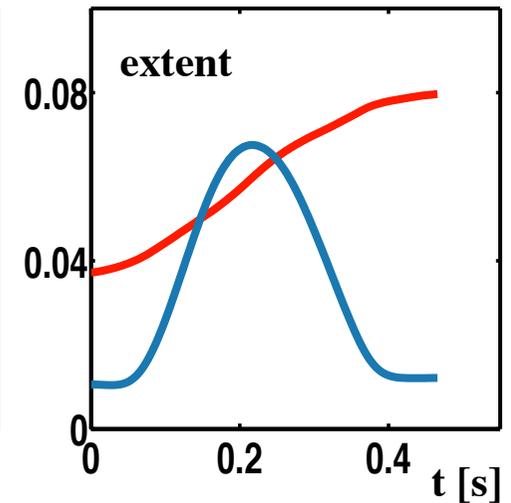
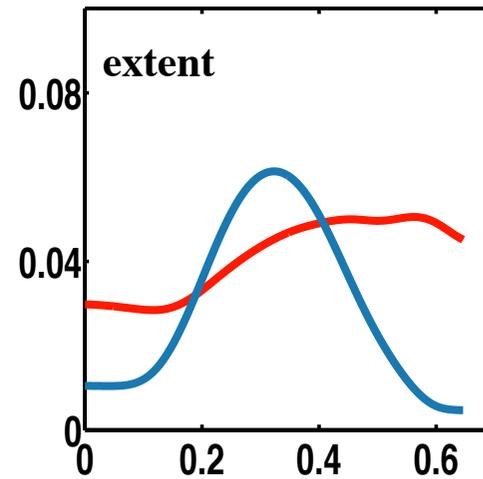
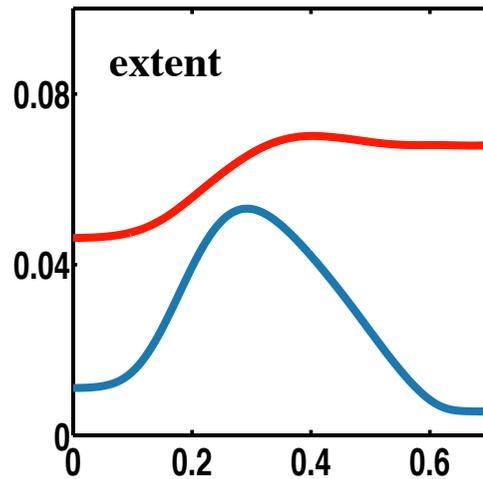
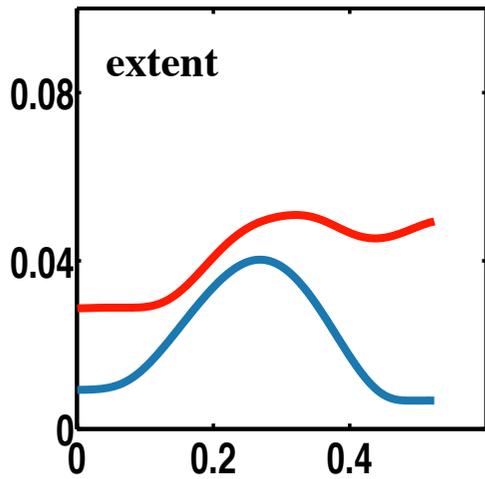
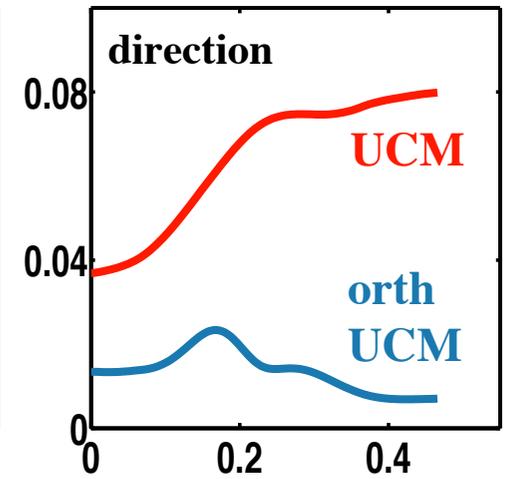
Experiment S2



Experiment S3

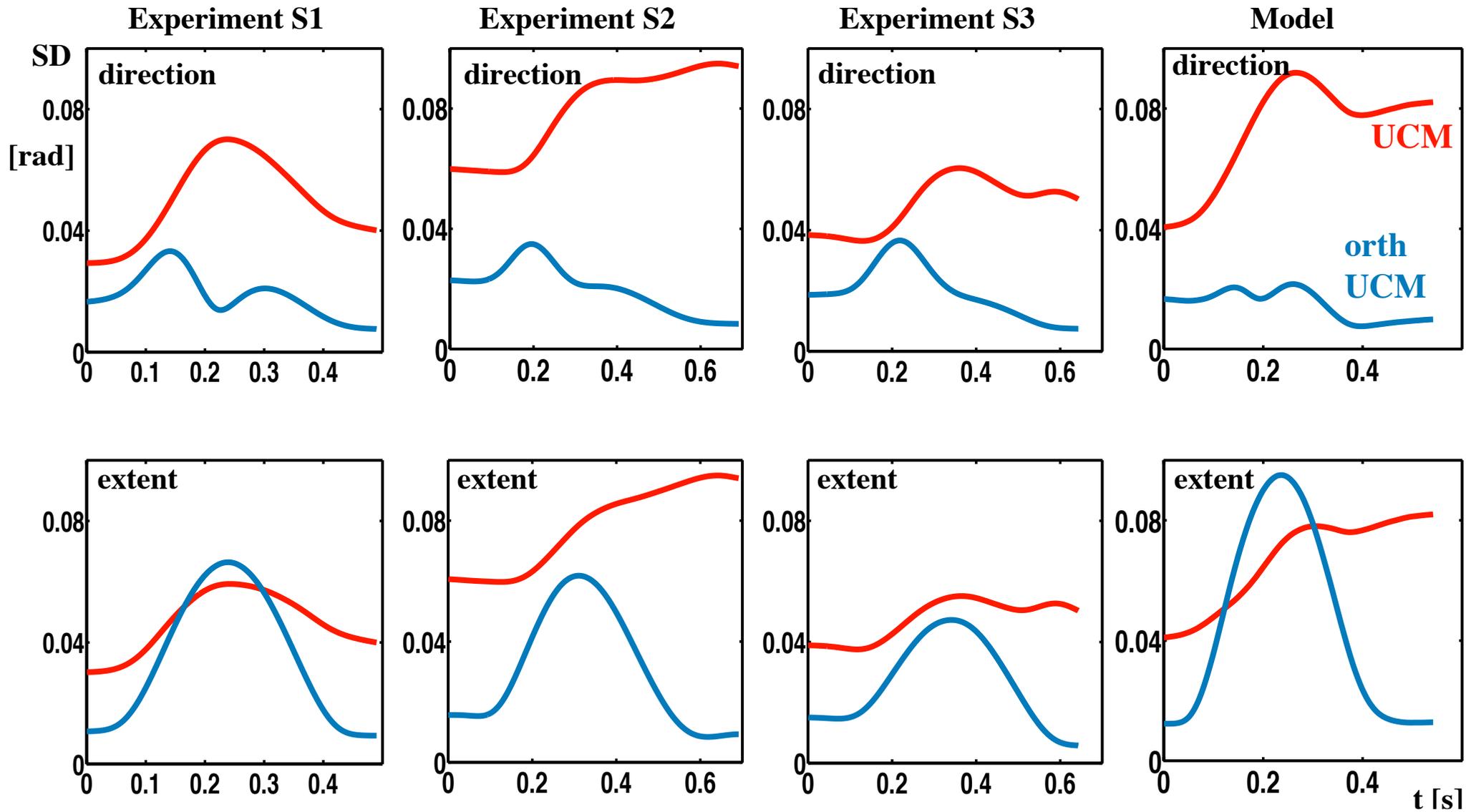


Model



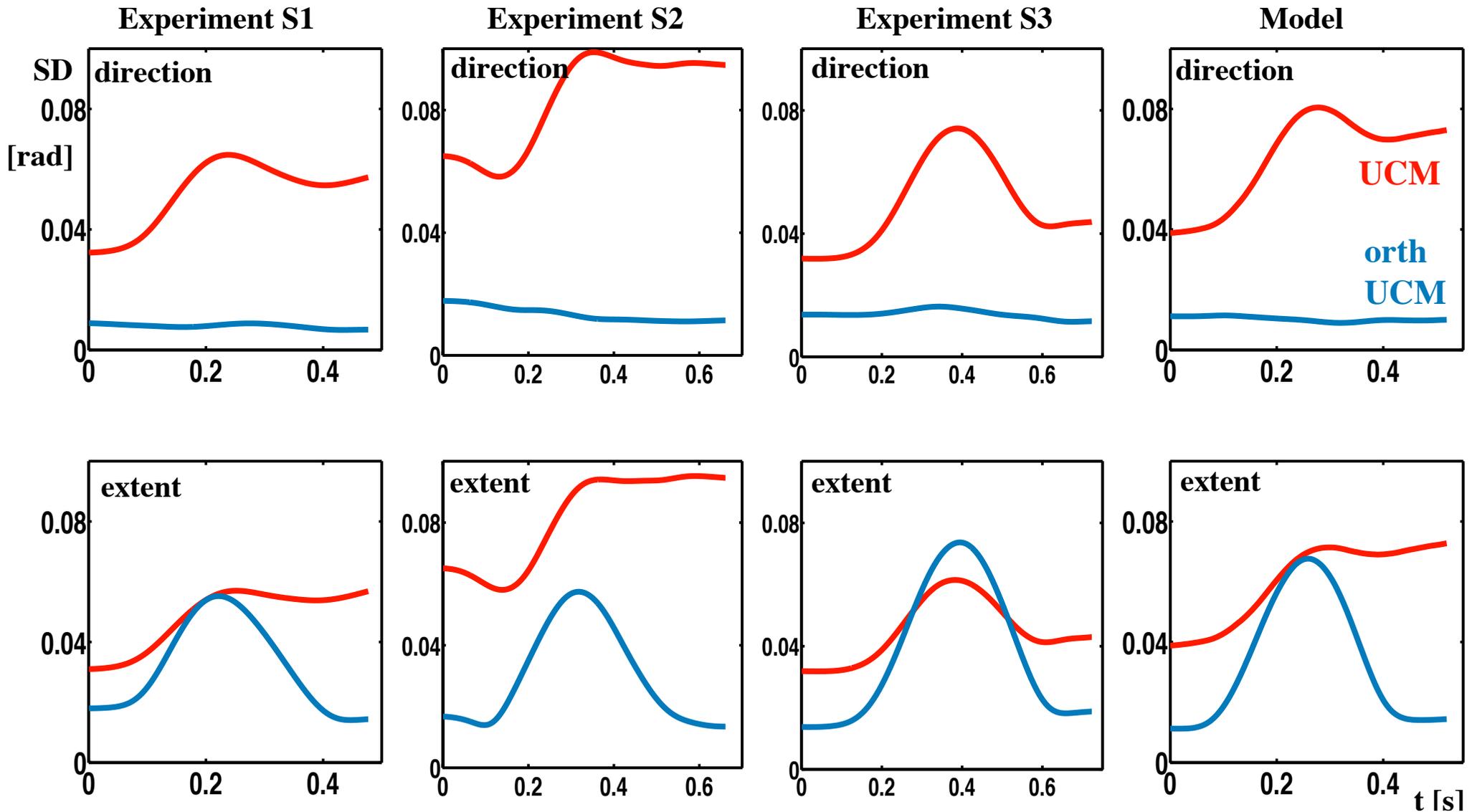
UCM structure of variance

Movement 3



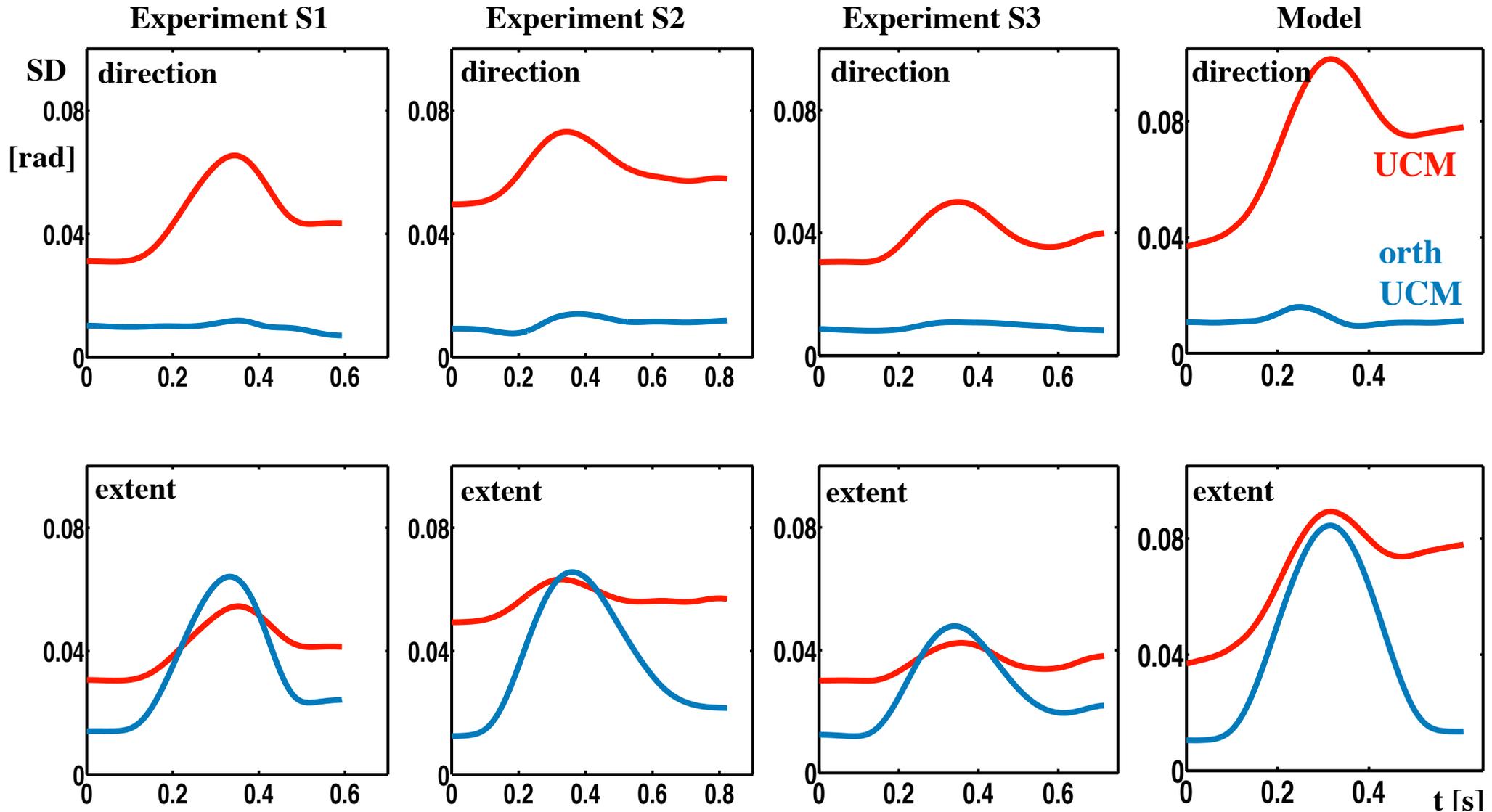
UCM structure of variance

Movement 4

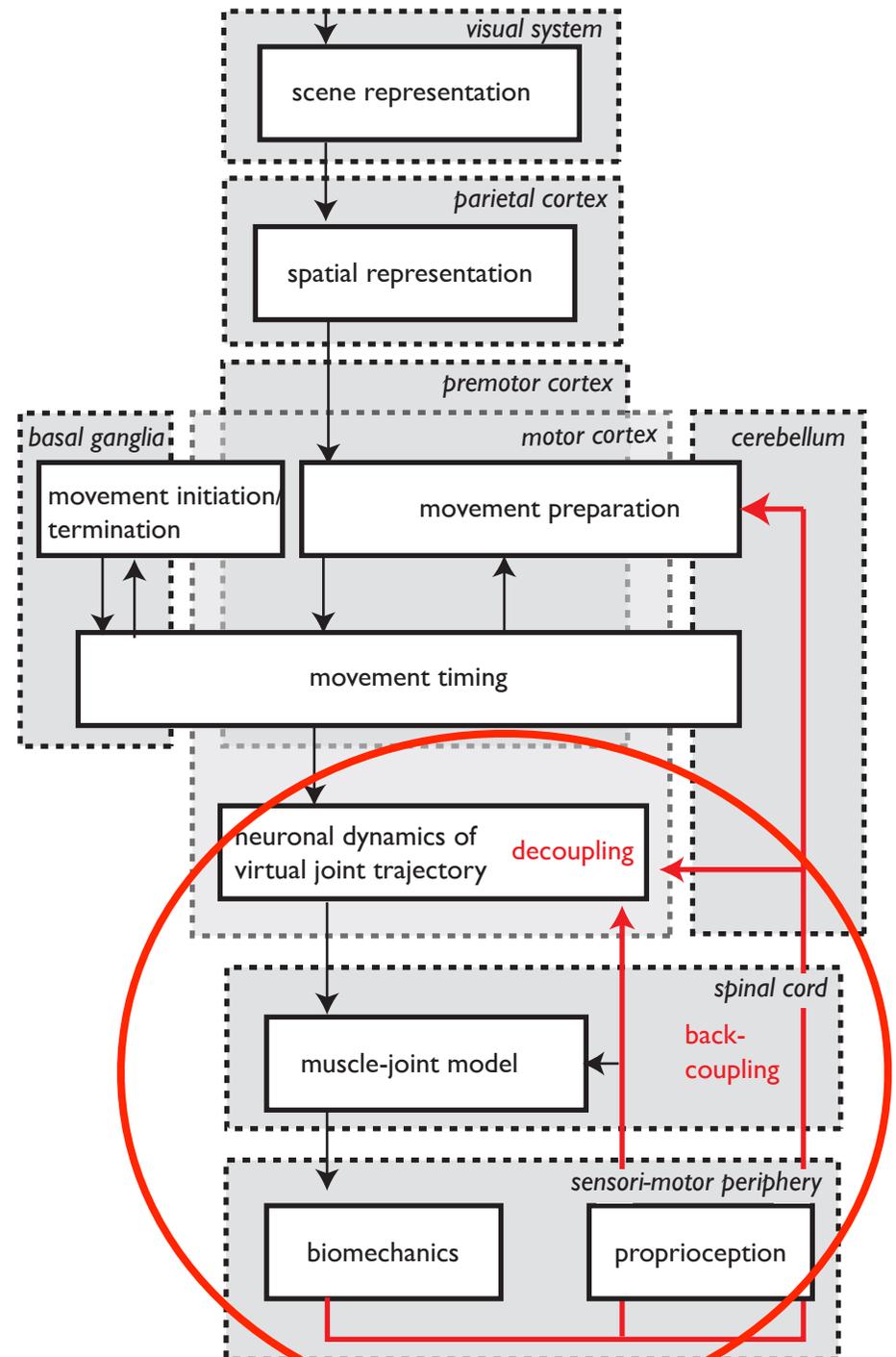


UCM structure of variance

Movement 6



Neural process model of 4DoF reaching



model

biomechanical dynamics

$$M(\boldsymbol{\theta}) \cdot \ddot{\boldsymbol{\theta}} + H(\boldsymbol{\theta}, \dot{\boldsymbol{\theta}}) = \mathbf{T}_m$$

muscle models

$$T_i = K_l \cdot \left((e^{[K_{nl} \cdot (\theta_i - \lambda_i^p)]^+} - 1) - (e^{-[K_{nl} \cdot (\theta_i - \lambda_i^m)]^-} - 1) \right) \\ + \mu_{bl} \cdot \text{asinh}(\dot{\theta}_i - \dot{\lambda}_i) + \mu_{rl} \cdot \dot{\theta}_i.$$

neural dynamics of lambda

$$\dot{\mathbf{v}} = -\beta_v(\mathbf{v} - \mathbf{u}(t)), \leftarrow \text{timing signal}$$

$$\mathbf{v}(t) = \mathbf{J}[\lambda(t)] \cdot \dot{\lambda}(t),$$

$$\ddot{\lambda} = (\mathbf{J}^+ \mathbf{E}) \cdot \begin{pmatrix} -\beta_v \mathbf{J} \cdot \dot{\lambda} + \beta_v \mathbf{u} - \cancel{\mathbf{J} \cdot \dot{\lambda}} \\ -\beta_{s1} \mathbf{E}^T \cdot (\lambda - \theta_d) - \beta_{s2} \mathbf{E}^T \cdot (\dot{\lambda} - \dot{\theta}_d) - \cancel{\mathbf{E}^T \cdot \dot{\lambda}} \end{pmatrix}$$

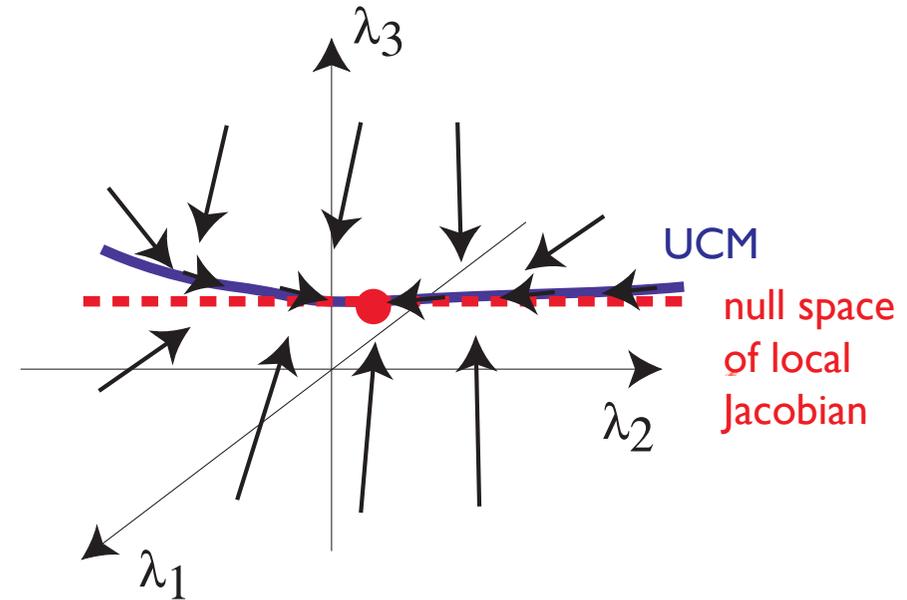
back-
coupling

approximation

timing signal



$$\ddot{\lambda} = (\mathbf{J}^+ \ \mathbf{E}) \cdot \begin{pmatrix} -\beta_v \mathbf{J} \cdot \dot{\lambda} + \beta_v \mathbf{u} \\ \mathbf{0} \end{pmatrix}$$



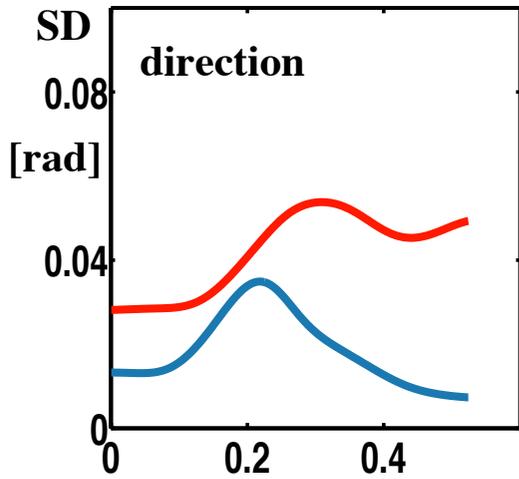
■ => control is stable in range space

■ => marginally stable in UCM/null space

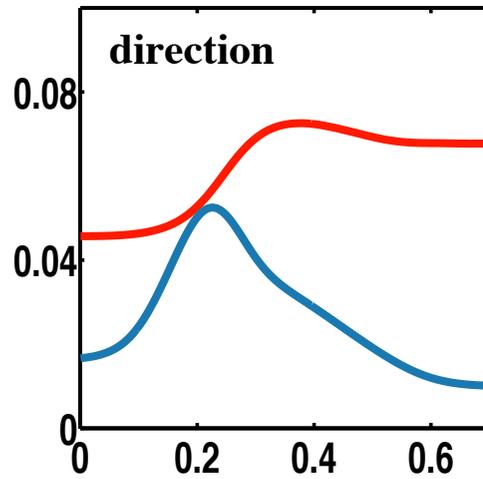
UCM structure of variance

Movement 1

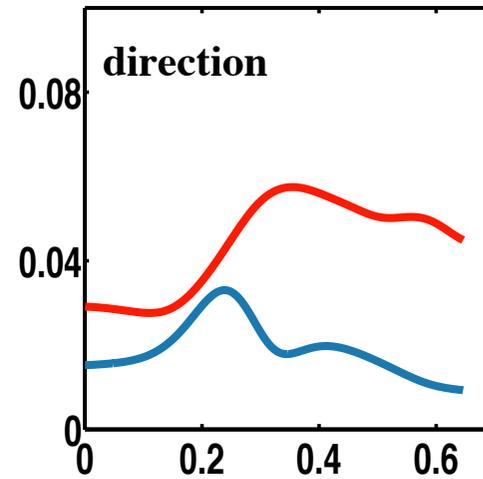
Experiment S1



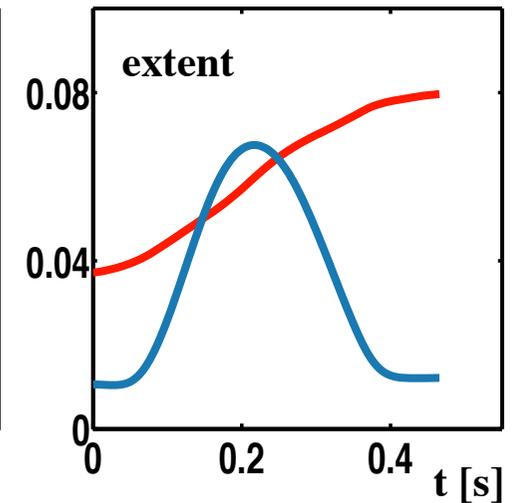
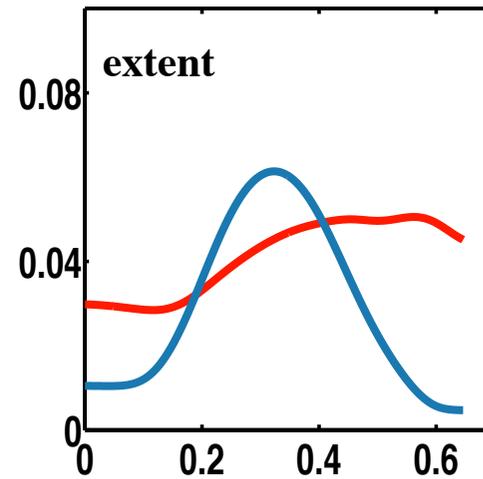
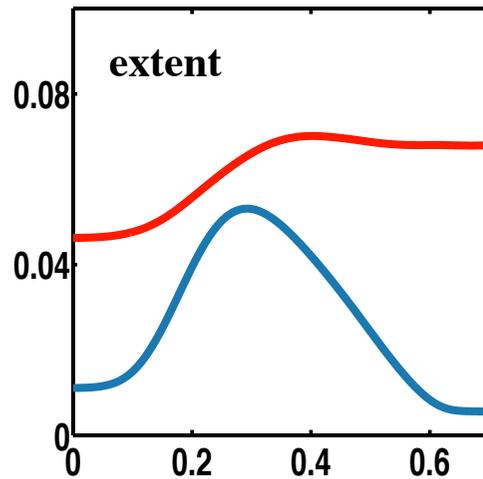
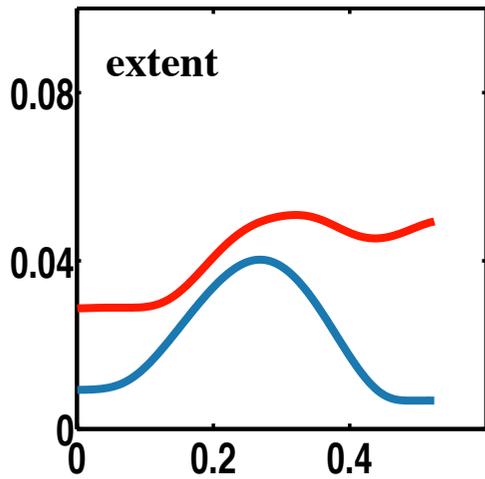
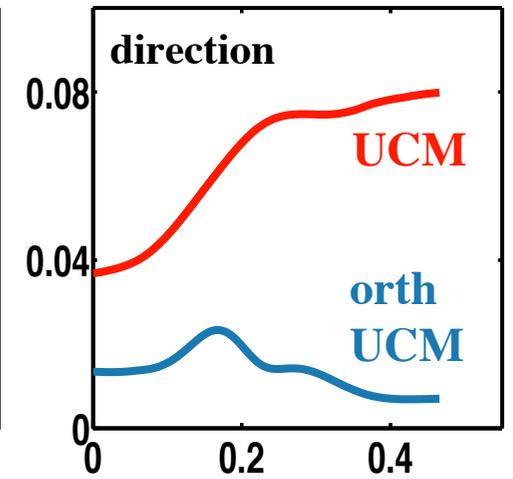
Experiment S2



Experiment S3

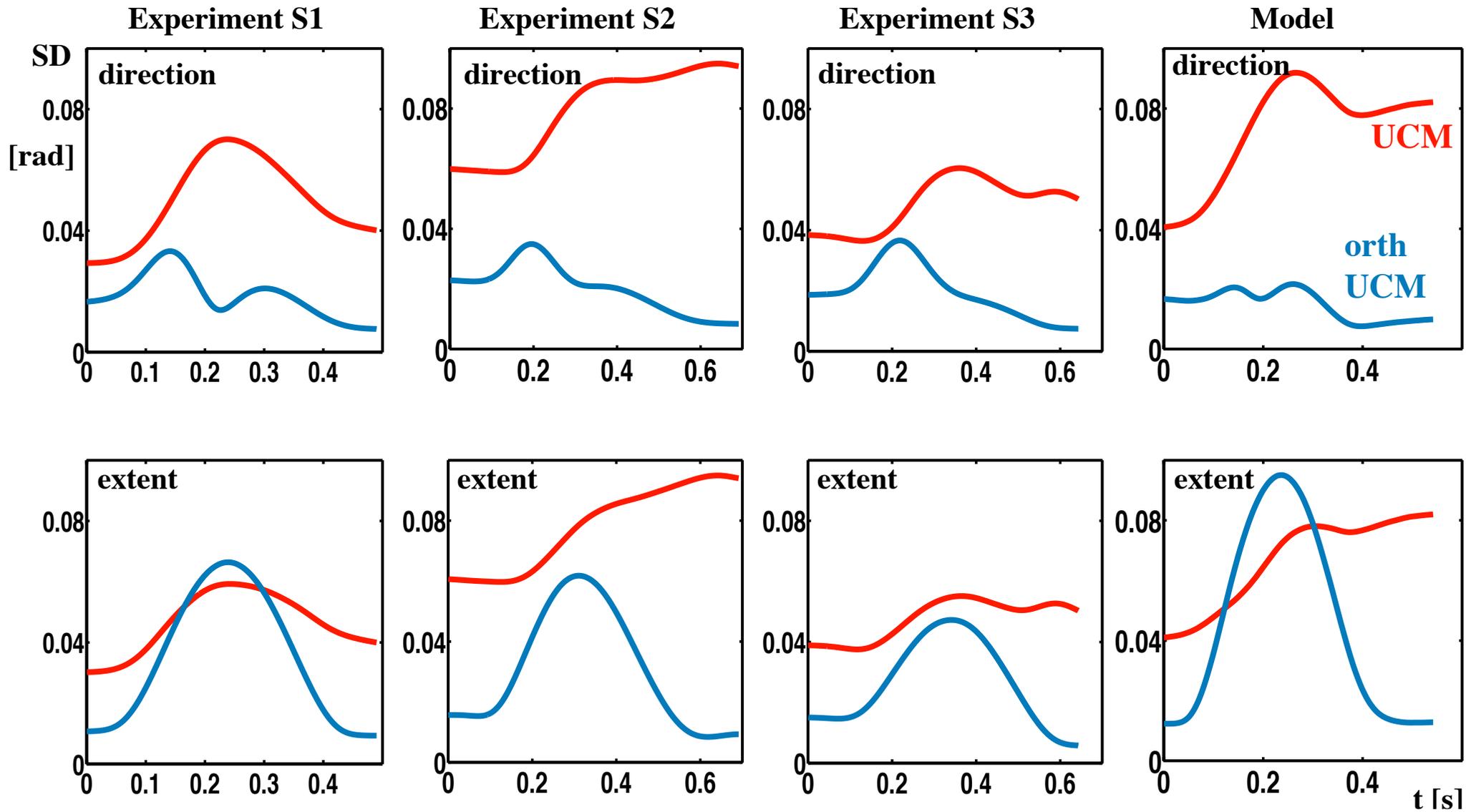


Model



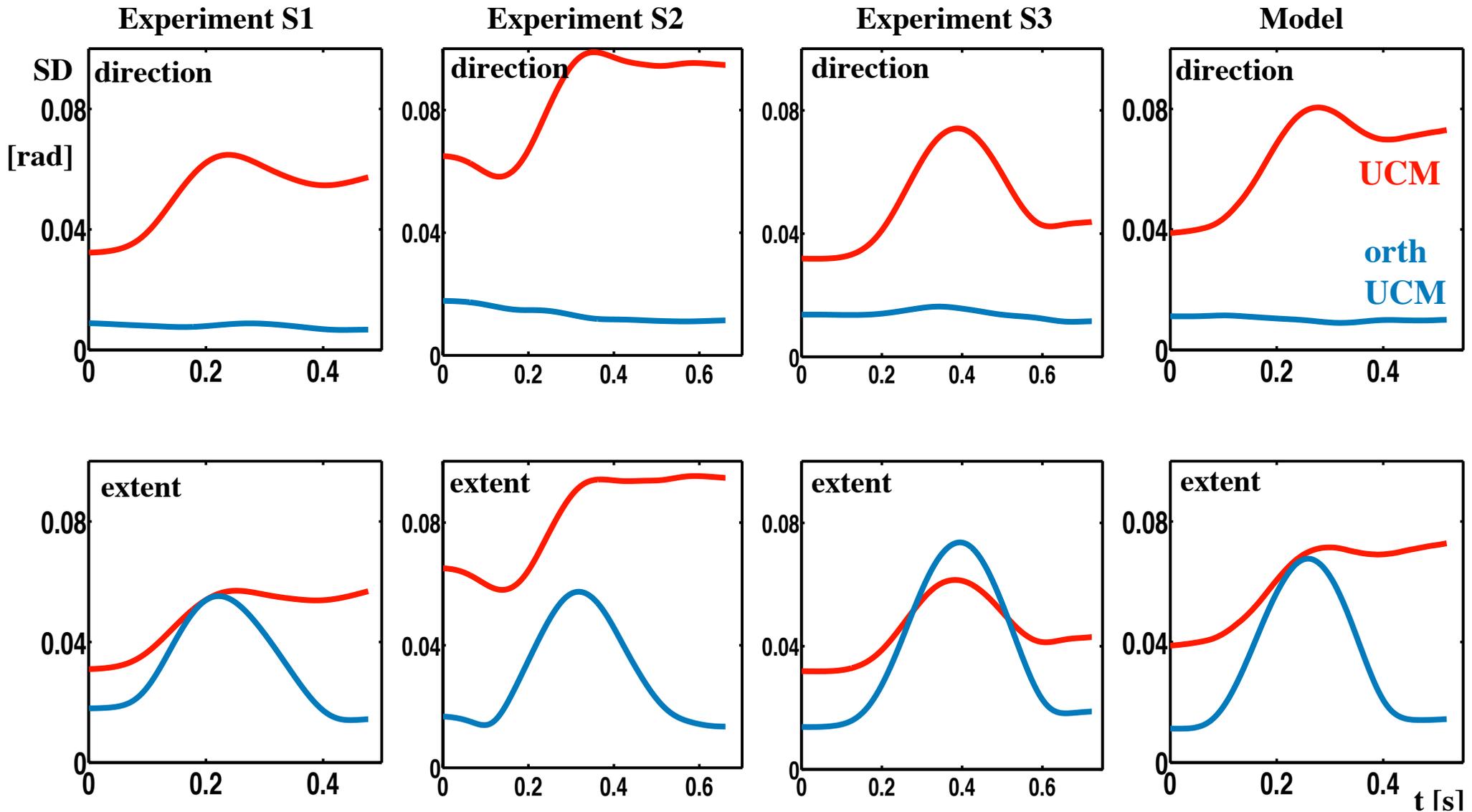
UCM structure of variance

Movement 3



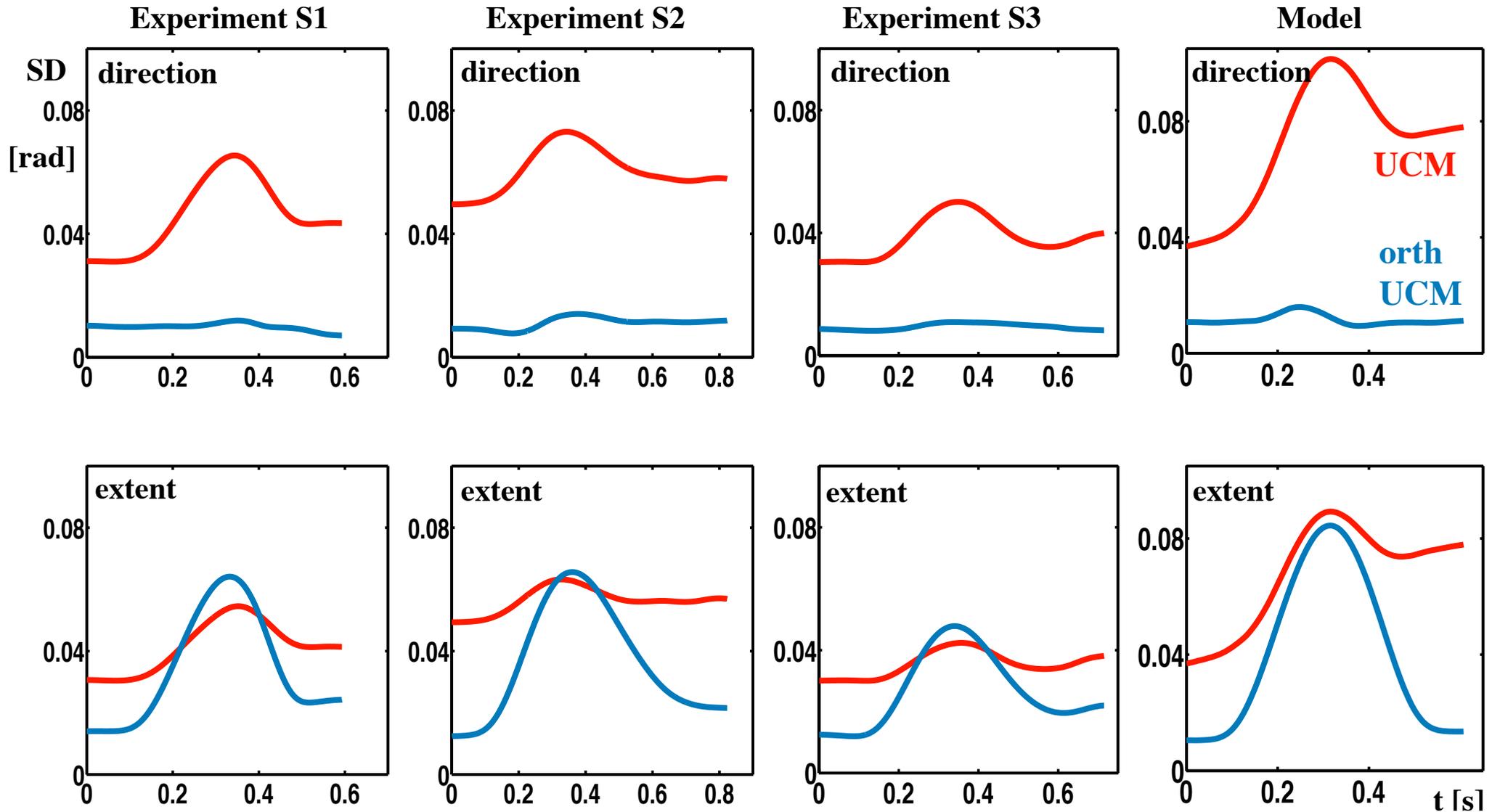
UCM structure of variance

Movement 4



UCM structure of variance

Movement 6



where does this come from?

start with pseudo-inverse of: $v = J\dot{\lambda}$

$$\dot{\lambda} = J^+ v$$

$$\ddot{\lambda} = J^+ \dot{v} \quad [+ J^+ v \approx 0]$$

a neuron, n , encoding rate of change of λ : $n = \dot{\lambda}$

$$\dot{n} = J^+ \dot{v} \quad \Leftarrow \text{insert timing signal} \quad \dot{v} = -v + u$$

$$\dot{n} = J^+ (-v + u) \quad \Leftarrow \text{insert } v = J\dot{\lambda}$$

$$\dot{n} = J^+ (-J\dot{\lambda} + u) \quad \Leftarrow \text{replace } n = \dot{\lambda}$$

$$\dot{n} = J^+ (-Jn + u)$$

$$\dot{n} = -J^+ Jn + J^+ u$$

where does this come from?

$$\dot{n} = -J^+ J n + J^+ u$$

$$\dot{n} = -n + n - J^+ J n + J^+ u$$

$$\dot{n} = -n + (1 - J^+ J)n + J^+ u$$



projection
onto null-
space



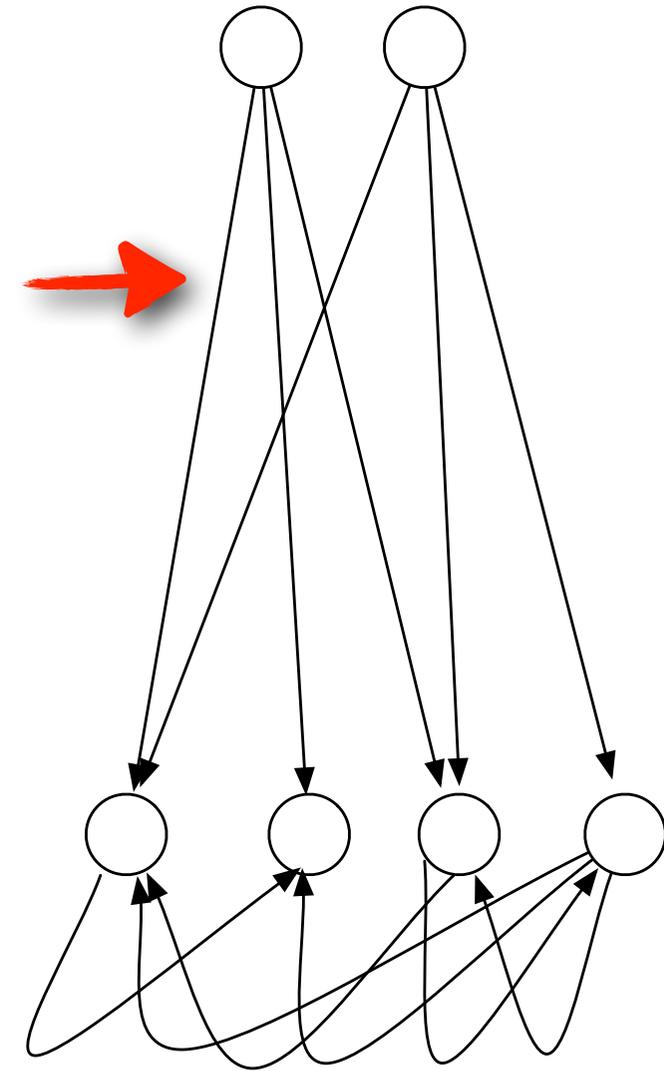
feed-
forward
from timing
command

where does this come from?

feed-
forward
from timing
command

$$\dot{n} = -n + (1 - J^+ J)n + J^+ u$$

projection
onto null-
space



how does this do the UCM effect?

projection
onto null-
space



feed-forward
from timing
command

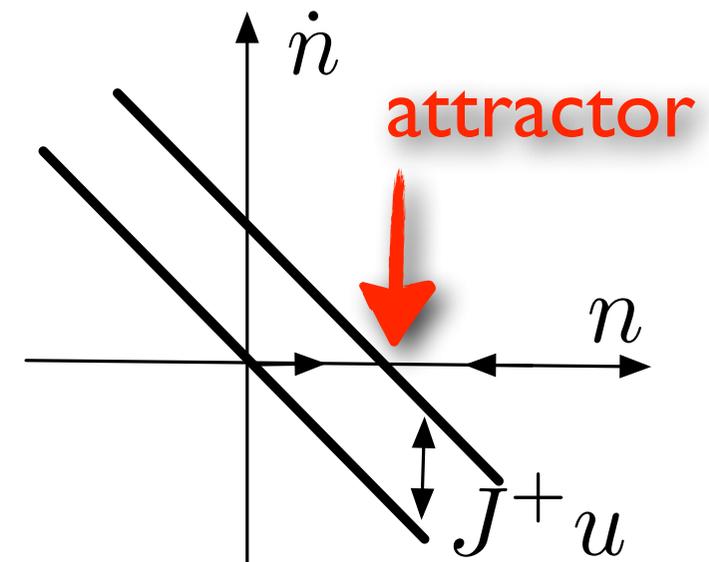


$$\dot{n} = -n + (1 - J^+ J)n + J^+ u$$

within the range-space

$$\dot{n} = -n + J^+ u$$

=> stability within the range-space



how does this do the UCM effect?

projection
onto null-
space



feed-forward
from timing
command



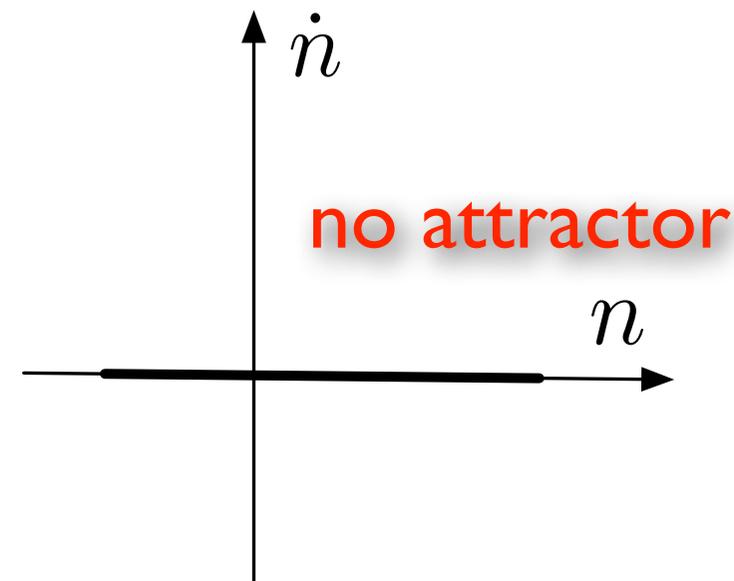
$$\dot{n} = -n + (1 - J^+ J)n + J^+ u$$

within the null-space

$$\dot{n} = -n + n + 0$$

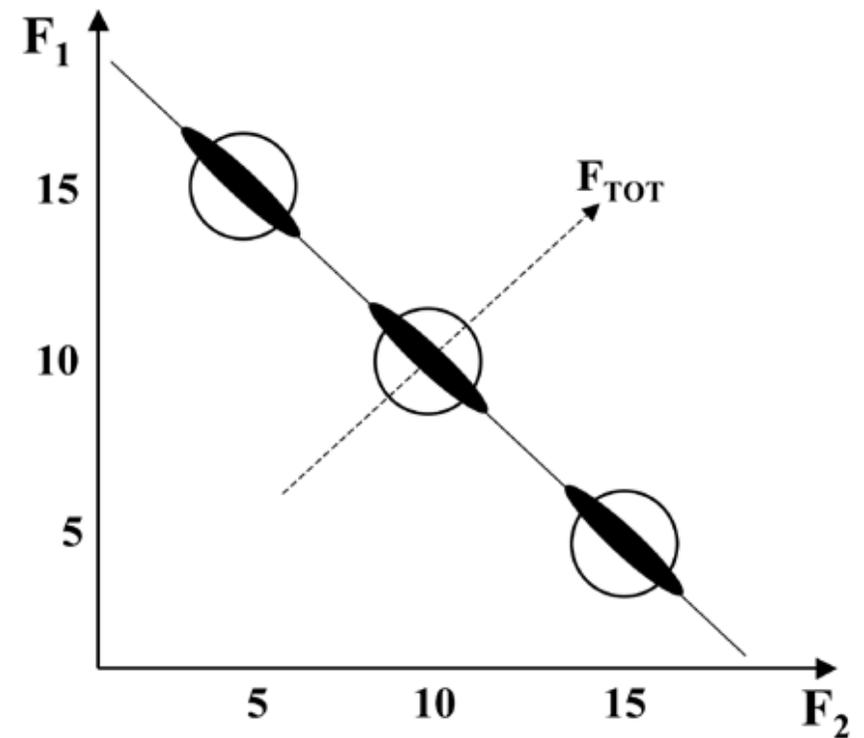
$$\dot{n} = 0$$

=> no stability within the null-space



UCM synergy accounts: case study finger movements

- Mark Latash et al: press with two fingers to produce fixed total force



model

task variable F

$$F = F_1 + F_2$$

Jacobian

$$J = (1 \ 1)$$

Pseudo-inverse

$$J^+ = \begin{pmatrix} 1/2 \\ 1/2 \end{pmatrix}$$

projection onto null space

$$1 - J^+ J = \begin{pmatrix} 1/2 & -1/2 \\ -1/2 & 1/2 \end{pmatrix}$$

model

two neurons to represent forces

$$n = \begin{pmatrix} F1 \\ F2 \end{pmatrix}$$

$$J^+ = \begin{pmatrix} 1/2 \\ 1/2 \end{pmatrix}$$


dynamics

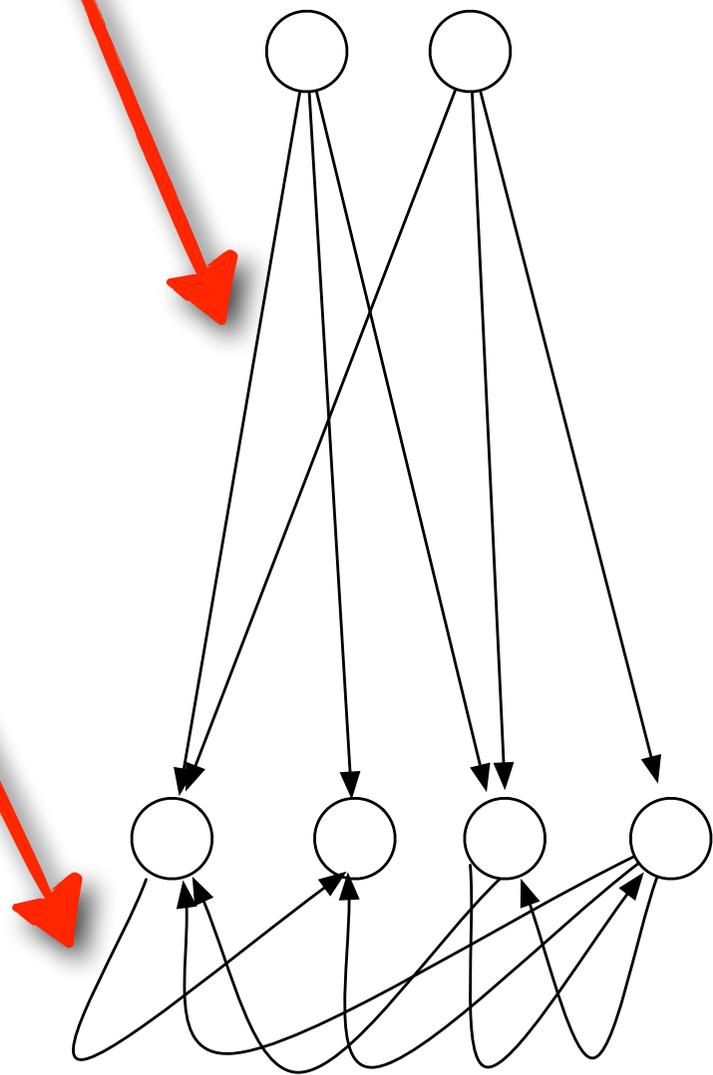
$$\dot{n} = -n + (1 - J^+ J)n + J^+ u$$


$$1 - J^+ J = \begin{pmatrix} 1/2 & -1/2 \\ -1/2 & 1/2 \end{pmatrix}$$

leads to

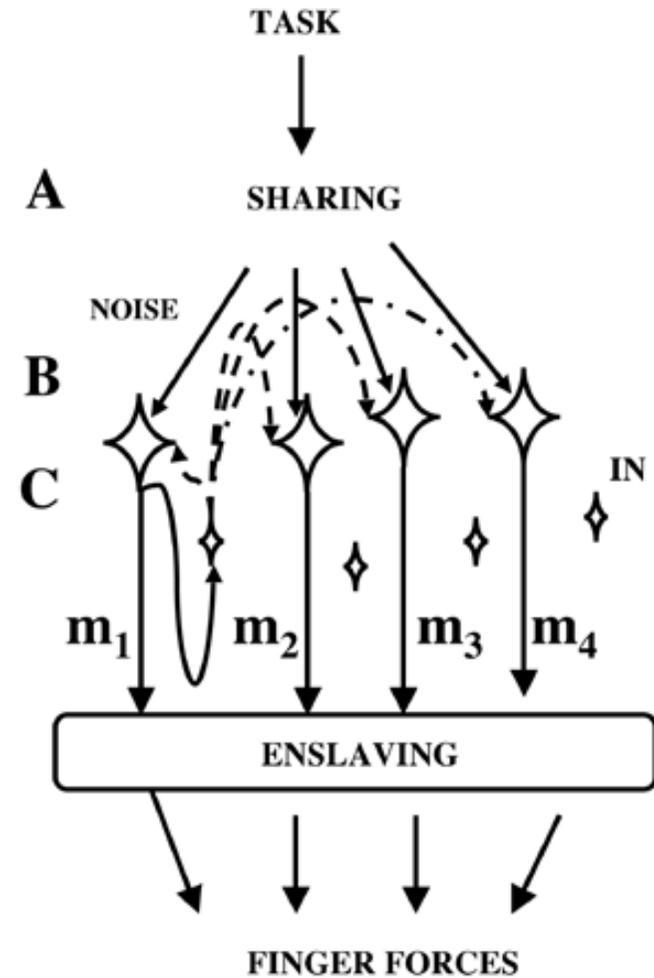
$$\dot{n} = - \begin{pmatrix} n_1 \\ n_2 \end{pmatrix} + \begin{pmatrix} n_1/2 - n_2/2 \\ n_2/2 - n_1/2 \end{pmatrix} + \begin{pmatrix} u/2 \\ u/2 \end{pmatrix}$$

$$\dot{n} = - \begin{pmatrix} n_1 \\ n_2 \end{pmatrix} + \begin{pmatrix} n_1/2 - n_2/2 \\ n_2/2 - n_1/2 \end{pmatrix} + \begin{pmatrix} u/2 \\ u/2 \end{pmatrix}$$



compare to Latash et al 2005

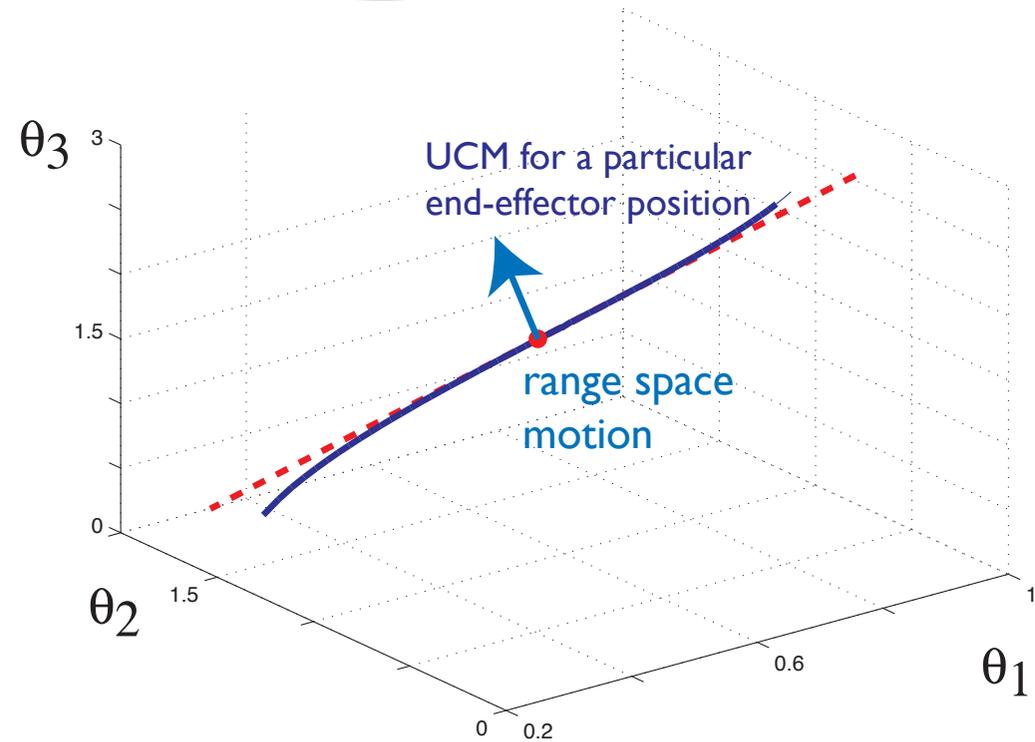
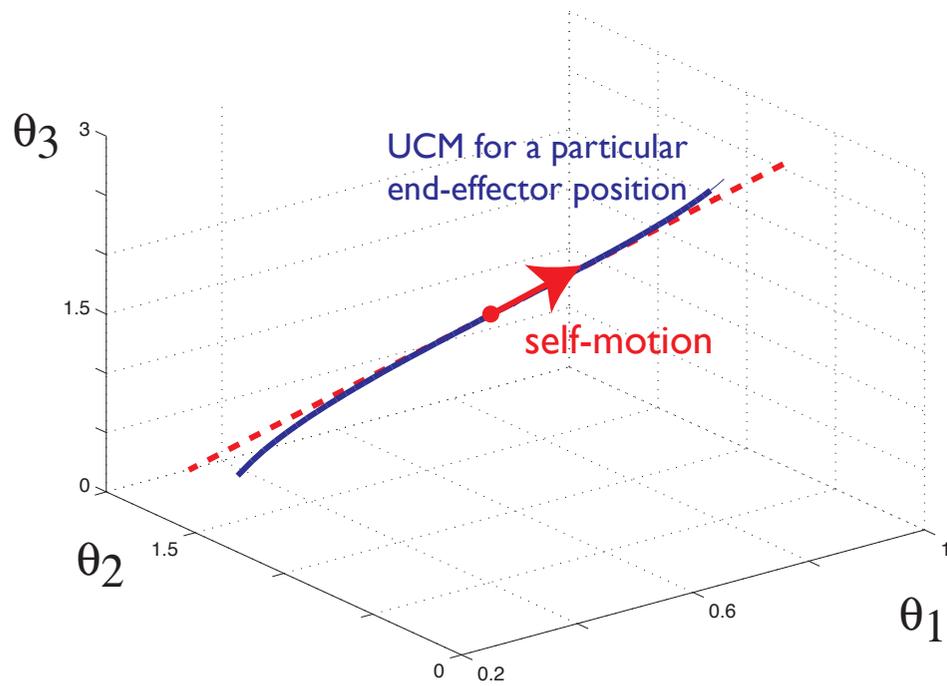
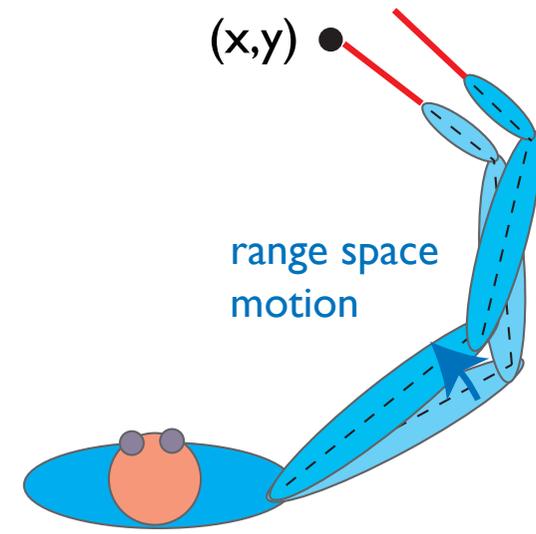
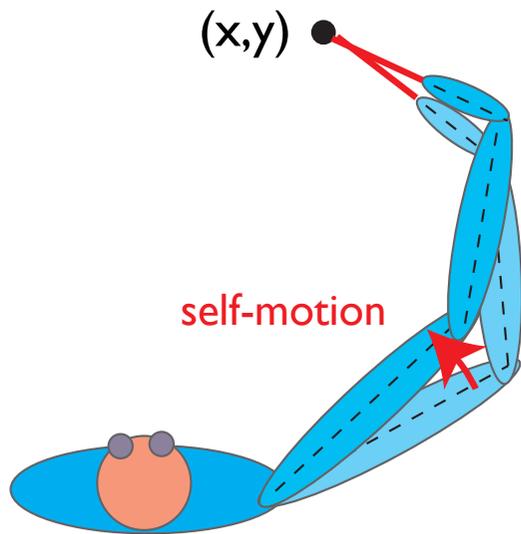
- candidate for recurrent inhibitory interaction: Renshaw system



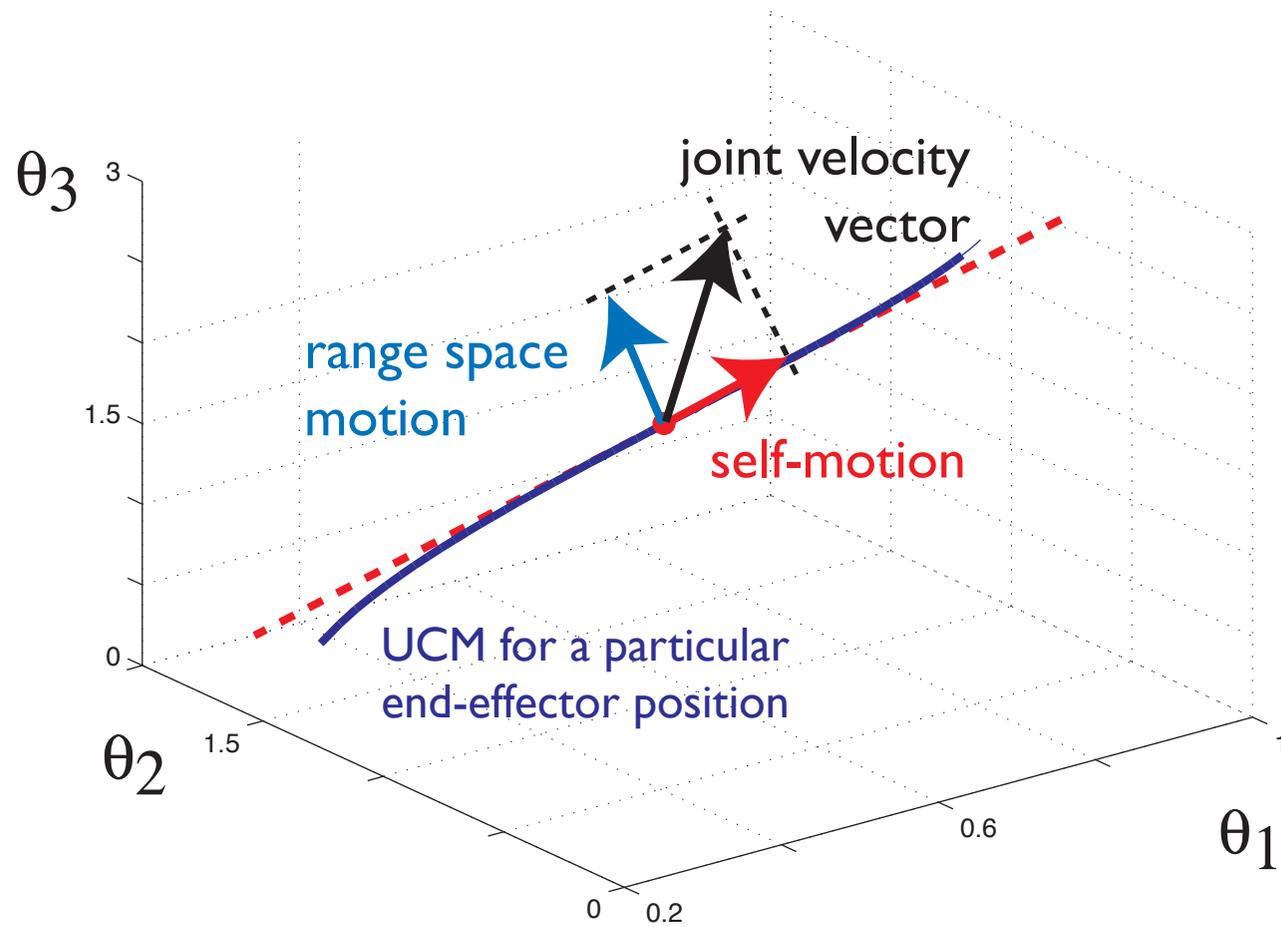
Self-motion

- all this was about variation/variance...
- how about the motion itself, the mean motion... does that reveal the DoF problem and its solution?
- => self-motion

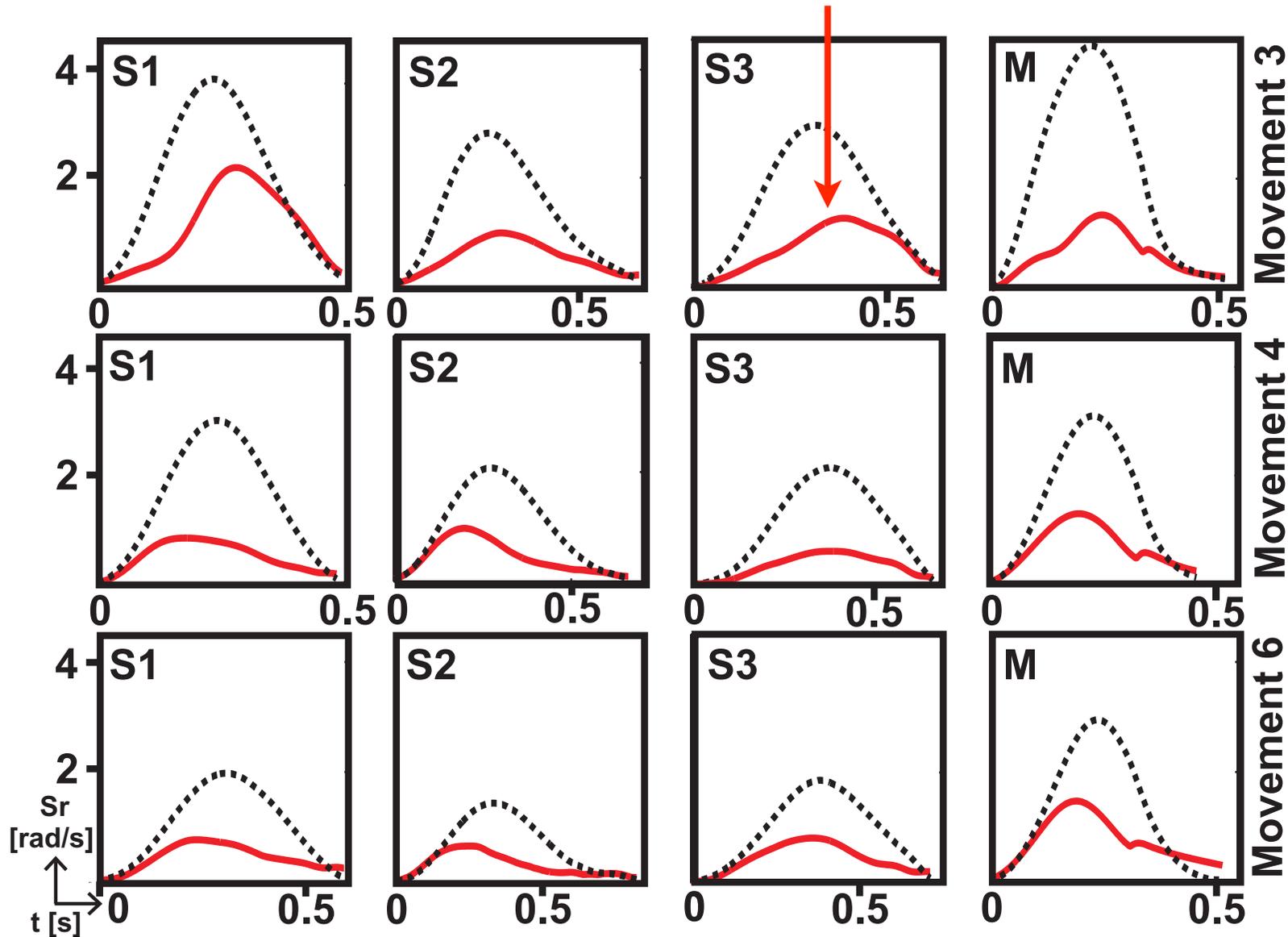
Self motion



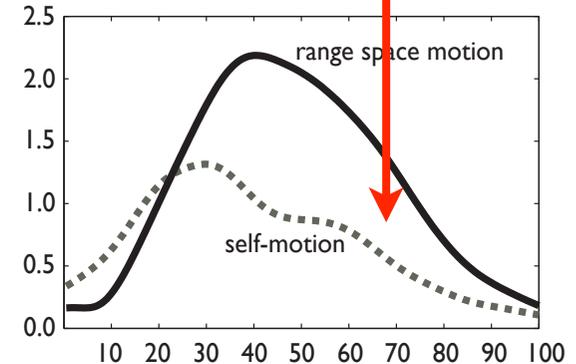
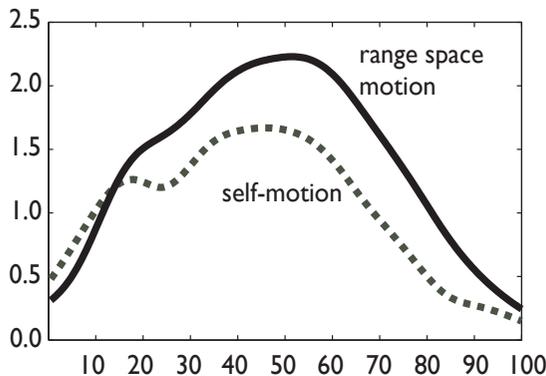
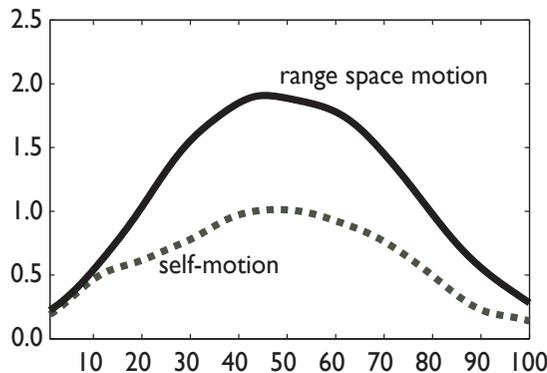
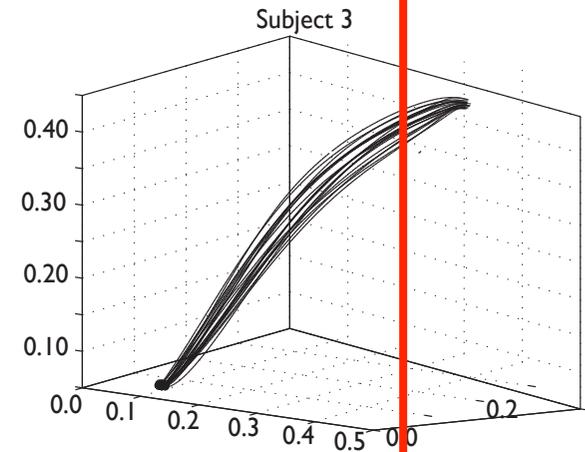
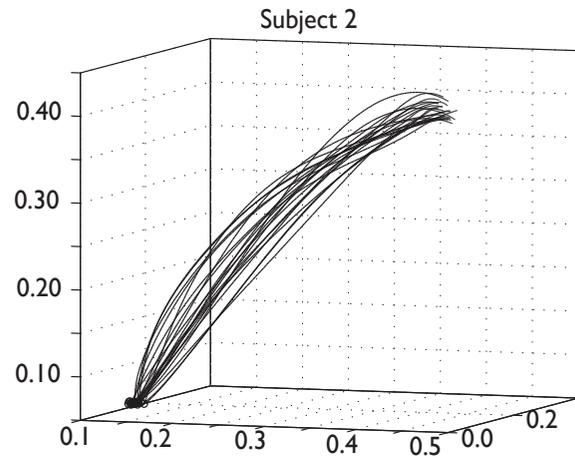
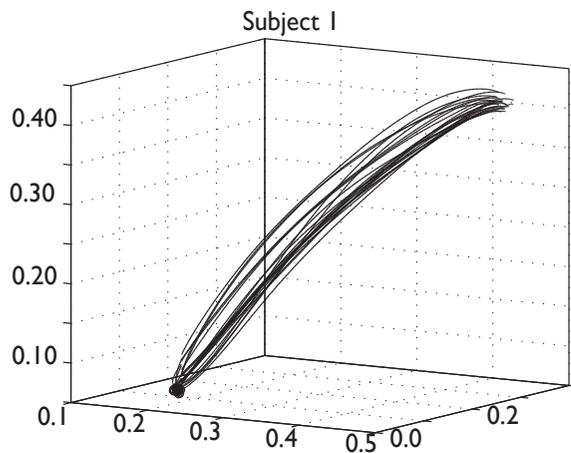
Self-motion



reaching in 2D, 4DoF: considerable amount of **self-motion!**



reaching movement in 3D, 10 DoF also shows considerable amount of **self-motion**



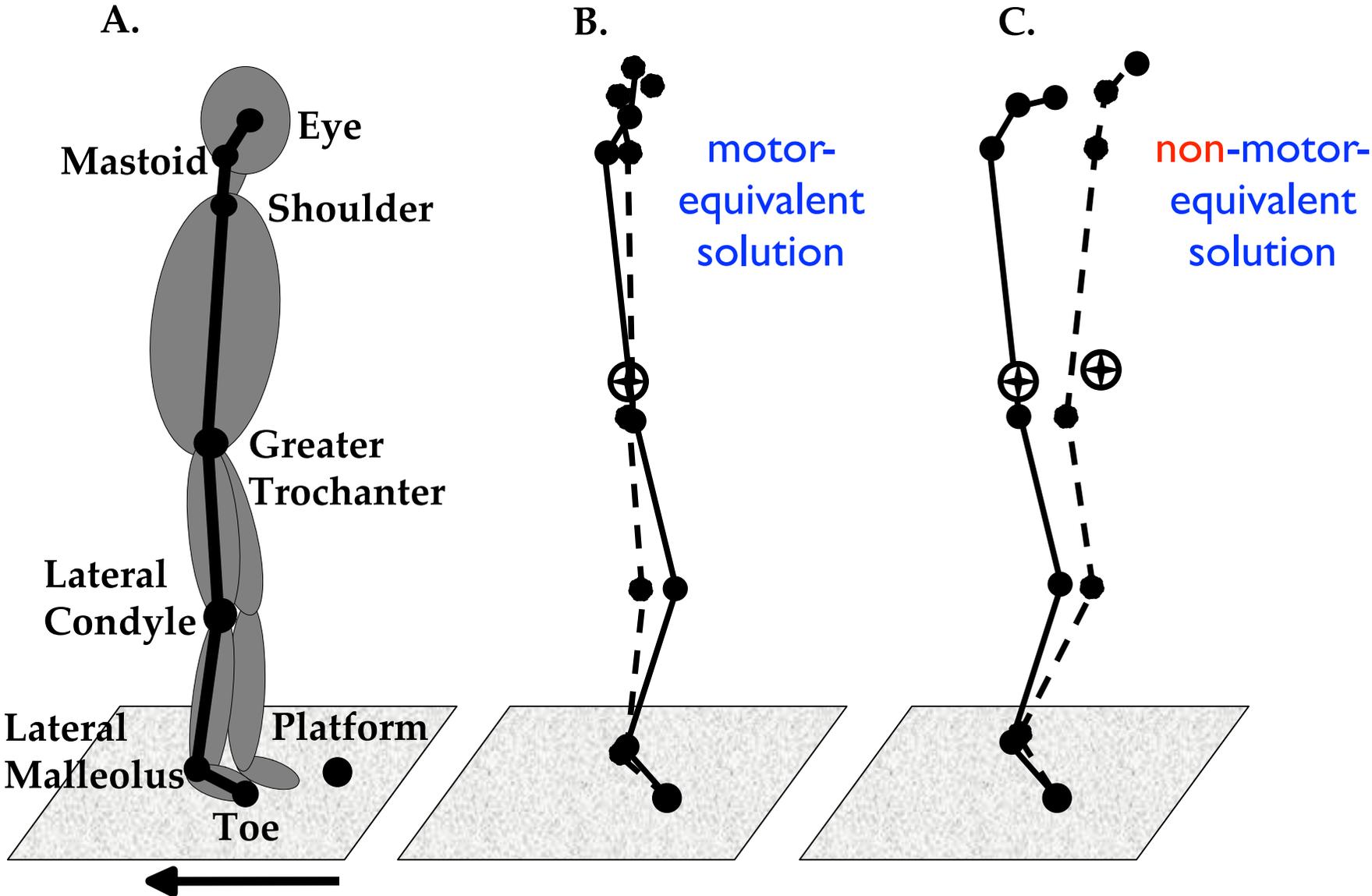
Motor equivalence

- can we see directly the use of the redundant/abundant DoF to solve some problem?
- motor equivalence: “task achieved with a new joint configuration following perturbation, different initial condition, or changed conditions”

Motor equivalence

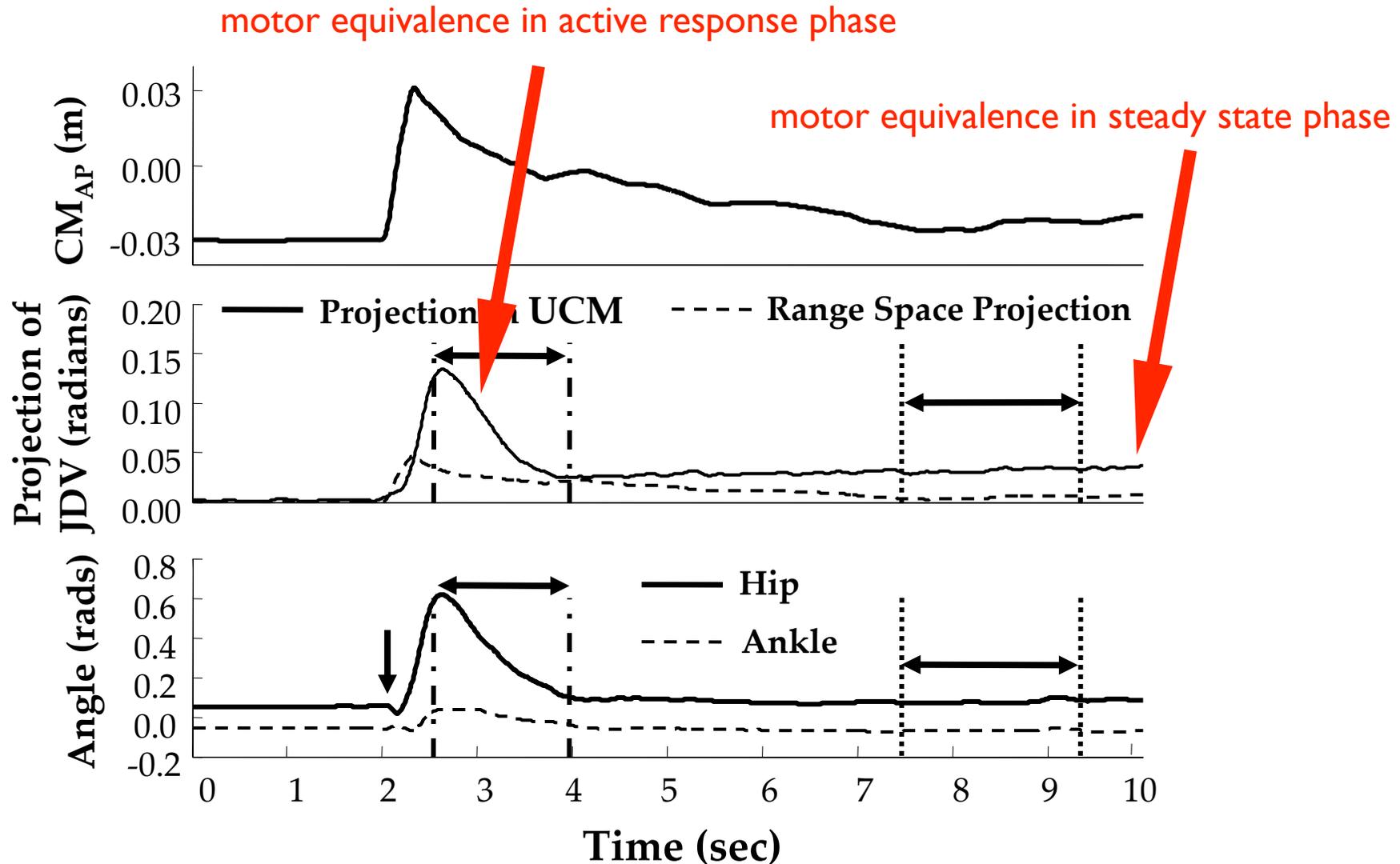
- “task achieved with other than standard joint configuration following perturbation or other change”
- but: task never achieved 100 percent
- how much error on task level compared to how much error at joint level? how do you compare?
- answer: error lies more within UCM than perpendicular!

Motor equivalence in quiet stance

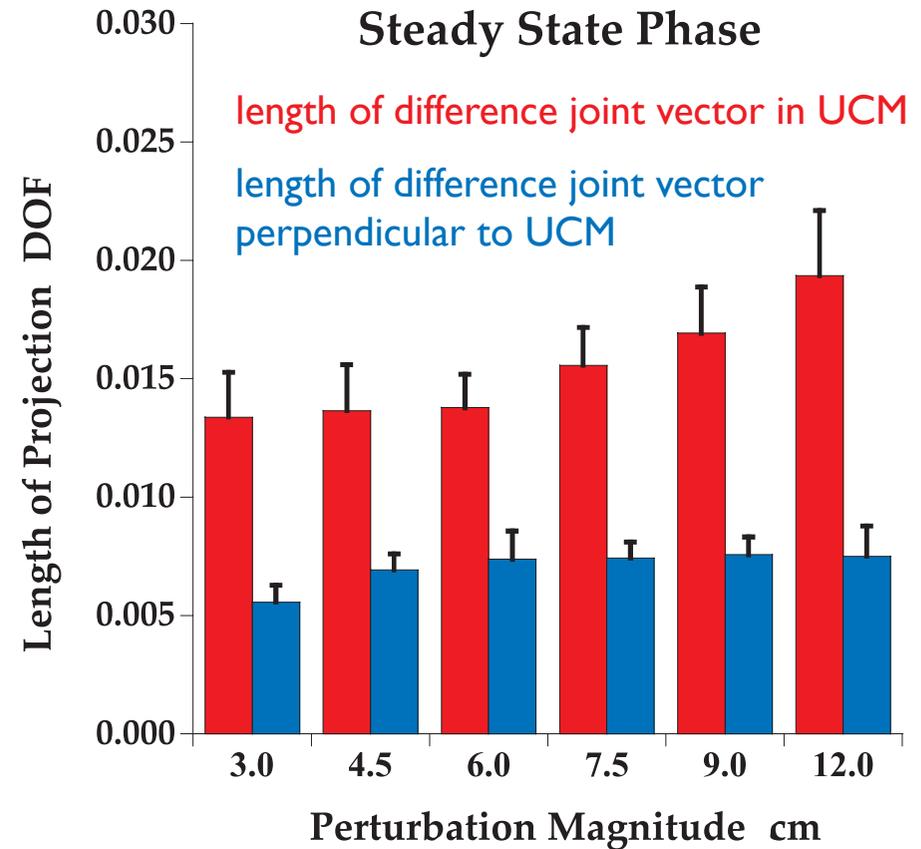
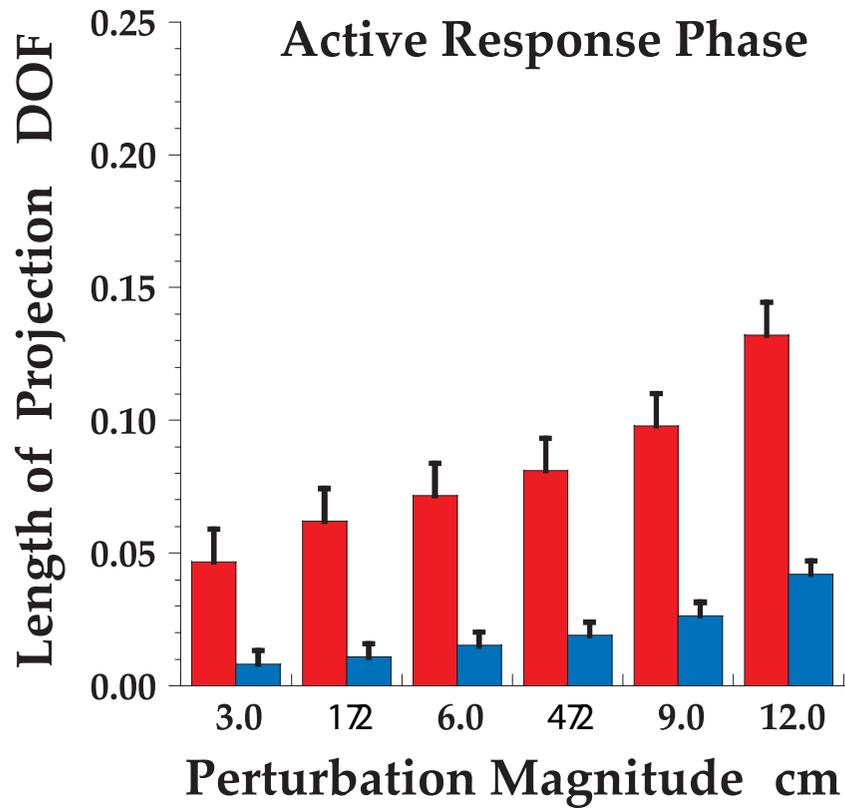


[Scholz, Schöner, Hsu, Jeka, Horak, Martin. *Exp Brain Res* (2007)]

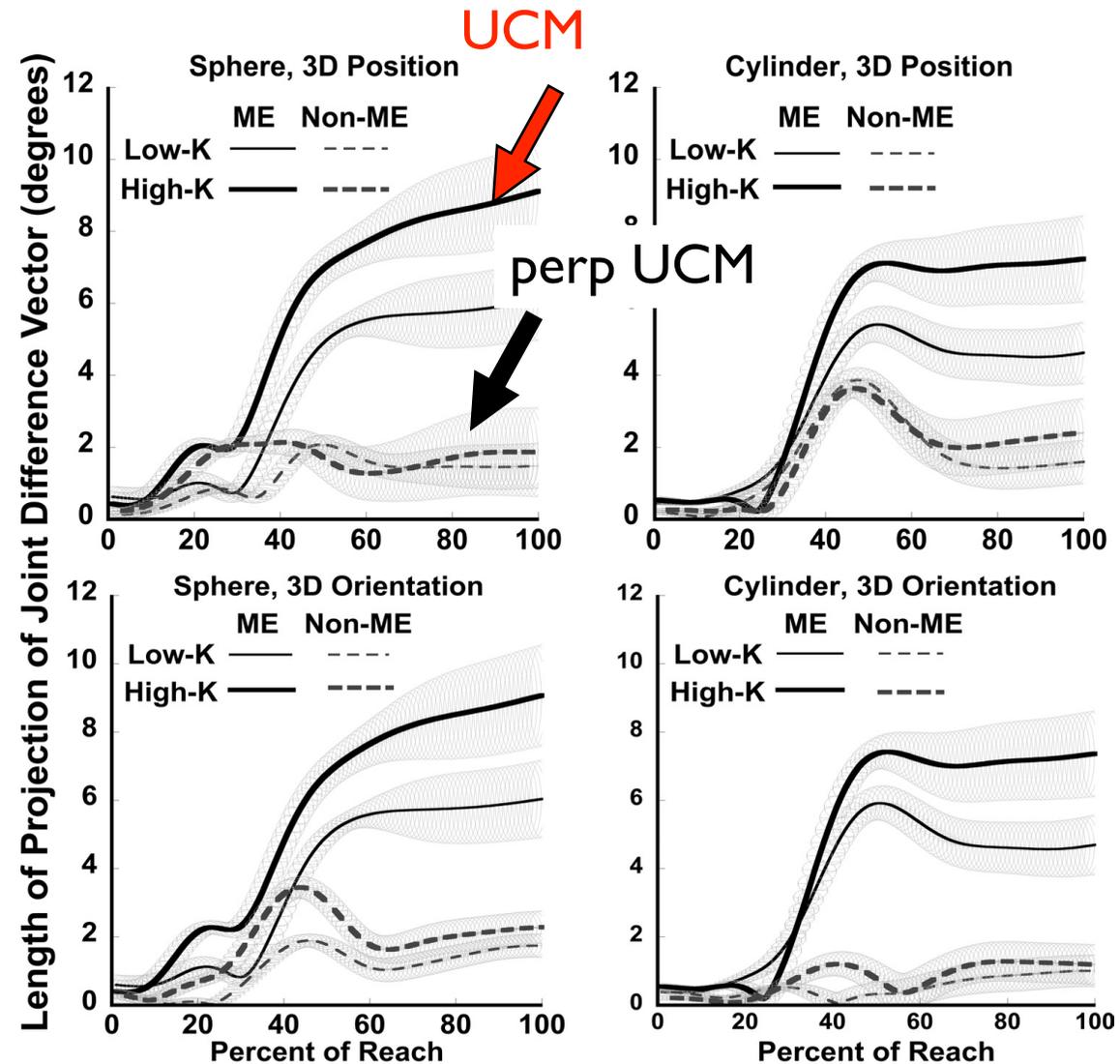
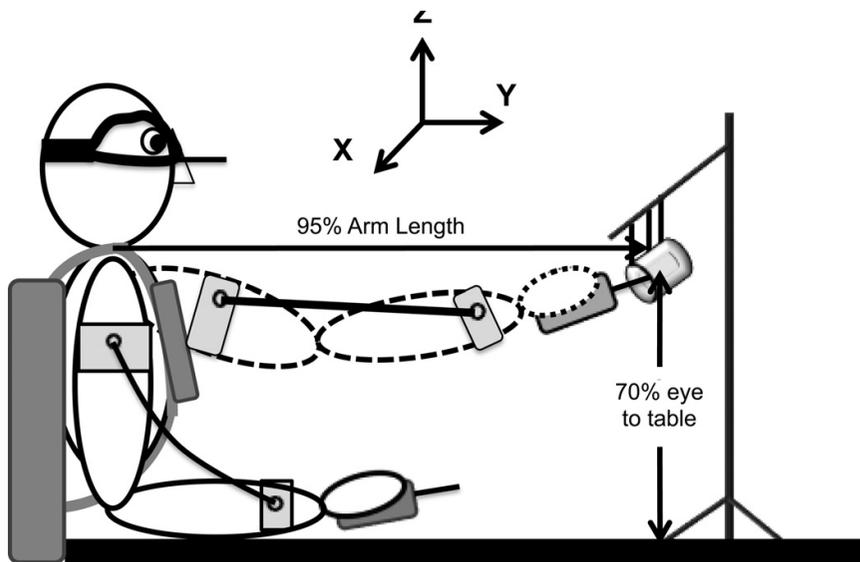
Motor equivalence in quiet stance



Motor equivalence in quiet stance



Motor equivalence in reaching



Model of UCM with back-coupling

$$\dot{\lambda} = \begin{pmatrix} \mathbf{J} \\ \mathbf{E}^T \end{pmatrix}^{-1} \cdot \begin{pmatrix} \mathbf{v} \\ \mathbf{s} \end{pmatrix} = \begin{pmatrix} \mathbf{J}^+ & \mathbf{E} \end{pmatrix} \cdot \begin{pmatrix} \mathbf{v} \\ \mathbf{s} \end{pmatrix} = \mathbf{J}^+ \cdot \mathbf{v} + \mathbf{E} \cdot \mathbf{s}$$

decoupling

end-effector virtual velocity

back-coupling into null space

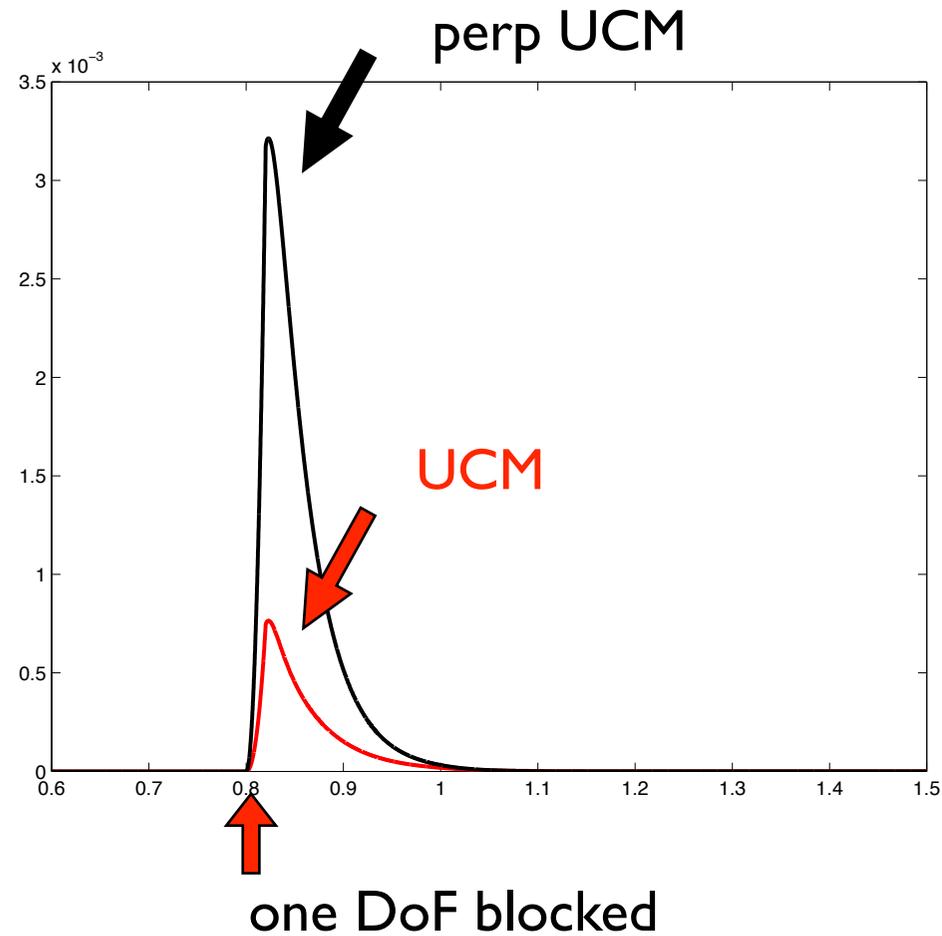
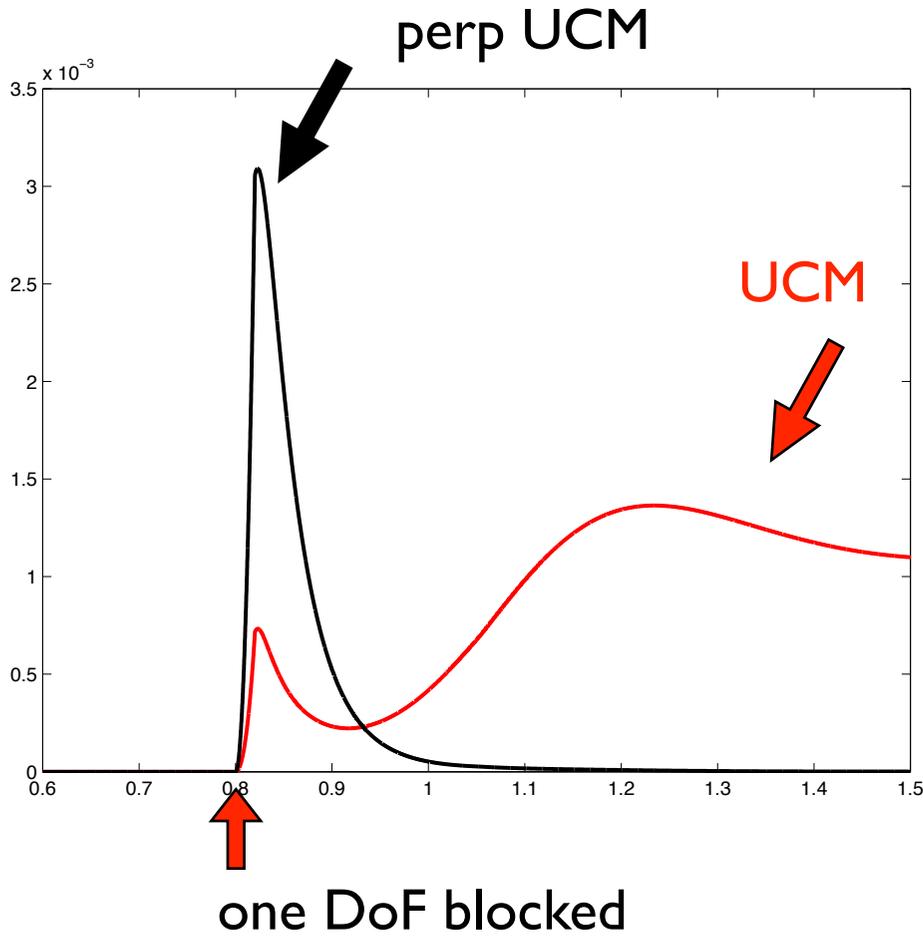
$$\dot{\mathbf{s}} = -\beta_{s1} \mathbf{E}^T \cdot (\boldsymbol{\lambda} - \boldsymbol{\theta}_d) - \beta_{s2} \mathbf{E}^T \cdot (\dot{\boldsymbol{\lambda}} - \dot{\boldsymbol{\theta}}_d).$$

Motor equivalence: model

amount of change in joint configuration induced by perturbation

with back-coupling

without back-coupling

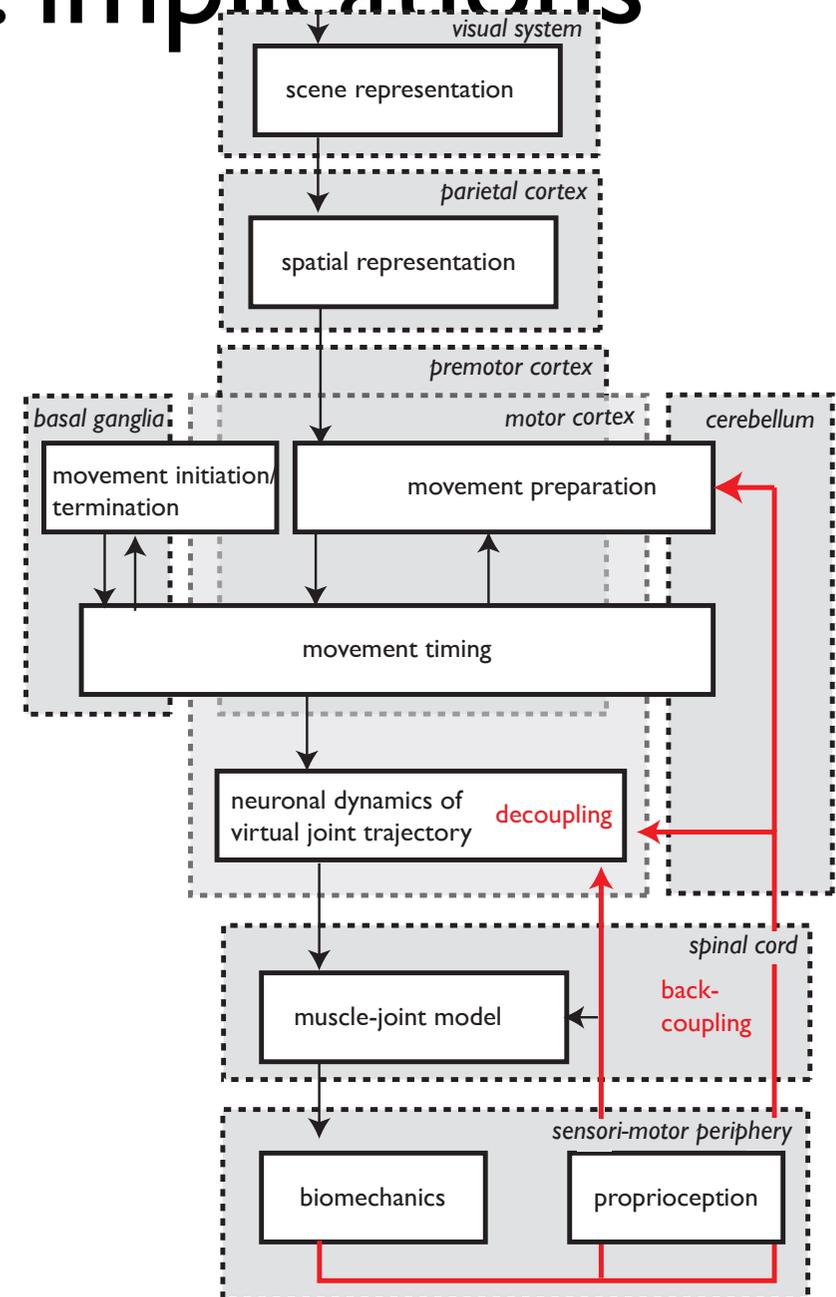


Motor equivalence: implications

- UCM structure of variance does not necessarily predict Motor Equivalence: a model that accounts for UCM variance does not predict Motor Equivalence
- But the mechanism that is critical for ME, back-coupling, also contributes to UCM variance.

Motor equivalence: implications

- back-coupling reflects that movement plans are in a loop, in which they “yield” to sensory information about the periphery
- => we need a better understanding of back-coupling



Conclusions

- Synergy has two aspects:

- descending neural organization induces co-variation

- recurrent coupling induces UCM structure

- these are caused by two different portions of a neural network

- the feed-forward projection from motor command to DoF

- and recurrent connections and/or feedback to the motor command level

- Back-coupling

- a new hypothesis that goes beyond UCM and synergy

Account for both/all

■ forward projection plus

■ external or

■ internal feedback loop

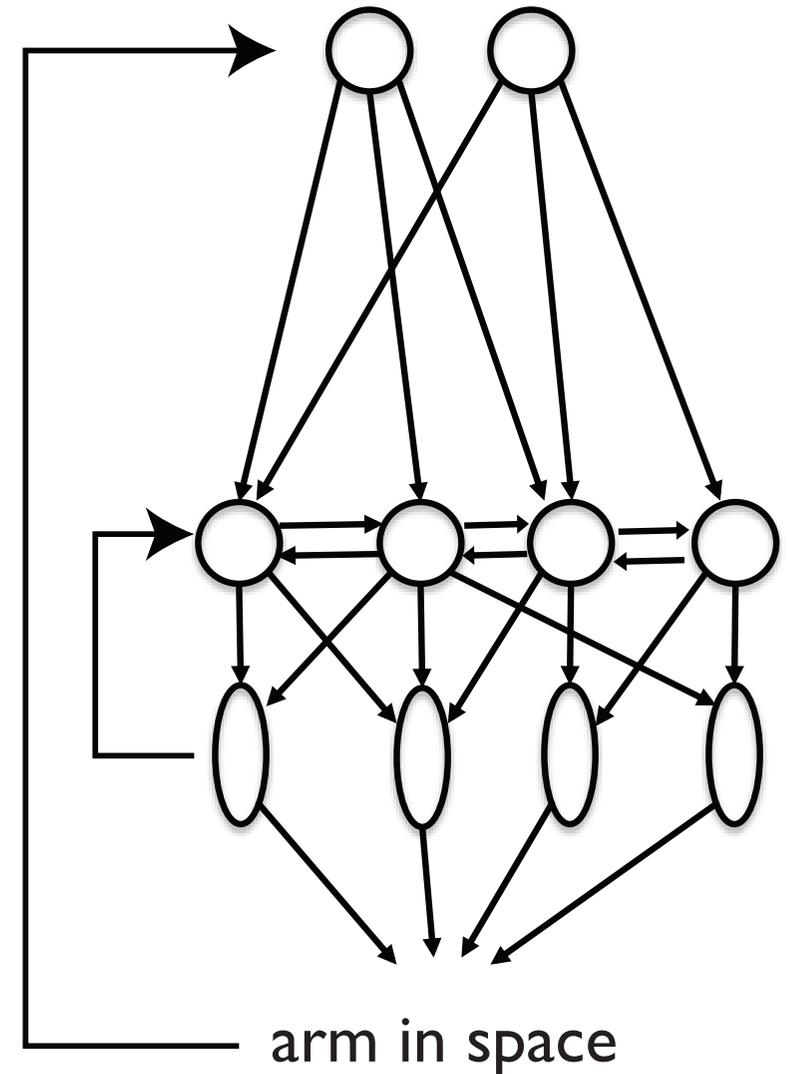
■ back-coupling

■ accounts for

■ structure of variance

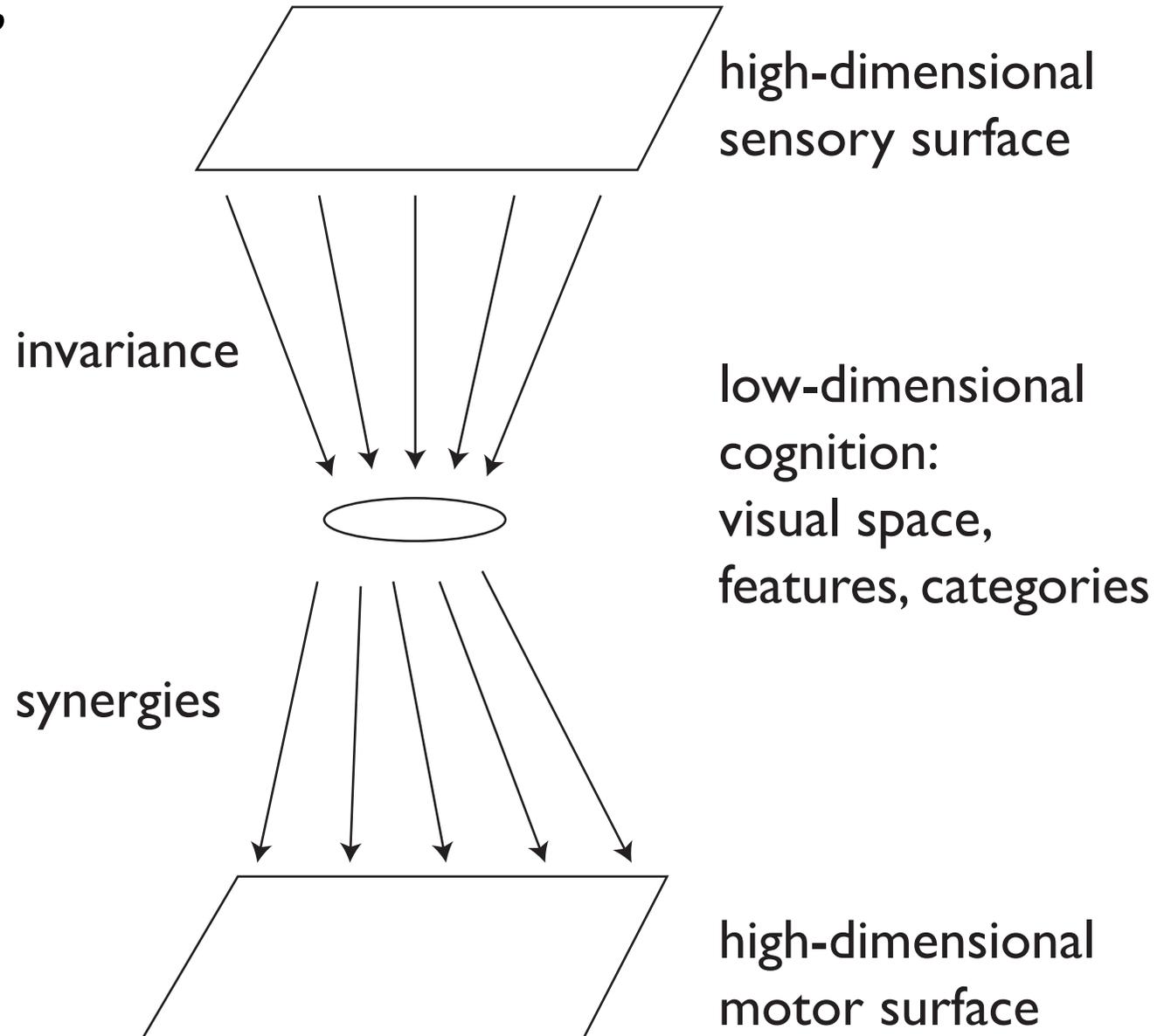
■ self-motion

■ motor equivalence



Conclusion

■ the “hour-glass” metaphor



Principles

